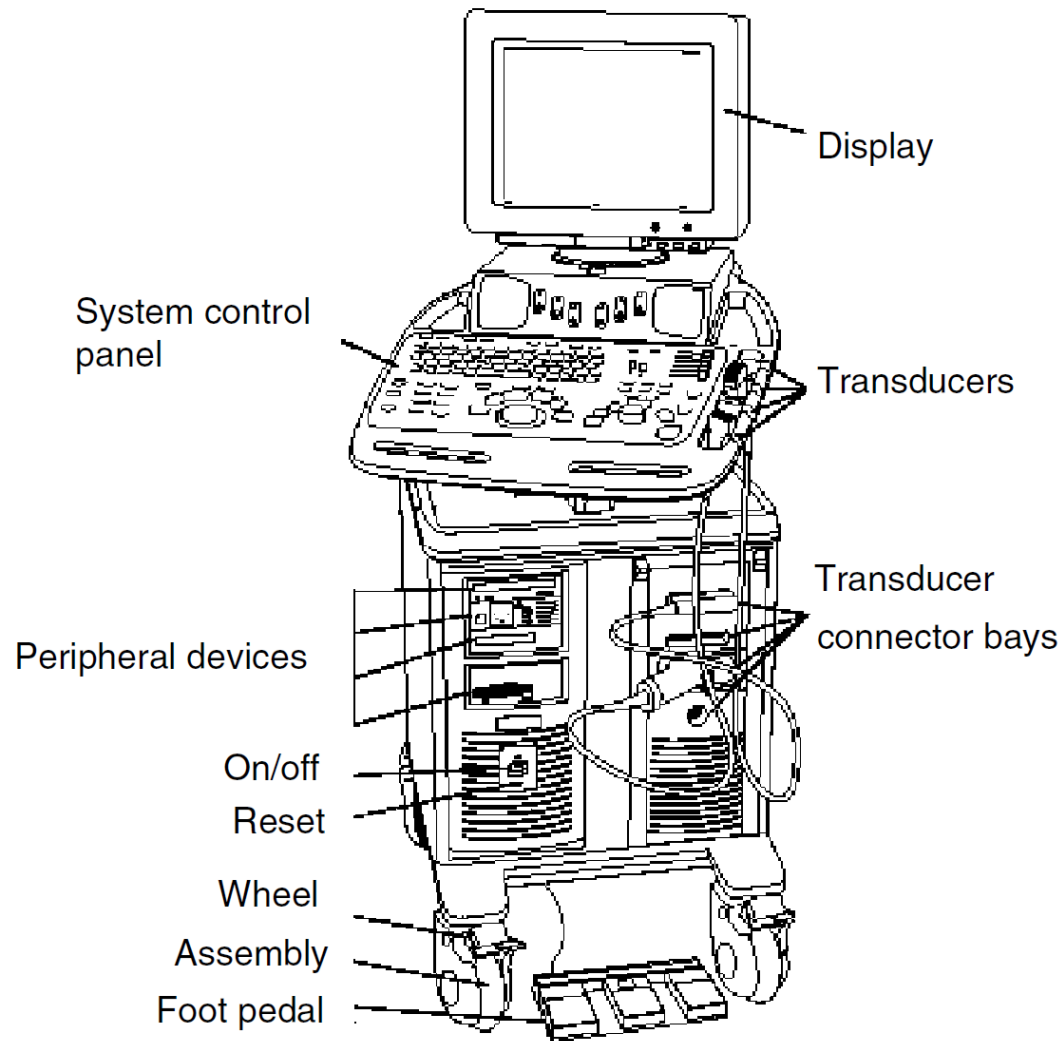


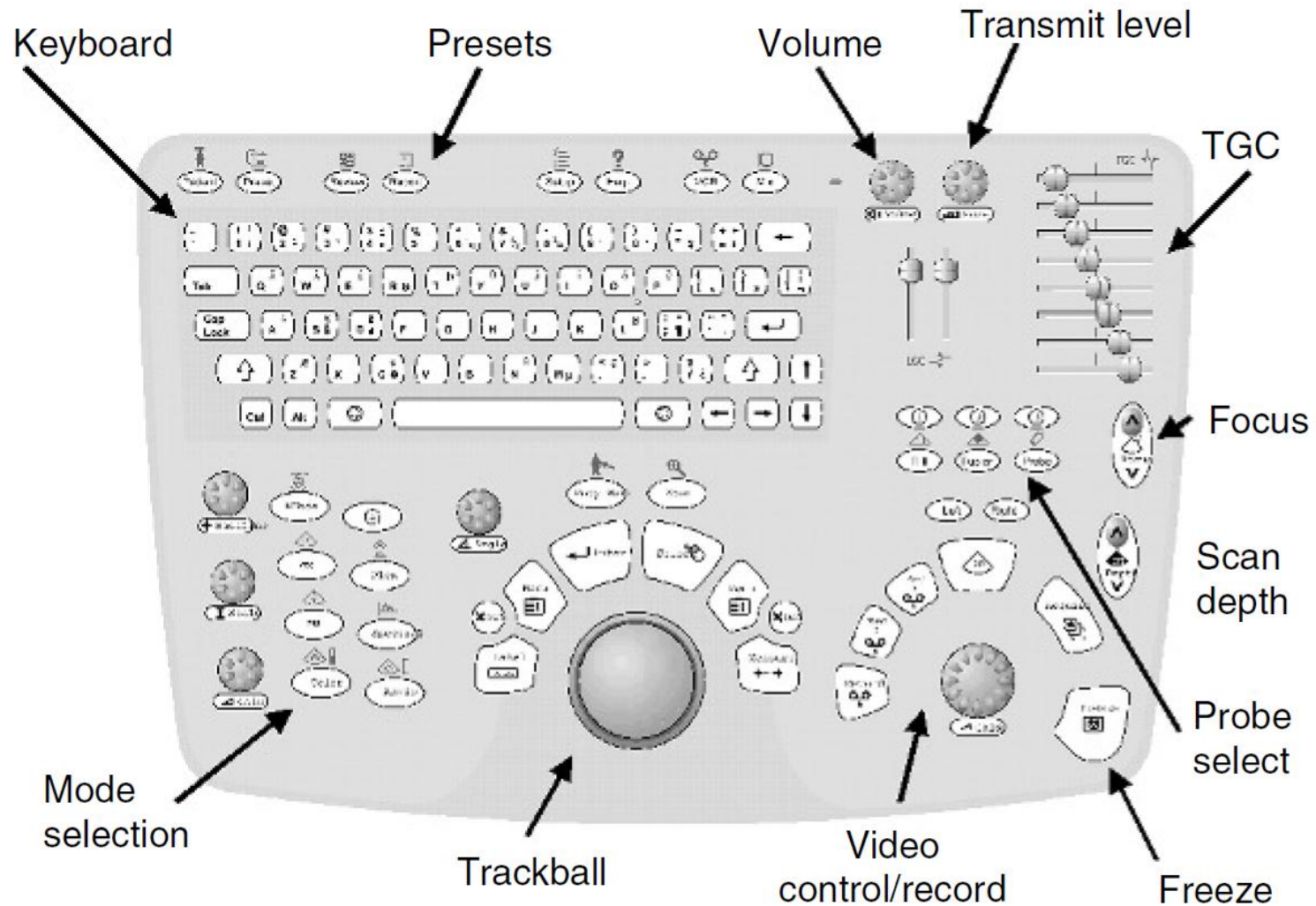
MEDICAL EQUIPMENT (4)

TOPIC 1: ULTRASOUND IMAGING

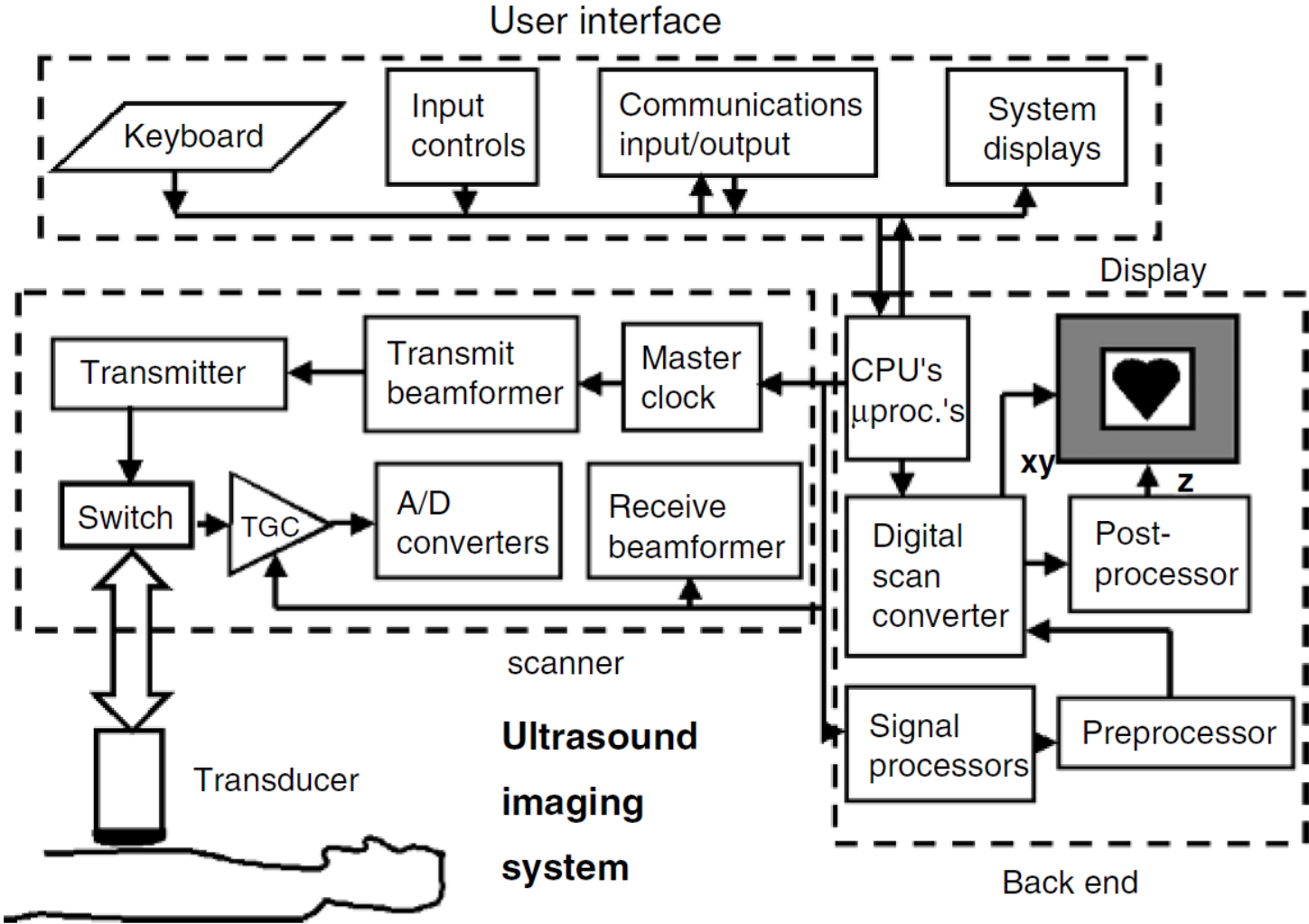
Ultrasound Imaging System: External Look



Keyboard Controls



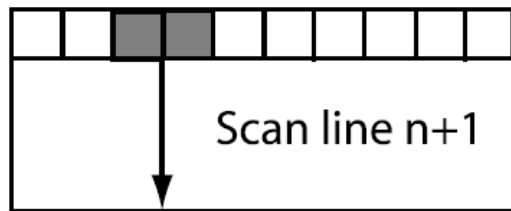
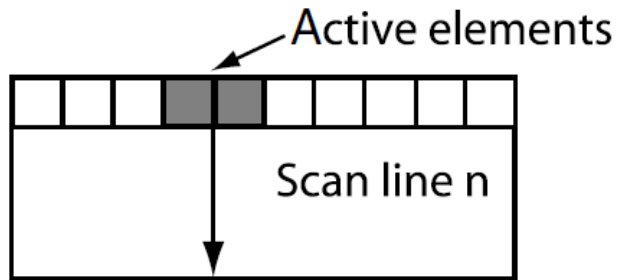
Block Diagram



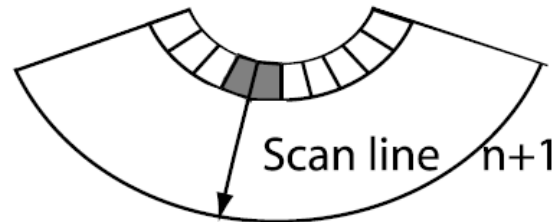
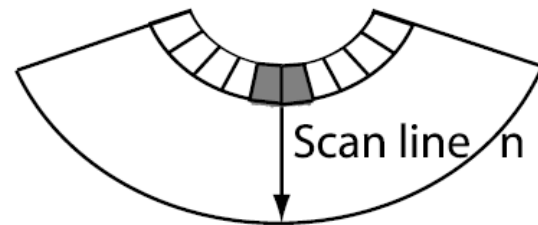
Ultrasound Transducers



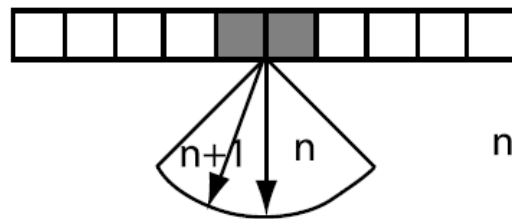
Image Formats



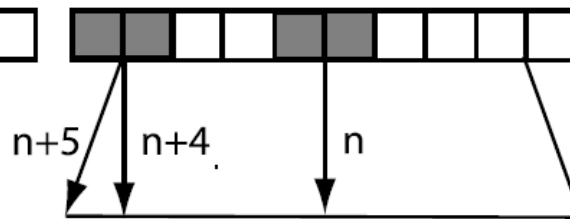
A Linear (translation)



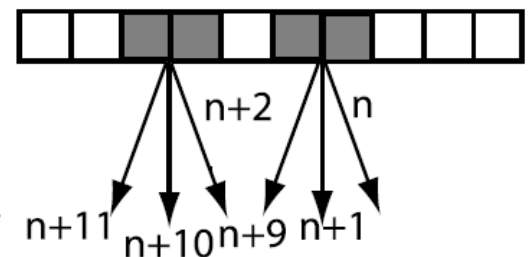
B Convex (translation)



C Sector (rotation)



D Trapezoidal (contiguous)



E Compound

Major Modes:

B-Mode (2D Mode)

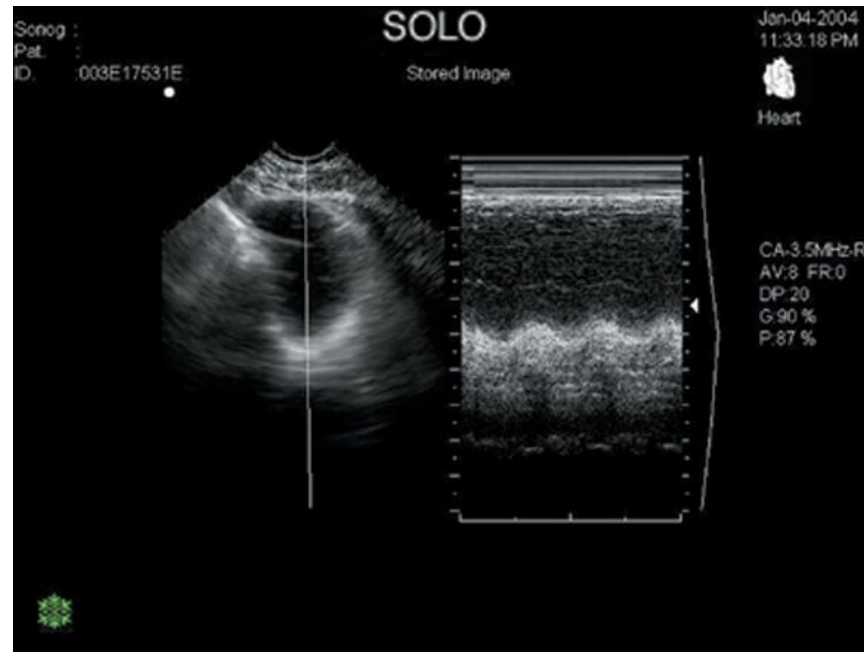
- Brightness-modulated image in which depth is along the z axis and azimuth is along the x axis.
 - The position of the echo is determined by its acoustic transit time and beam direction in the plane.



Major Modes:

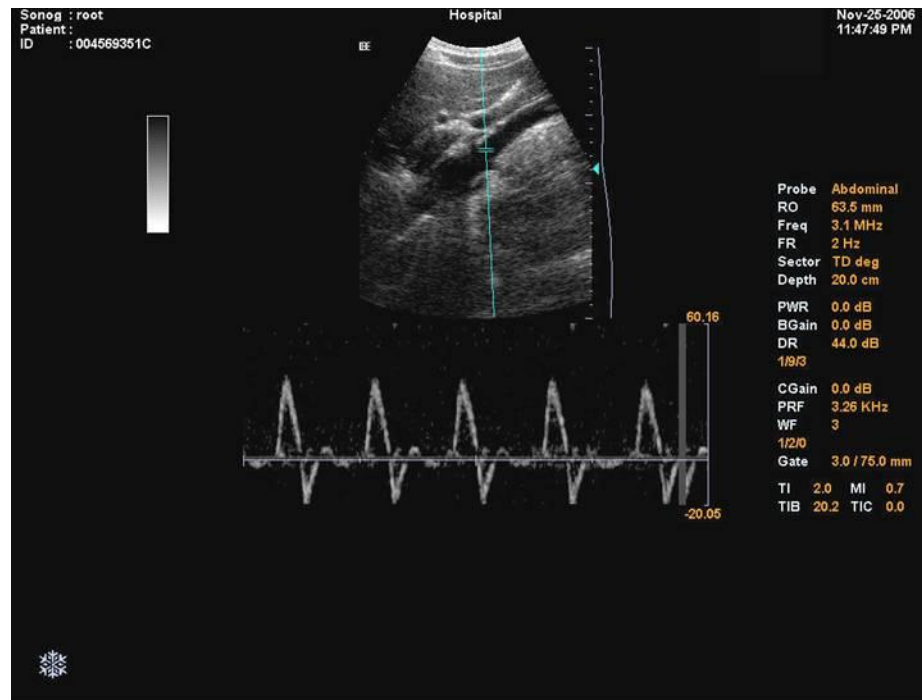
M-Mode

- Brightness modulated, where depth is the y deflection (fast time), and the x deflection is the same imaging line shown as a function of slow time.
 - ▣ Time history of single line at the same position over time



Major Modes: Doppler-Mode

- This is the presentation of the Doppler spectrum
 - ▣ Continuous wave (CW) Doppler
 - ▣ Pulsed wave (PW) Doppler



Major Modes:

Color Flow Mapping Mode (CFM)

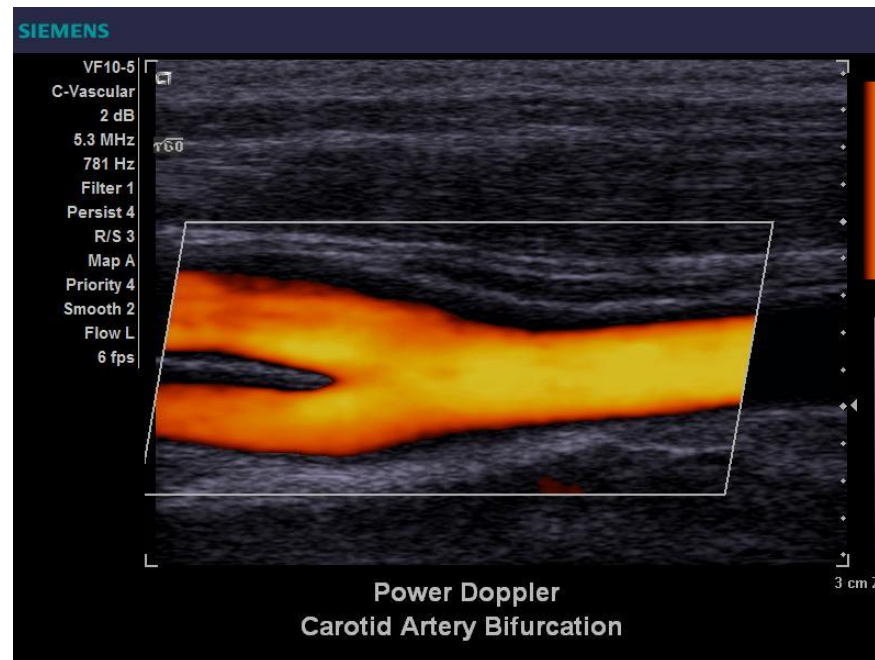
- Spatial map overlaid on a B-mode gray-scale image that depicts an estimate of blood flow mean velocity
 - Direction of flow encoded in colors (blue away from the transducer and red toward it)
 - Amplitude of mean velocity by brightness, and turbulence by a third color (often green).



Major Modes:

Power Doppler Mode

- This color-coded image of blood flow is based on intensity rather than on direction of flow, with a paler color representing higher intensity.
 - ▣ It is also known as “angio”



Secondary Modes

- Duplex
 - ▣ Presentation of two modes simultaneously: usually 2D and pulsed (wave) Doppler
- Triplex
 - ▣ Presentation of three modes simultaneously: usually 2D, color flow, and pulsed Doppler
- 3D
 - ▣ Display or Surface/volume rendering used to visualize volume composed of multiple 2D slices.
- 4D
 - ▣ A 3D image moving in time

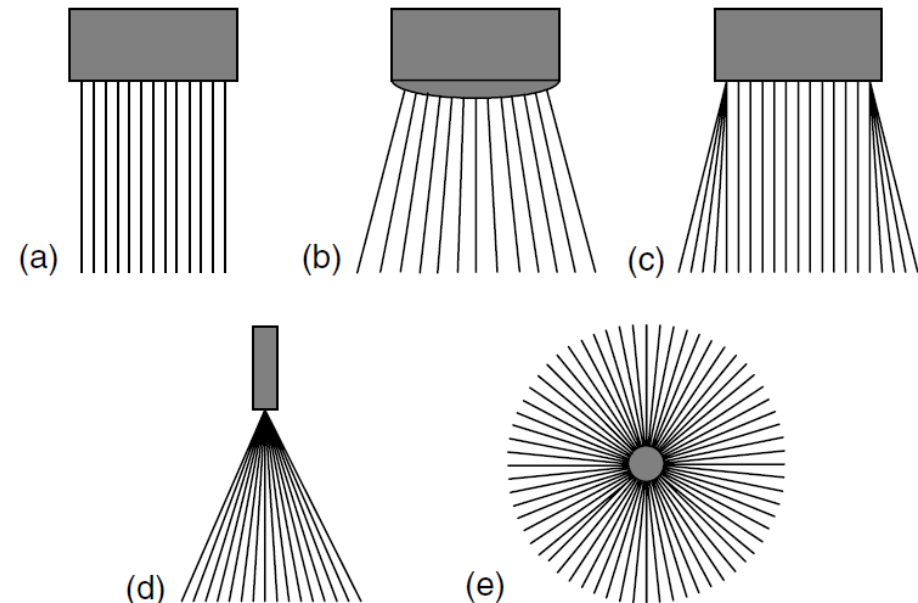
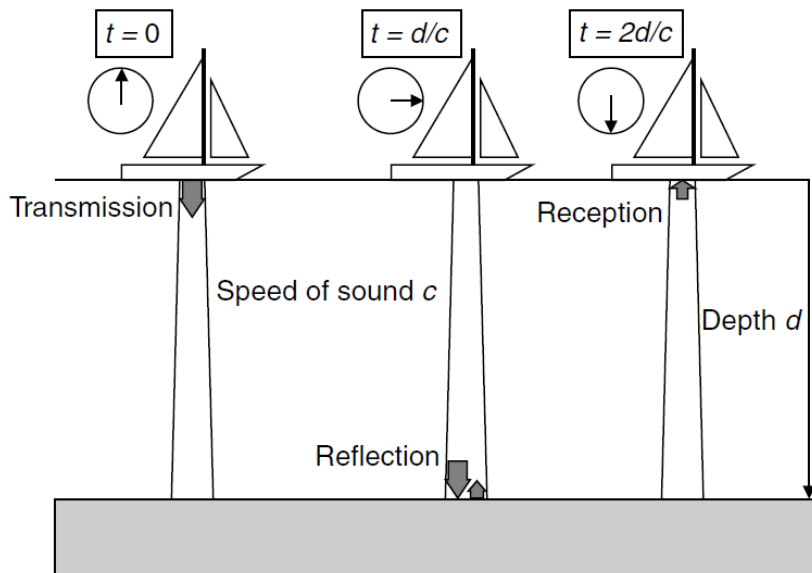
Introduction to B-mode imaging

- B-mode image is an anatomic cross-sectional image
- Constructed from echoes (reflection and scattering) of waves
- Echo is displayed at a point in image, which corresponds to relative position of its origin within the body cross section
- Brightness of image at each point is related to strength of echo
 - ▣ Term B-mode stands for Brightness-mode



Echo Ranging

- To display each echo in a position corresponding to that of the interface or feature (known as a target) that caused it, the B-mode system needs two pieces of information:
 - ▣ (1) Range (distance) of the target from the transducer
 - ▣ (2) Position and orientation of the ultrasound beam



Ultrasound Physics

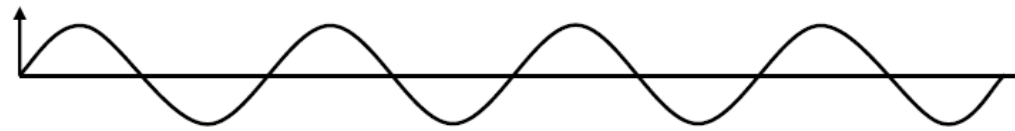
- Sound waves used to form medical images are longitudinal waves, which propagate (travel) only through a physical medium (usually tissue or liquid)
 - ▣ Characterized by frequency, wavelength, speed and phase

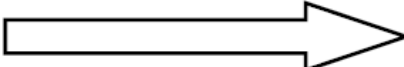
$$c = f\lambda$$

$$\text{Speed of sound } c = \sqrt{\frac{k}{\rho}}$$

Material	c (m s ⁻¹)
Liver	1578
Kidney	1560
Amniotic fluid	1534
Fat	1430
Average tissue	1540
Water	1480
Bone	3190–3406
Air	333

Pressure



Direction of propagation 



Particle displacement

Ultrasound Physics

- Medical ultrasound frequencies used in the range 2–15 MHz
 - Higher frequencies are now utilized for special applications
 - Resolution proportional to wavelength

f (MHz)	λ (mm)
2	0.77
5	0.31
10	0.15
15	0.1

- Acoustic impedance

- p is the local pressure $z = p/v$ the local particle velocity.
- Analogous to electrical impedance (or resistance R)

$$z = \sqrt{\rho k} = \rho c$$

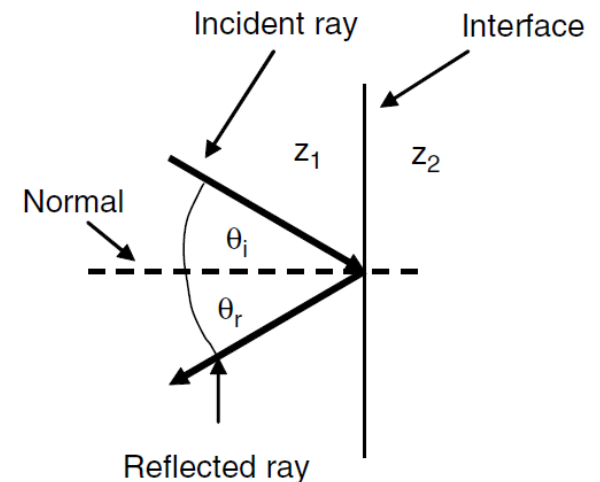
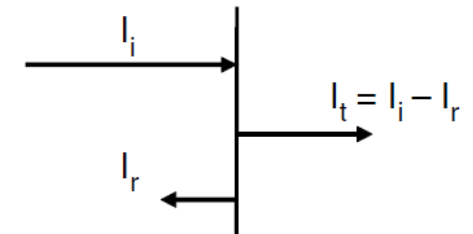
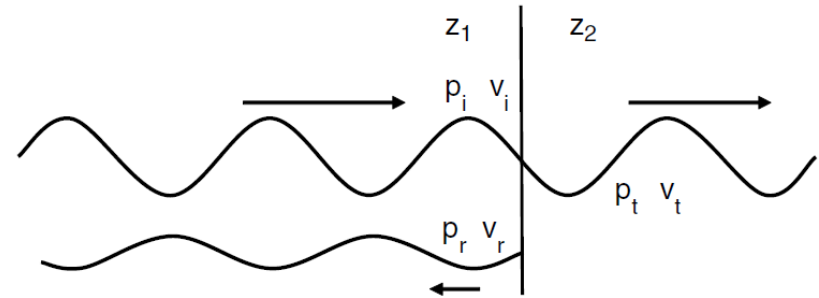
Material	z ($\text{kg m}^{-2} \text{s}^{-1}$)
Liver	1.66×10^6
Kidney	1.64×10^6
Blood	1.67×10^6
Fat	1.33×10^6
Water	1.48×10^6
Air	430
Bone	6.47×10^6

Ultrasound Physics

□ Reflection: Large Interfaces

$$R_A = \frac{P_r}{P_i} = \frac{z_2 - z_1}{z_2 + z_1}$$

$$\frac{I_r}{I_i} = R_i = R_A^2$$



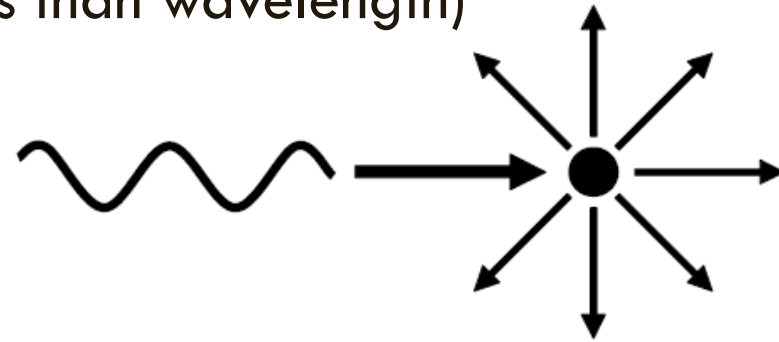
$$\theta_r = \theta_i$$

Interface	R_A
Liver-kidney	0.006
Kidney-spleen	0.003
Blood-kidney	0.009
Liver-fat	0.11
Liver-bone	0.59
Liver-air	0.9995

Ultrasound Physics

- Scattering: **Small Interfaces** (size less than wavelength)

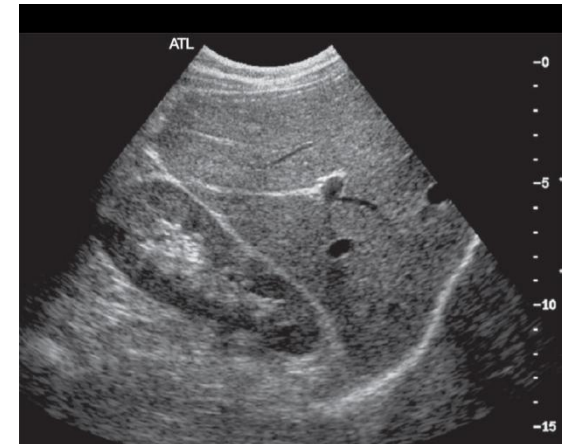
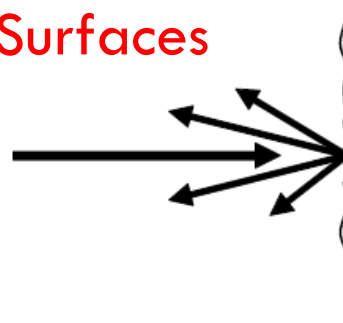
$$W_s \propto \frac{d^6}{\lambda^4} \propto d^6 f^4$$



- Two important aspects of scattering:

- ▣ Ultrasonic power scattered back is small compared to reflections
- ▣ Beam angle-independent appearance in the image unlike reflections

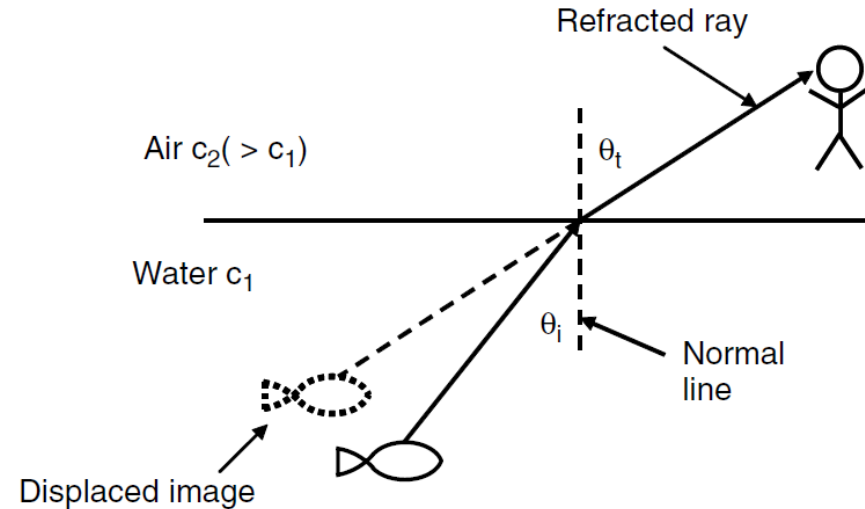
- Diffuse Reflection: **Rough Surfaces**



Ultrasound Physics

□ Refraction: Snell's law

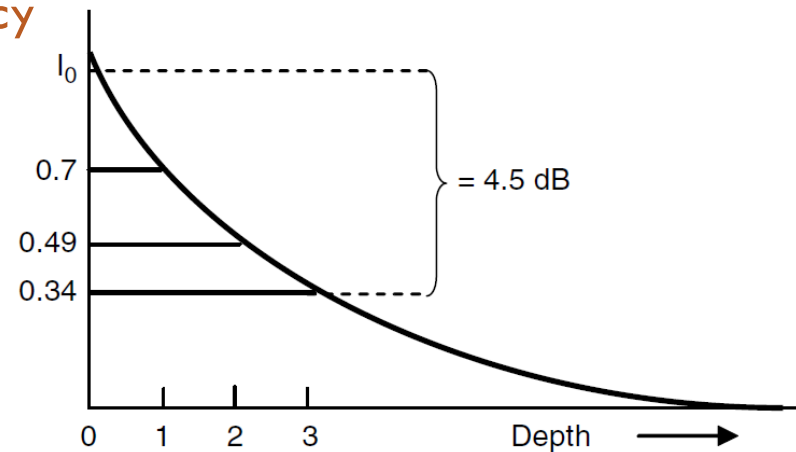
$$\frac{\sin \theta_i}{\sin \theta_t} = \frac{c_1}{c_2}$$



□ Attenuation: gradual loss of beam energy

□ Depends on both distance and frequency

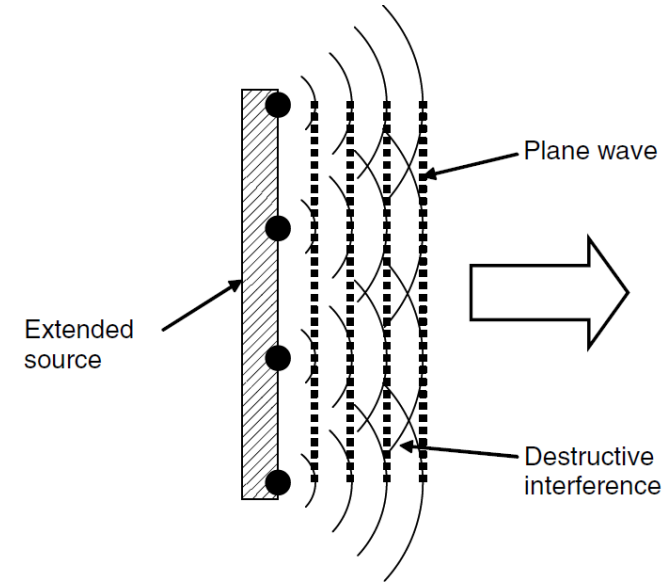
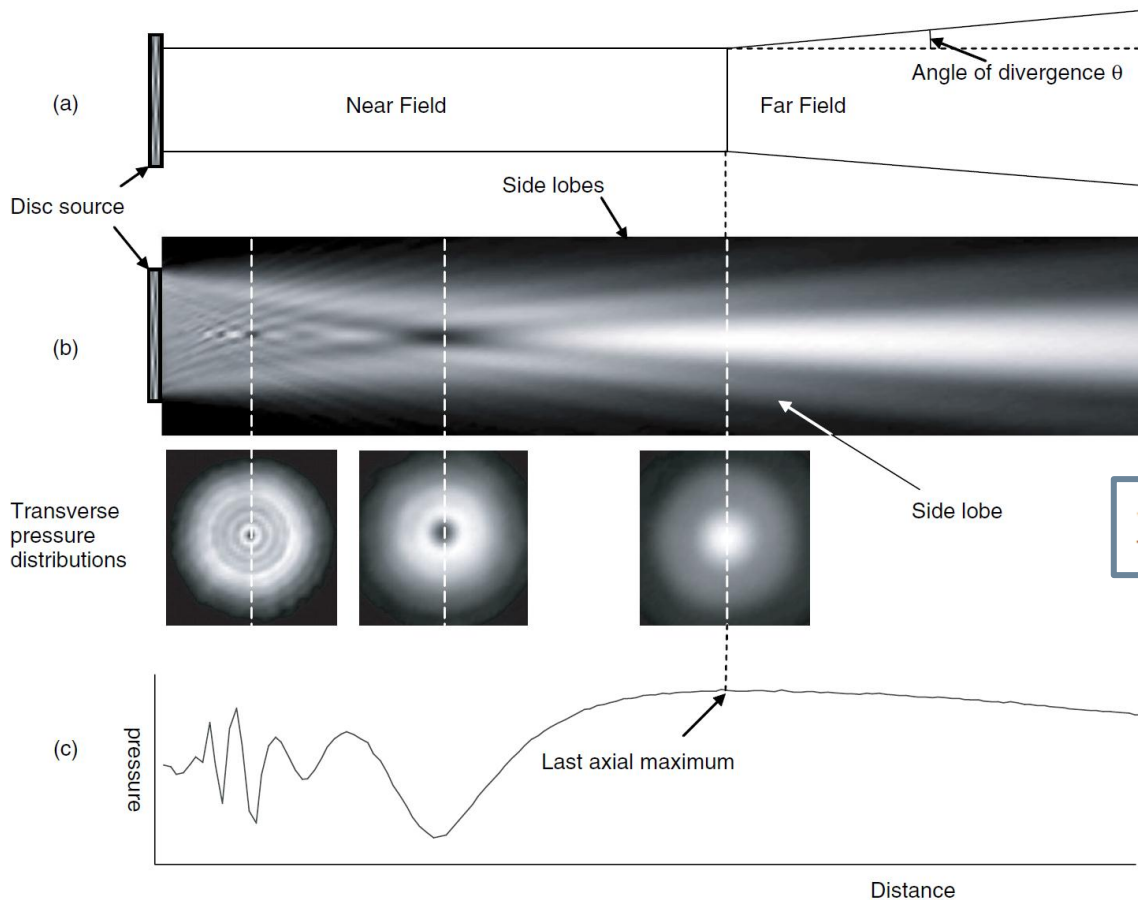
Tissue	Attenuation (dB cm ⁻¹ MHz ⁻¹)
Liver	0.399
Brain	0.435
Muscle	0.57
Blood	0.15
Water	0.02
Bone	22



Ultrasound Physics

□ Interference and diffraction

▣ Constructive/Destructive interference

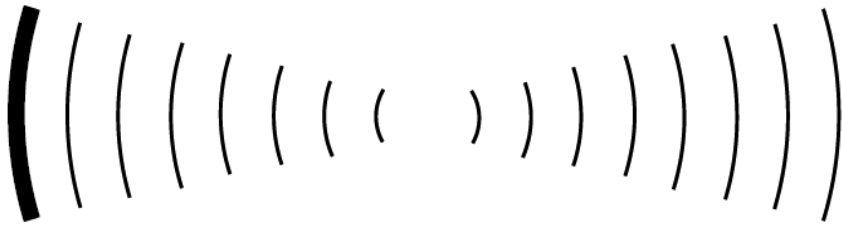


$$\text{near field length} = a^2/\lambda$$

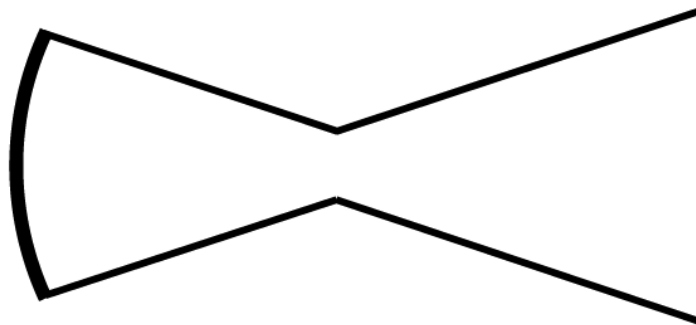
$$\sin \theta = 0.61 (\lambda/a)$$

Ultrasound Physics

□ Focusing: narrower ultrasound beam



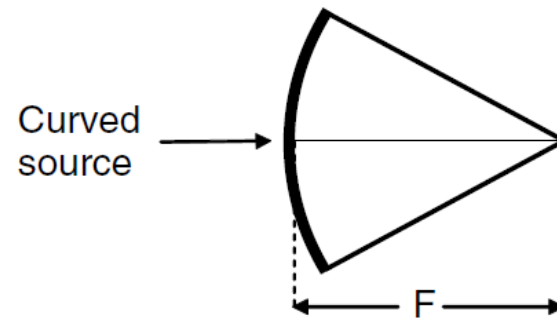
(a)



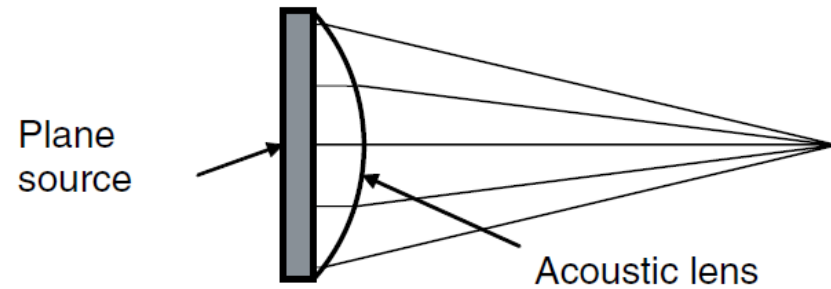
(b)



(c)



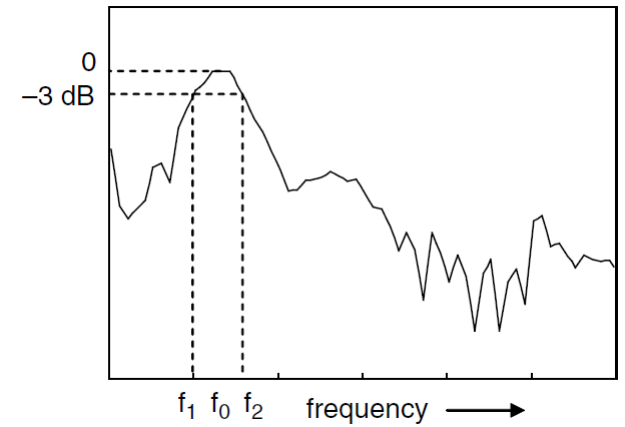
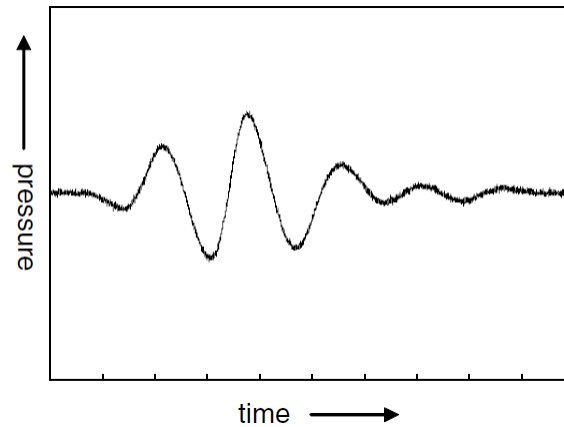
(a)



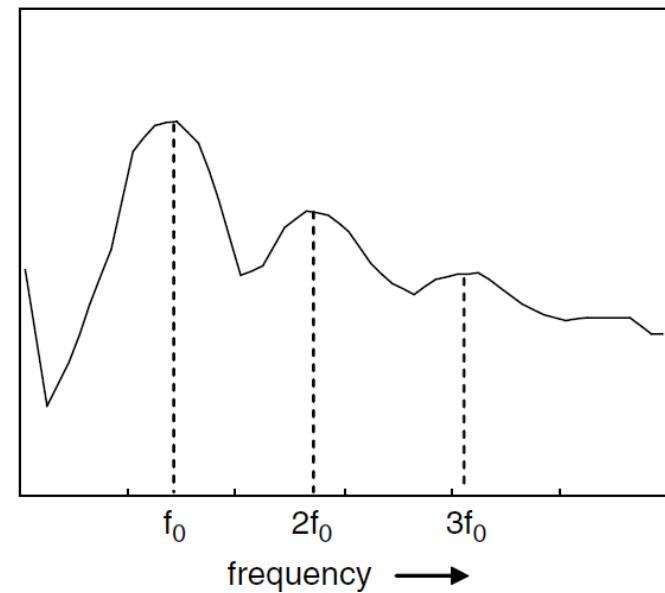
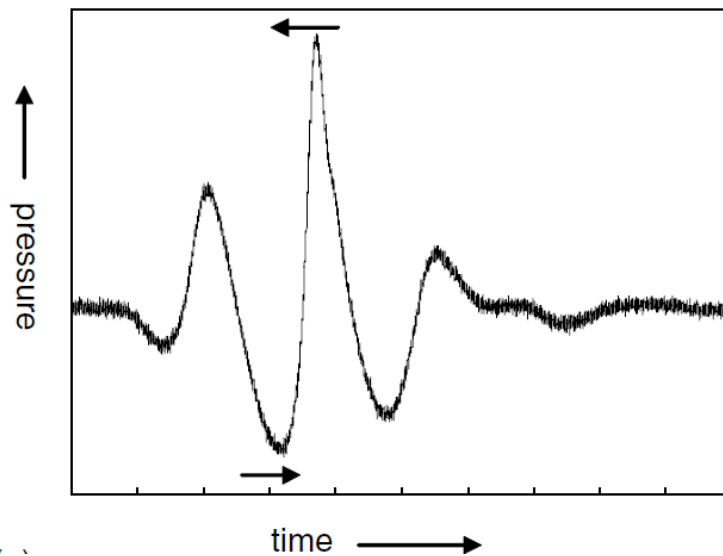
(b)

Ultrasound Physics

□ Ultrasound pulse

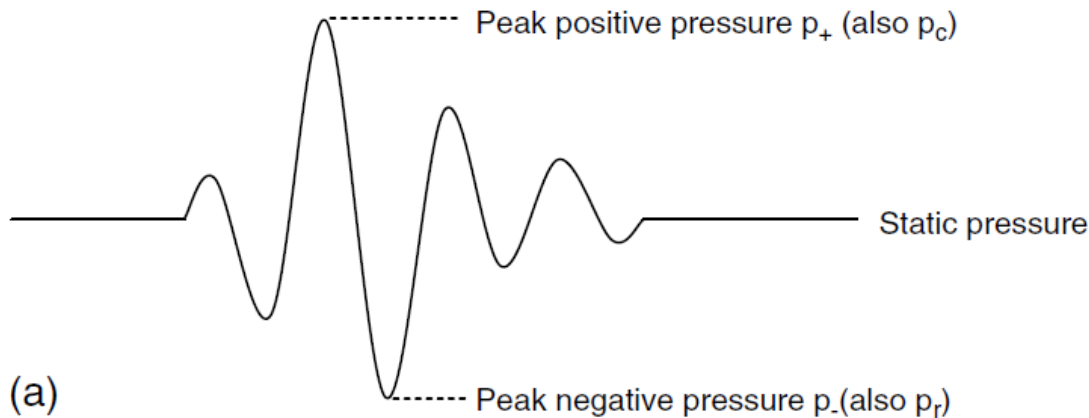


□ Harmonic Imaging

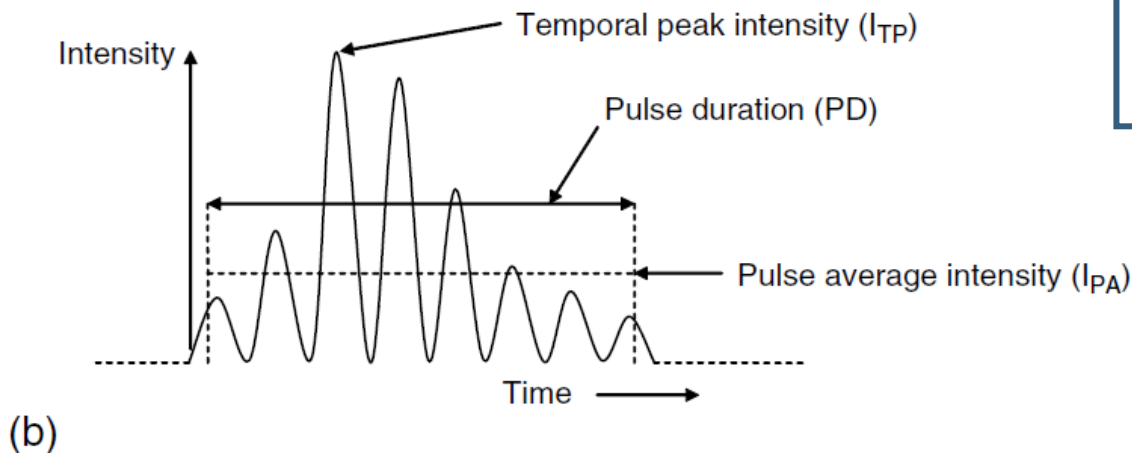


Ultrasound Physics

□ Acoustic pressure and intensities within ultrasound beam



$$I = \frac{p^2}{z}$$

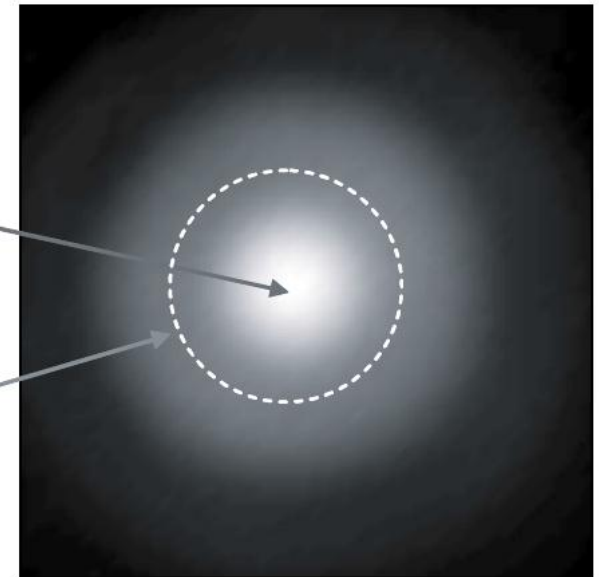
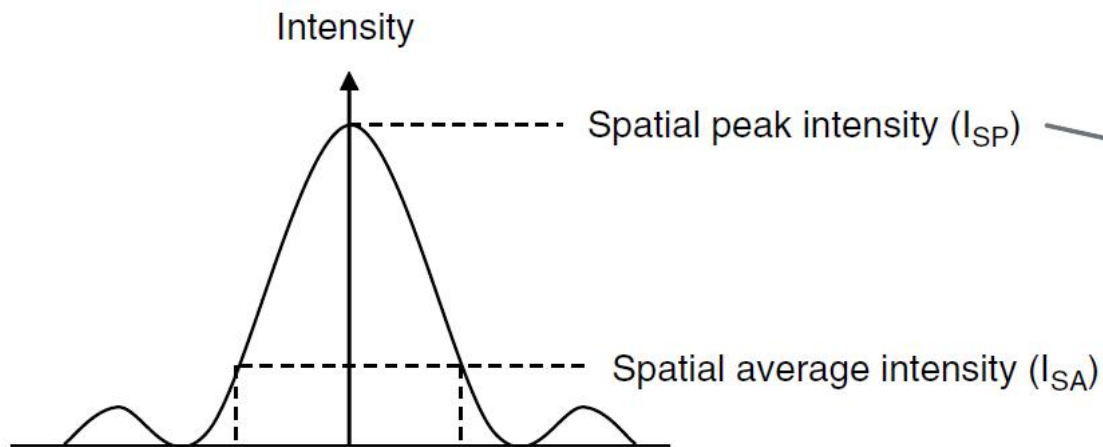
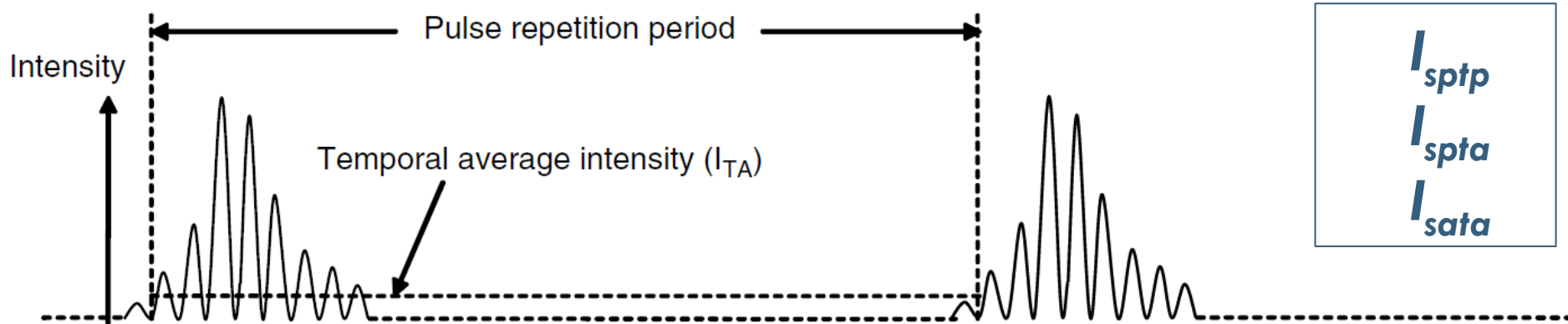


$$PD = 1.25 \times (T_{90} - T_{10})$$

$$I_{PA} = PII / PD$$

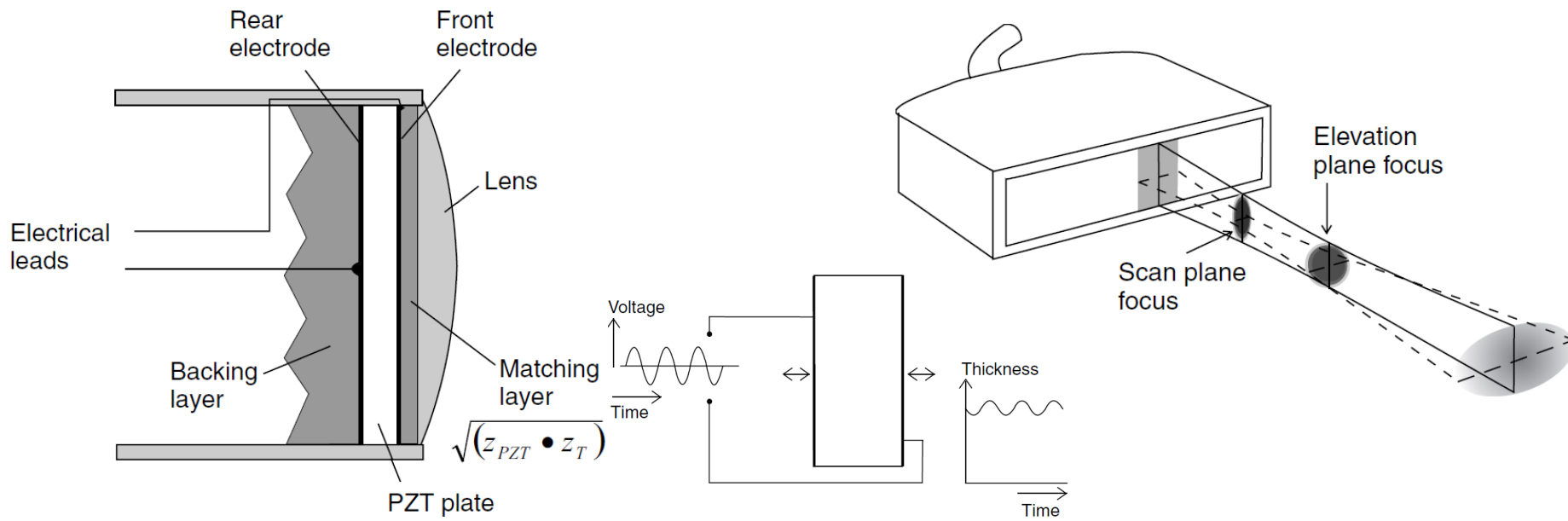
Ultrasound Physics

□ Acoustic pressure and intensities within ultrasound beam



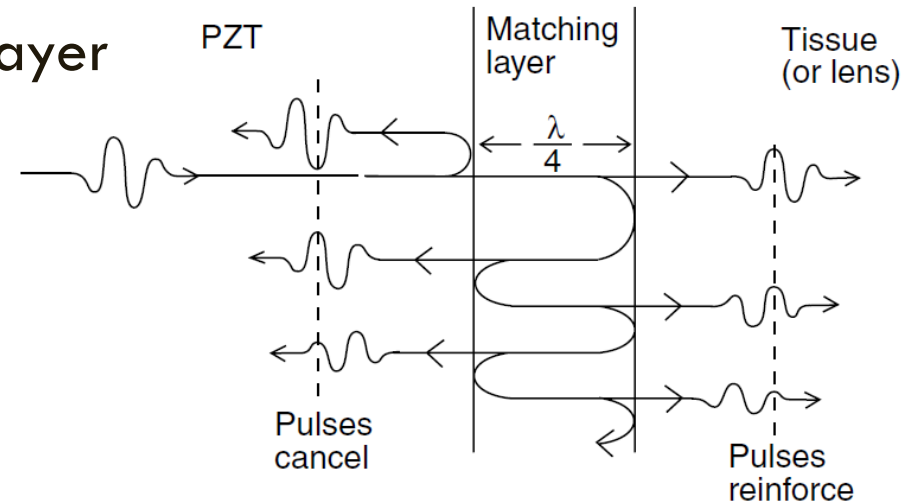
Transducers and Beamforming

- Transducer: device that actually converts electrical transmission pulses into ultrasonic pulses and, conversely, ultrasonic echo pulses into electrical echo signals
- Beamformer: part of scanner that determines the shape, size and position of the interrogating beams by controlling electrical signals to and from the transducer array elements

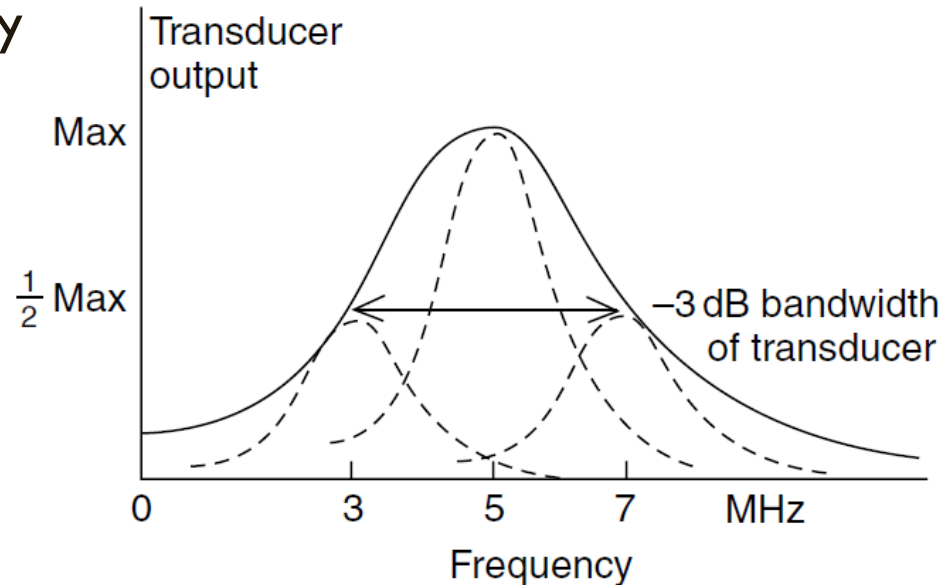


Transducers and Beamforming

□ Quarter-wavelength matching layer

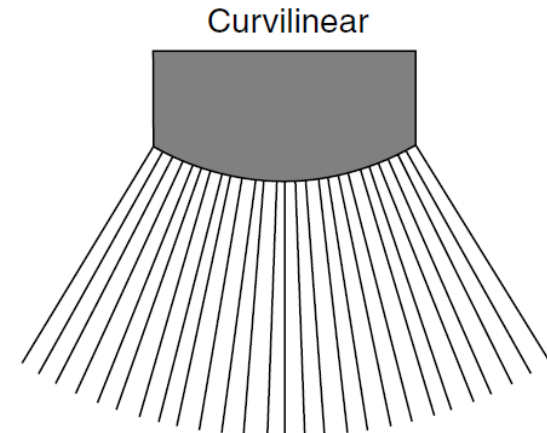
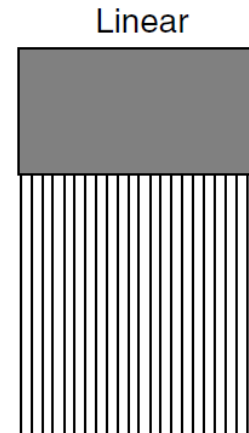
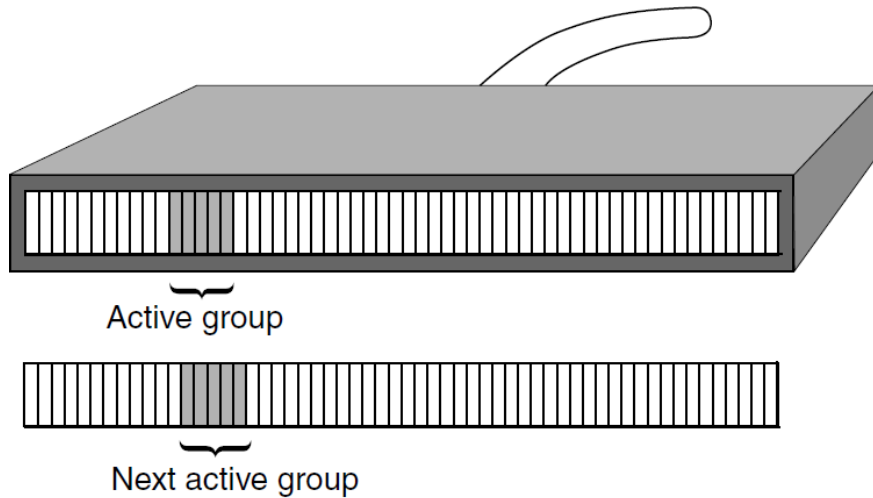
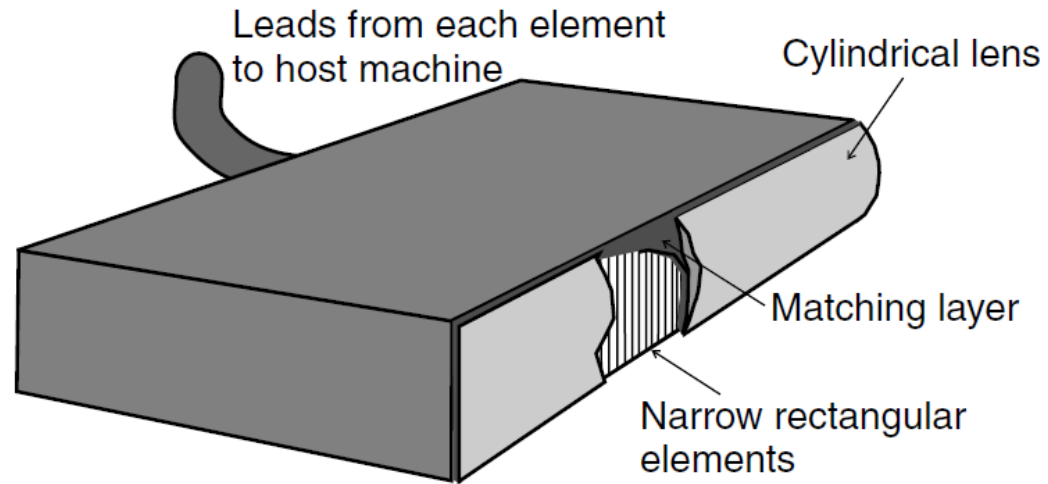
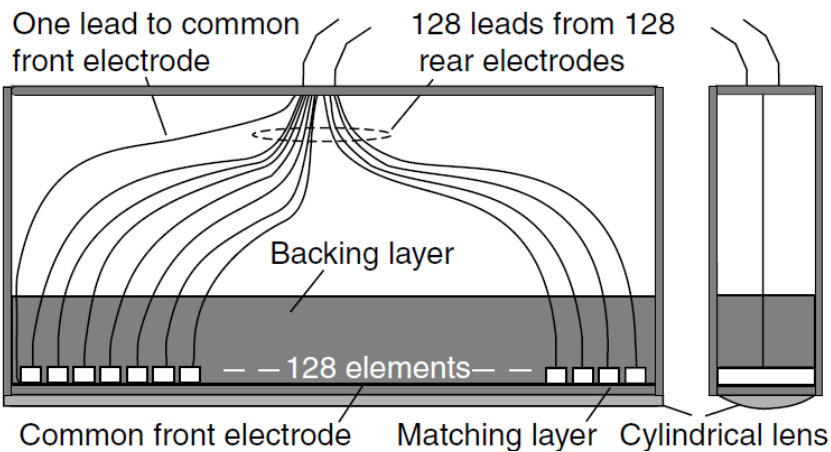


□ Bandwidth for multi-frequency transducers



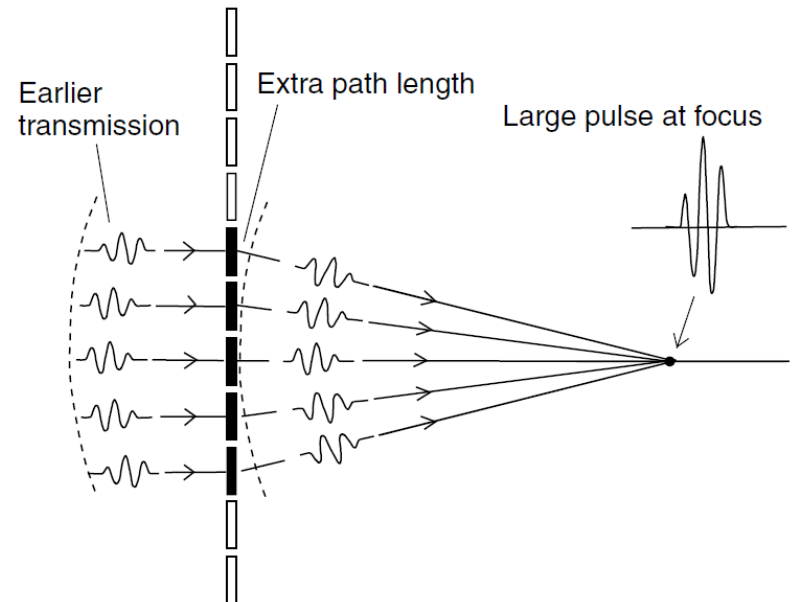
Transducers and Beamforming

Linear- and curvilinear-array transducers



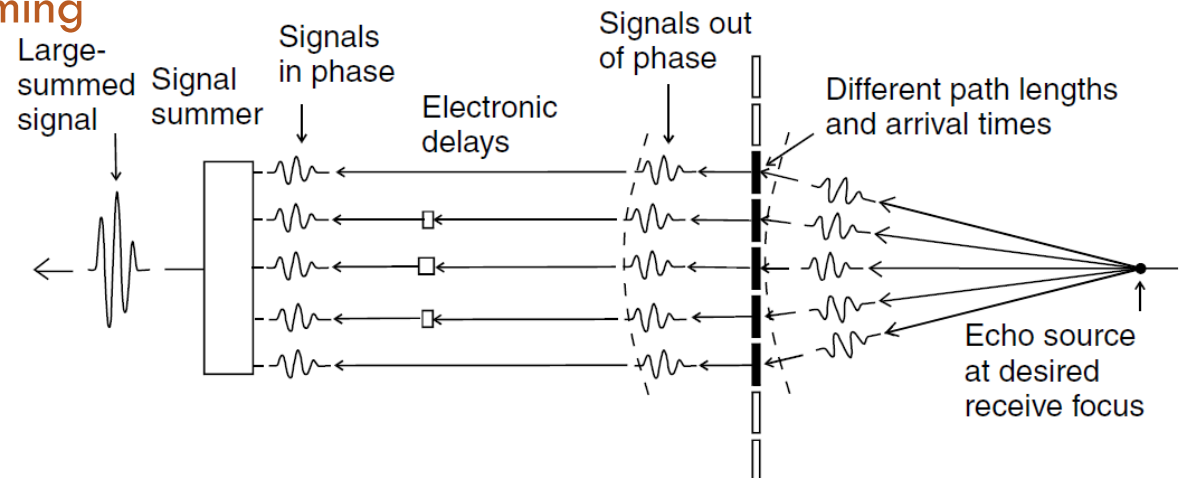
Transducers and Beamforming

□ Transmission Focusing



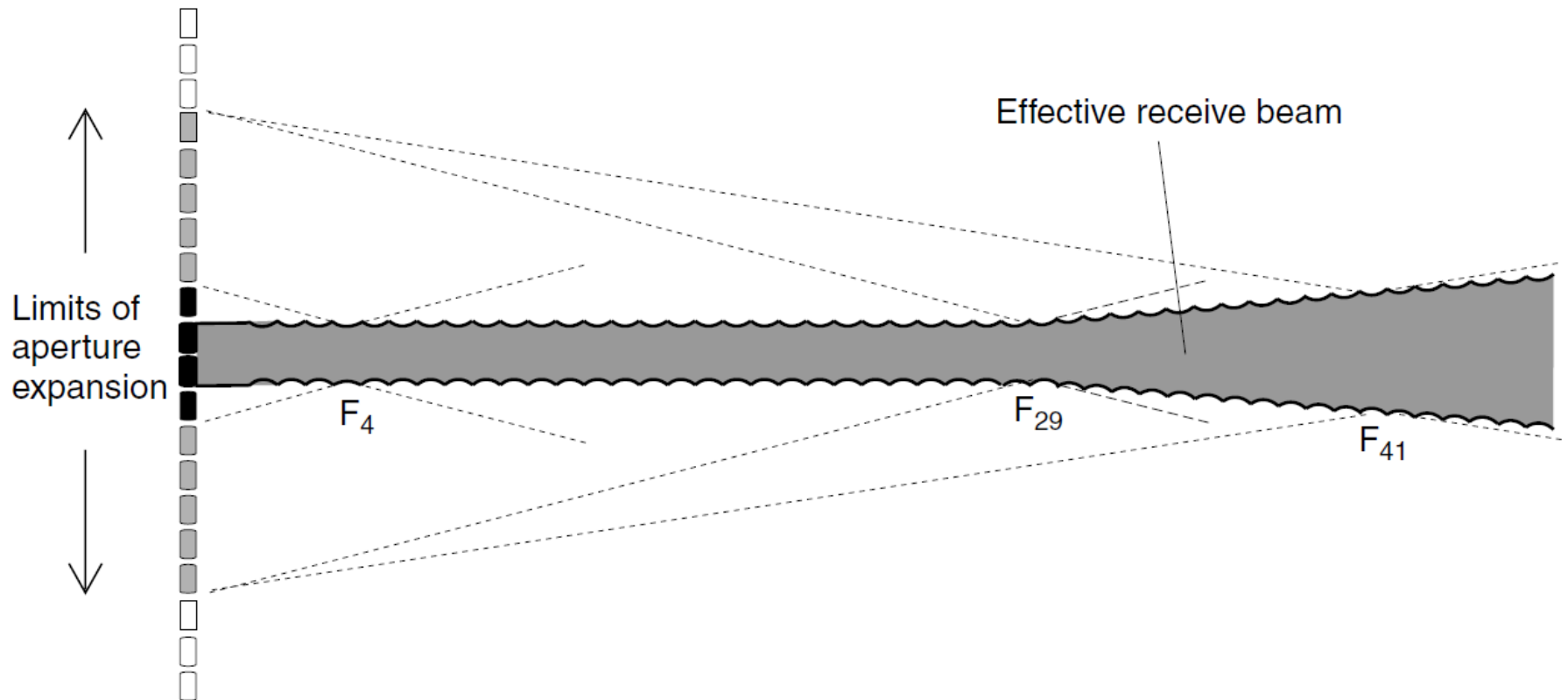
□ Reception focusing

▣ Delay-Sum beamforming



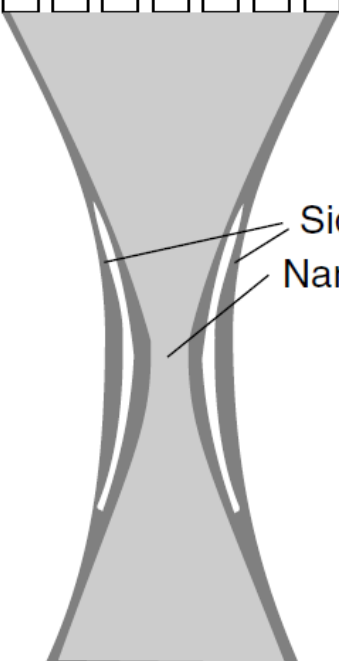
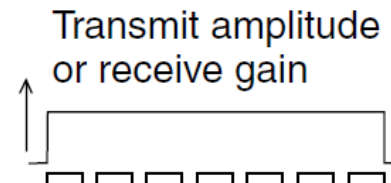
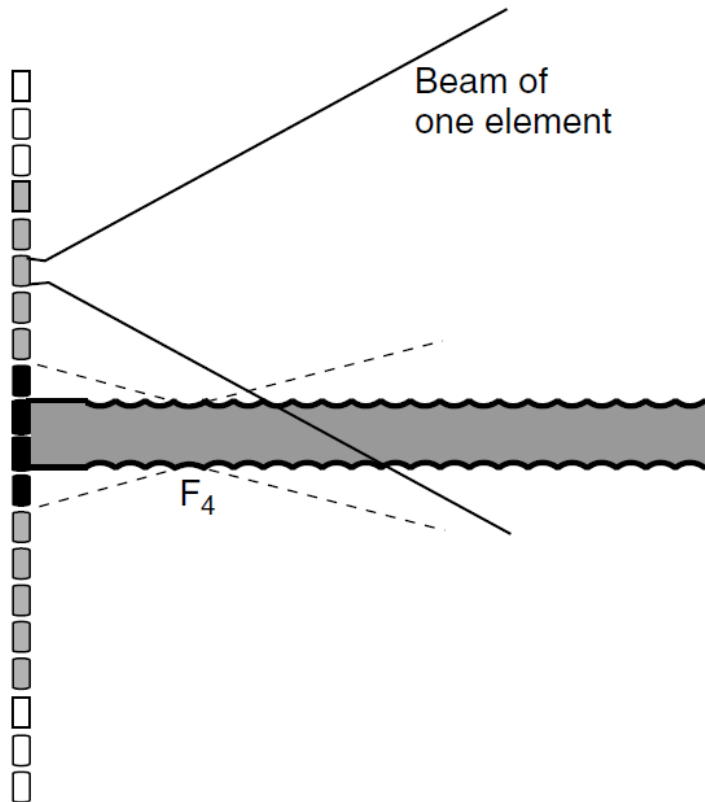
Transducers and Beamforming

- Dynamic reception focusing

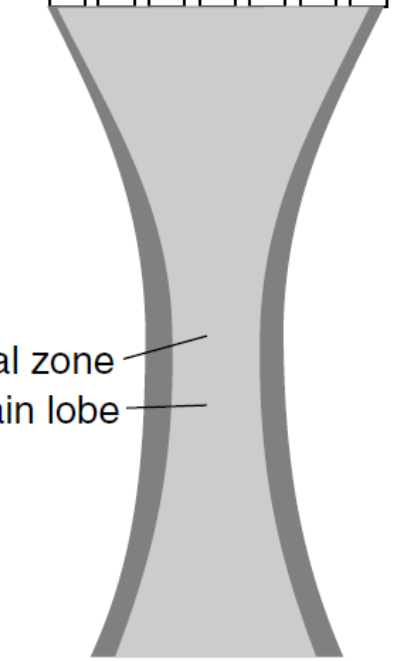
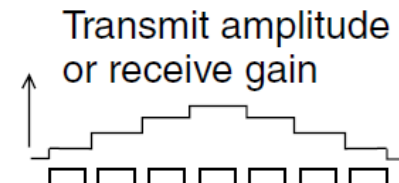


Transducers and Beamforming

- Beamforming: selecting active elements and apodization



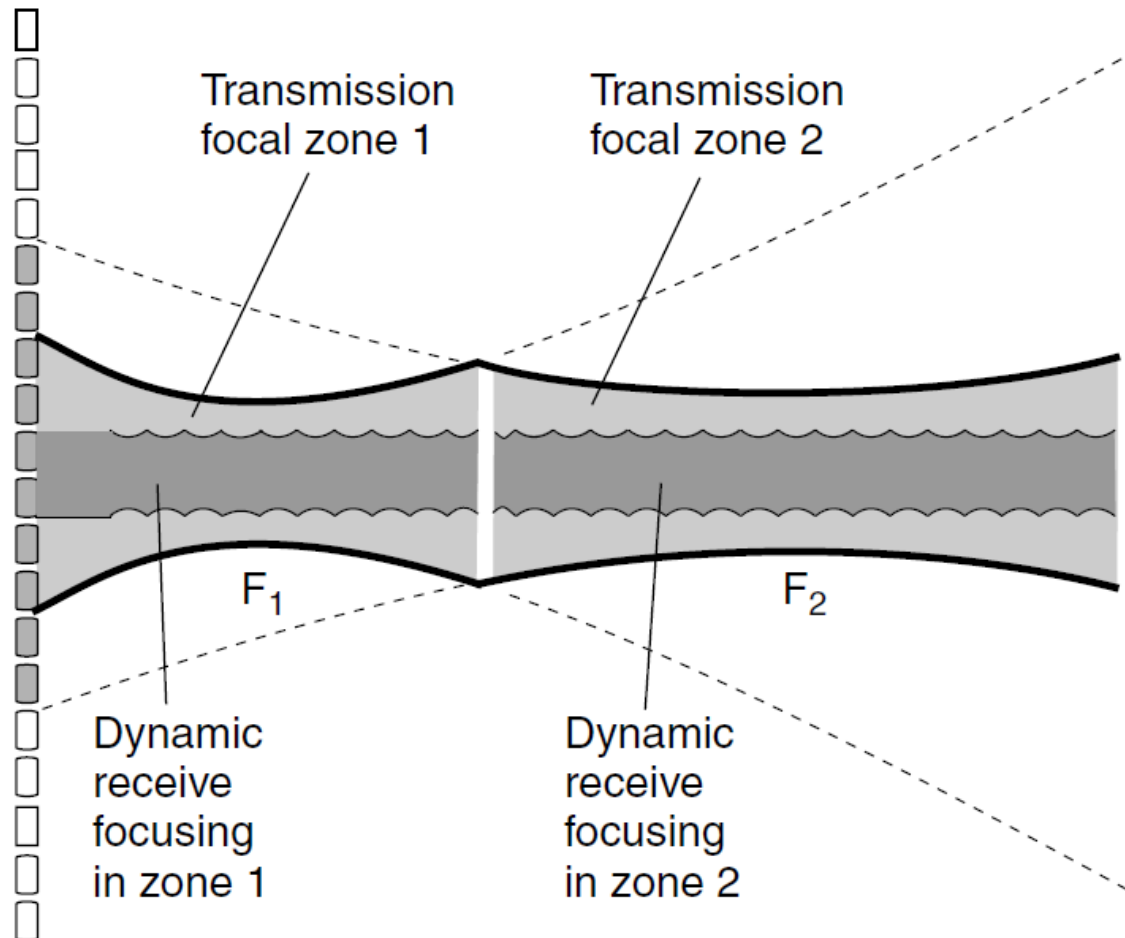
Uniform excitation



Non-uniform excitation (apodization)

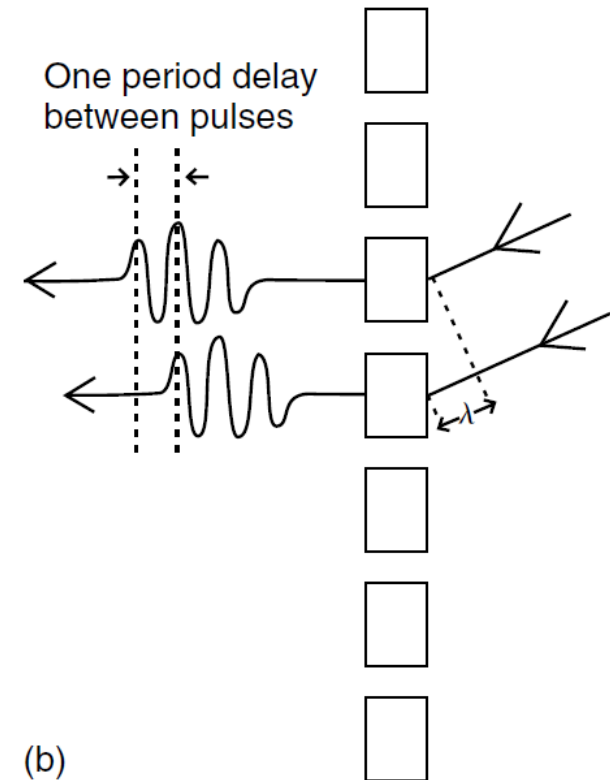
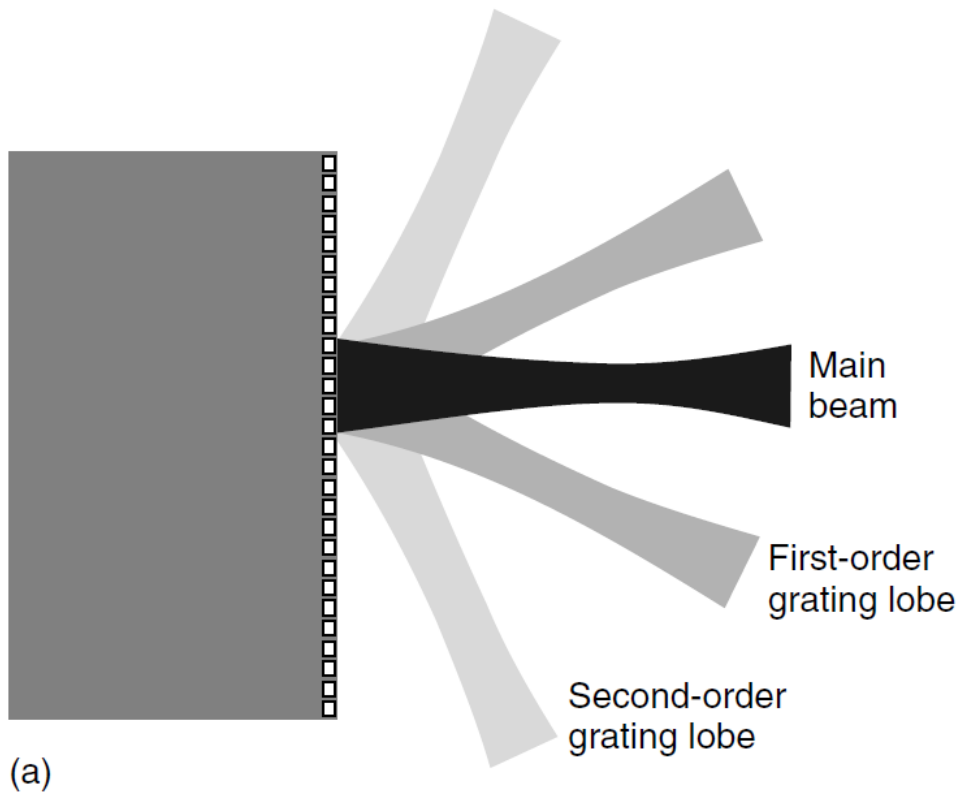
Transducers and Beamforming

- Beamforming: Multiple Transmission zones



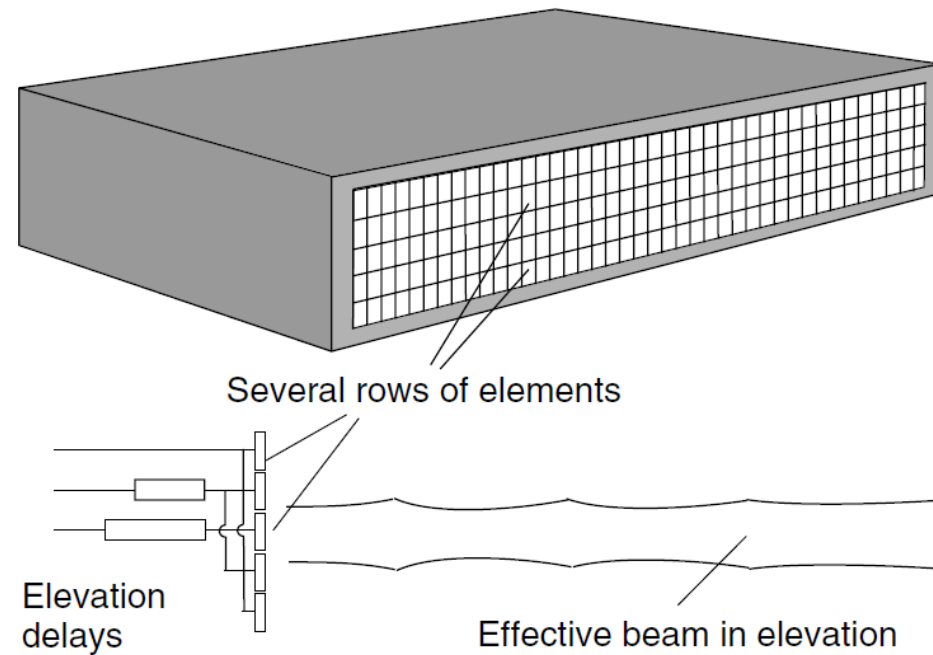
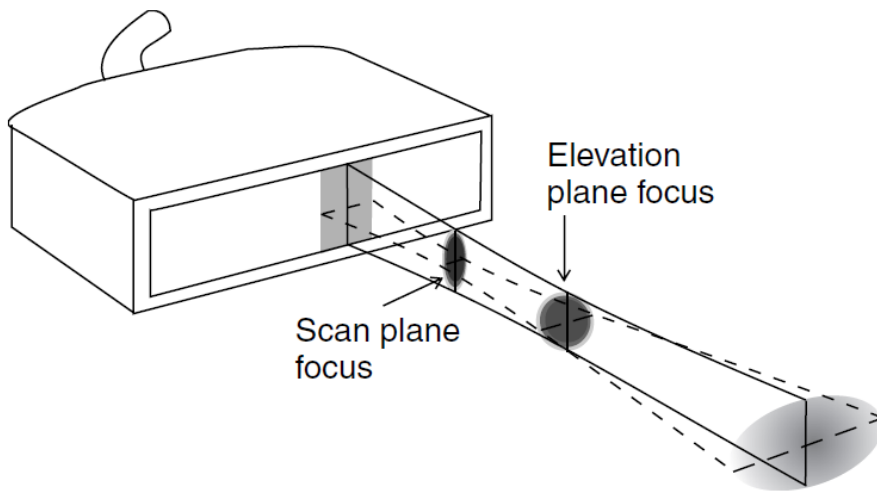
Transducers and Beamforming

- Beamforming: Grating lobes
 - ▣ No grating lobes, if the center-to-center distance between elements is half a wavelength or less



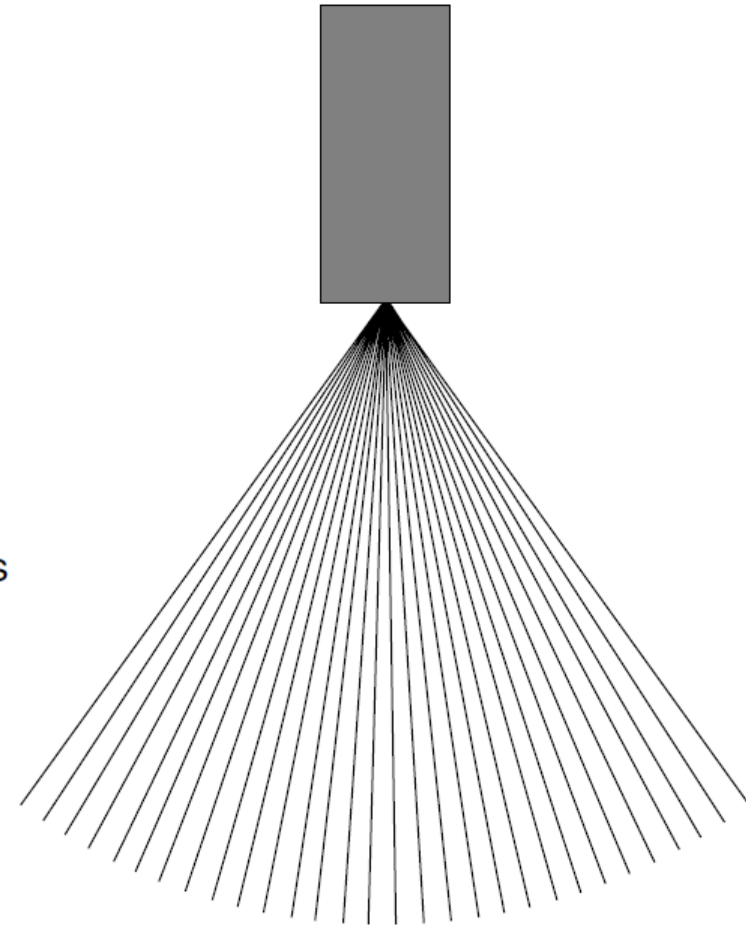
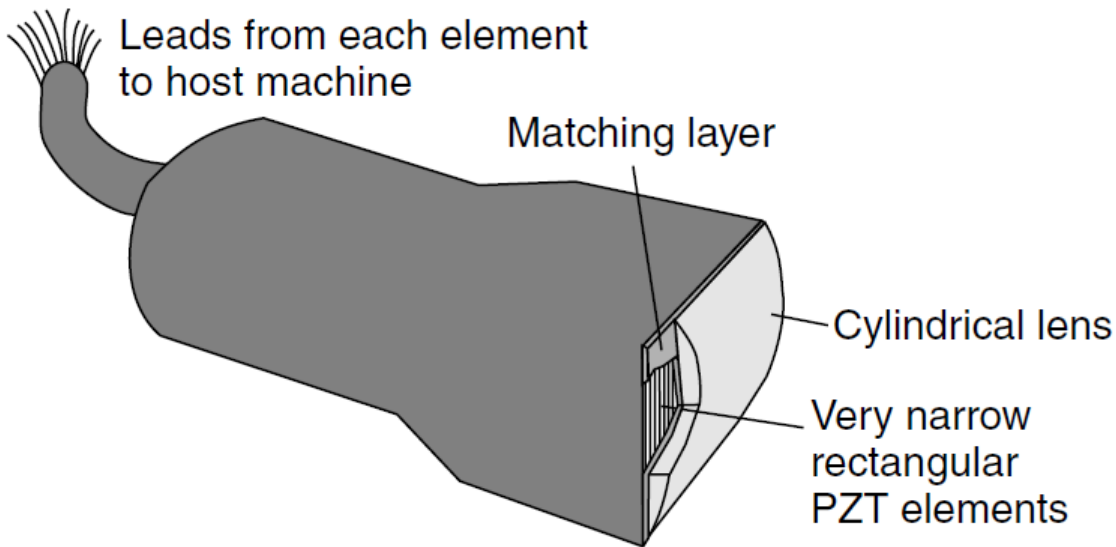
Transducers and Beamforming

- Slice thickness: elevation direction
 - ▣ 1.5D or 2D arrays



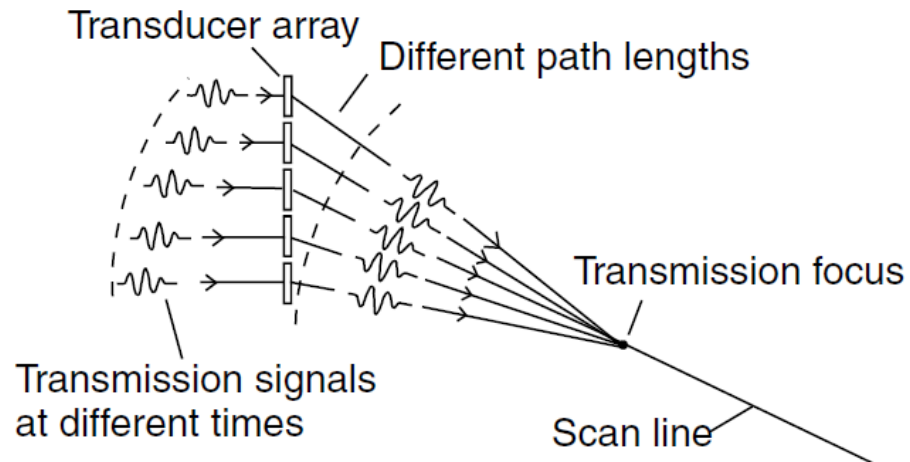
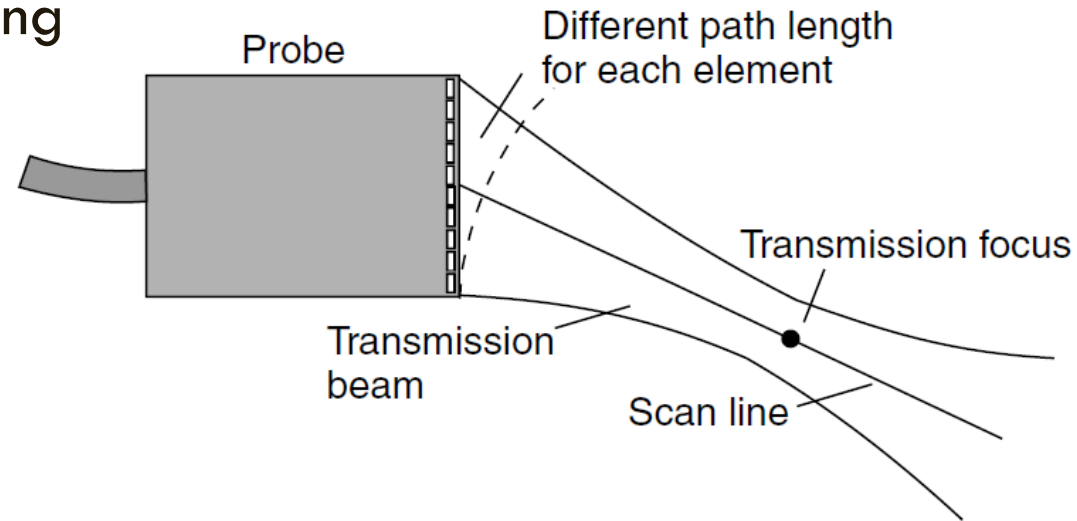
Transducers and Beamforming

□ Phased Array transducers



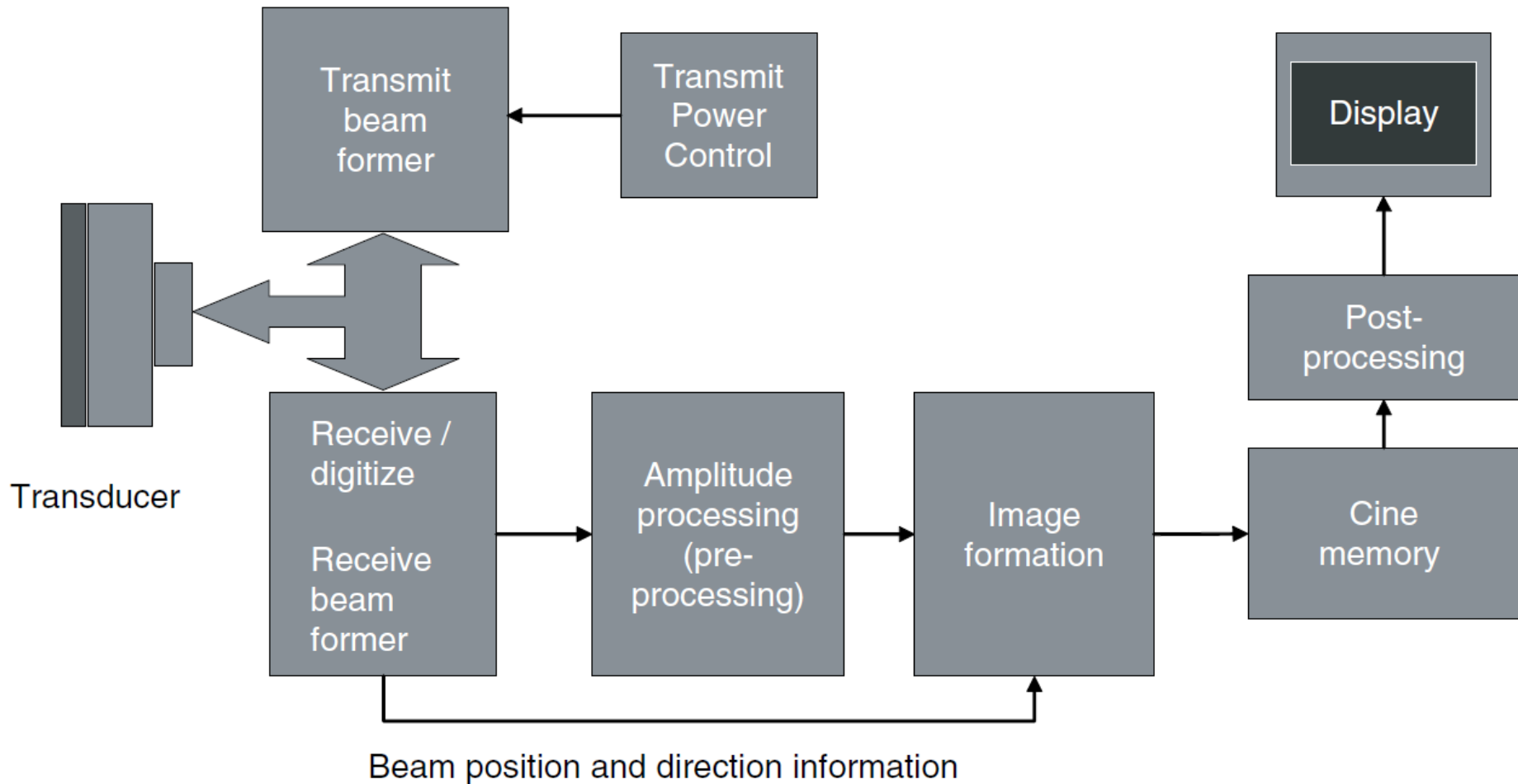
Transducers and Beamforming

□ Electronic steering/focusing



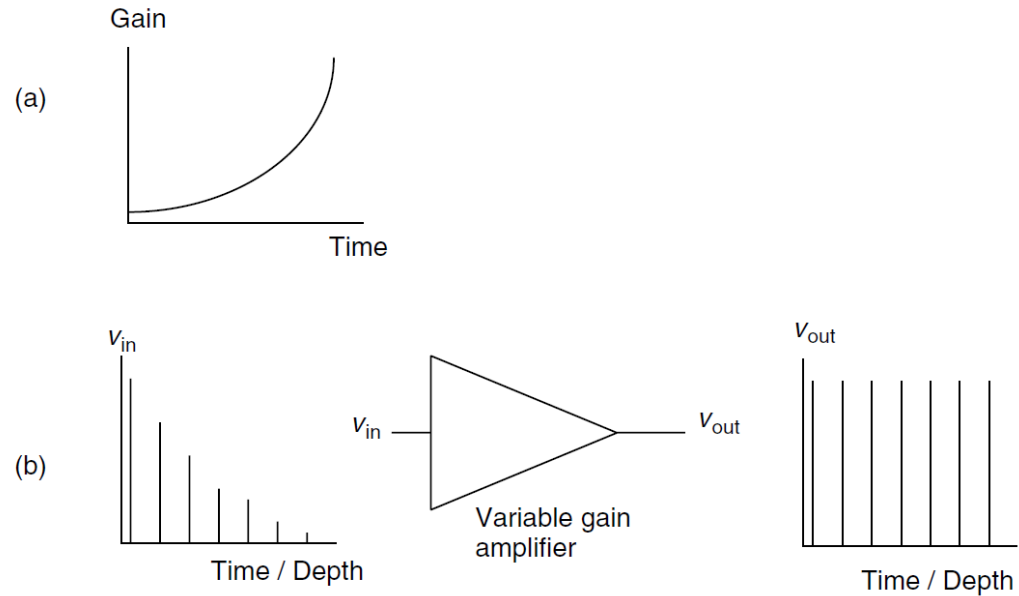
B-Mode Instrumentation

Processing block diagram



B-Mode Instrumentation

□ Time-Gain Compensation



TGC slide controls

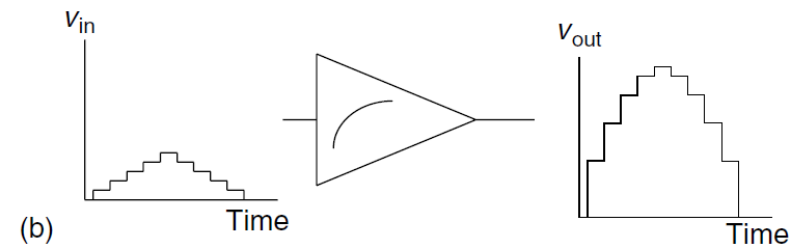
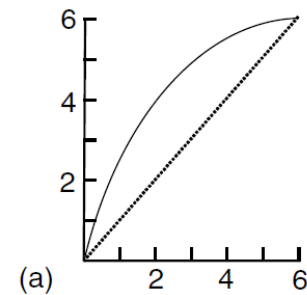
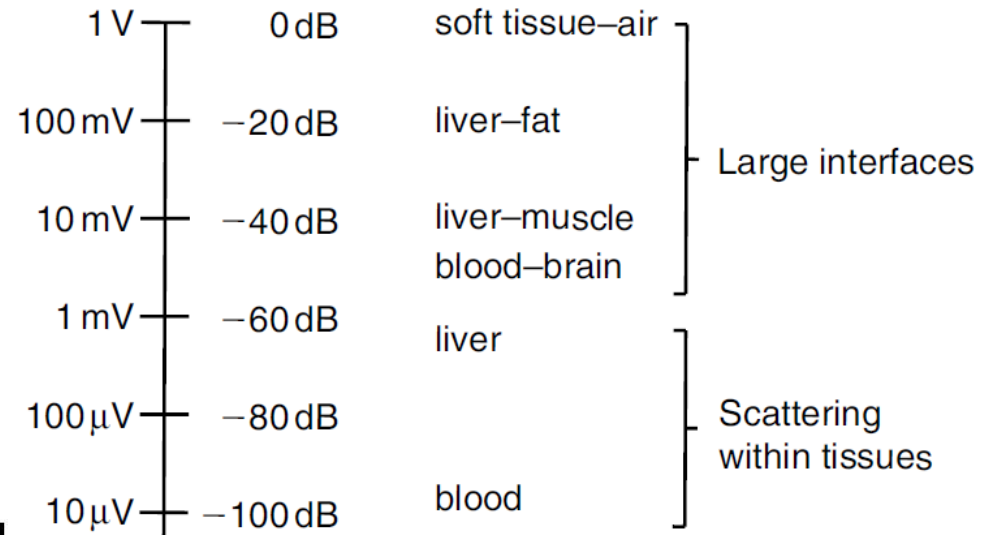
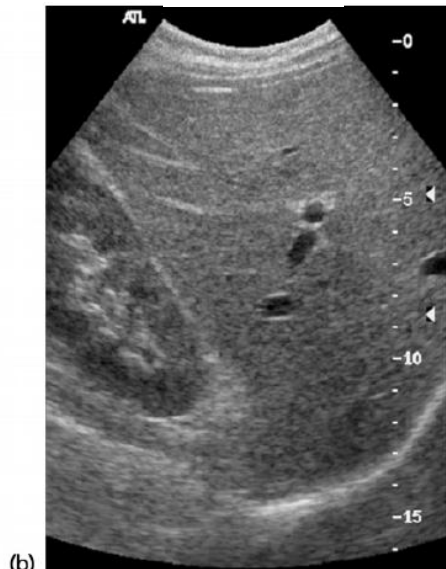
B-Mode Instrumentation

Dynamic range of echoes

Bits	Max count	DR (dB)
4	15	24
8	255	48
10	1023	60
12	4095	72

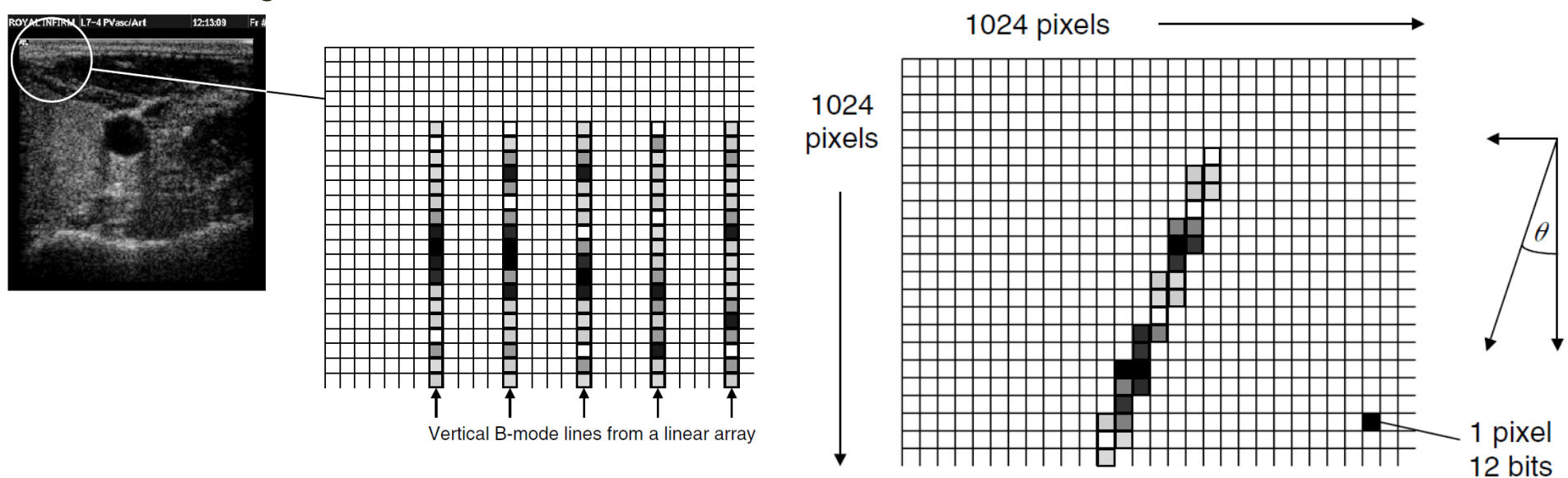
40 dB

80 dB



B-Mode Instrumentation

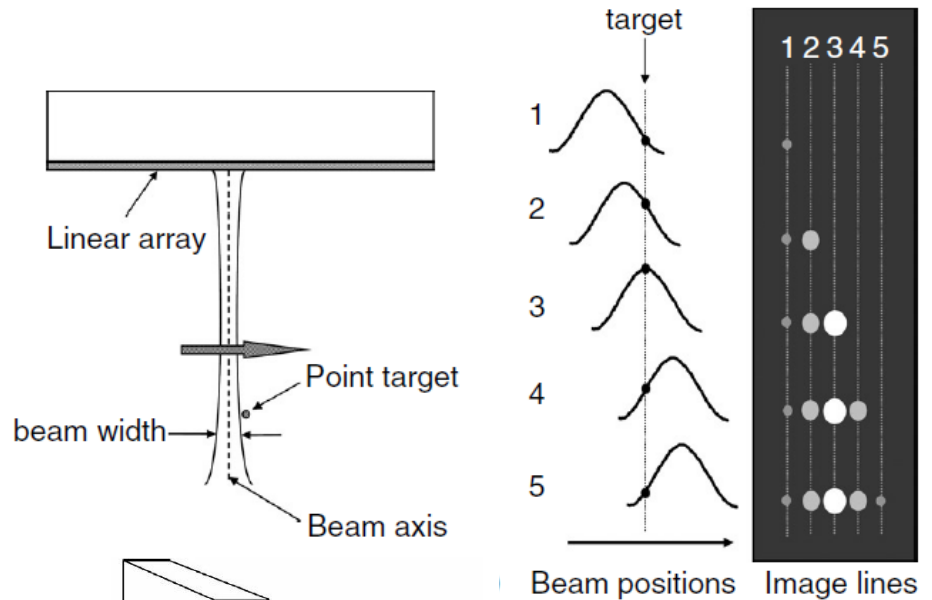
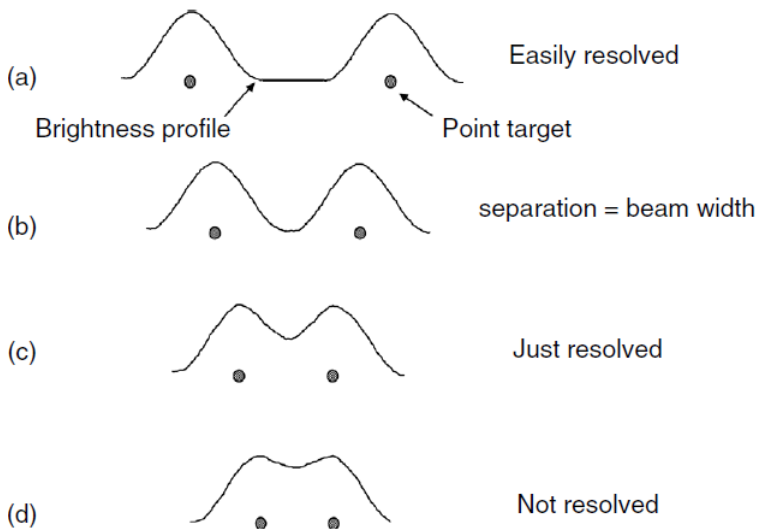
- Image reconstruction: scan conversion and interpolation



- Real-time display: frame every $1/25$ s
- Freeze: updating frame stops
- Cine Loop: recording of real-time scan as a movie
- Frame Averaging: moving average filter to improve SNR

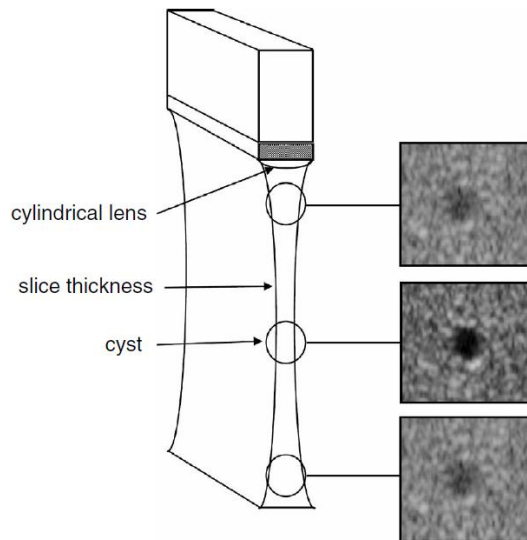
B-Mode Image Properties

□ Lateral Resolution



□ Thickness resolution

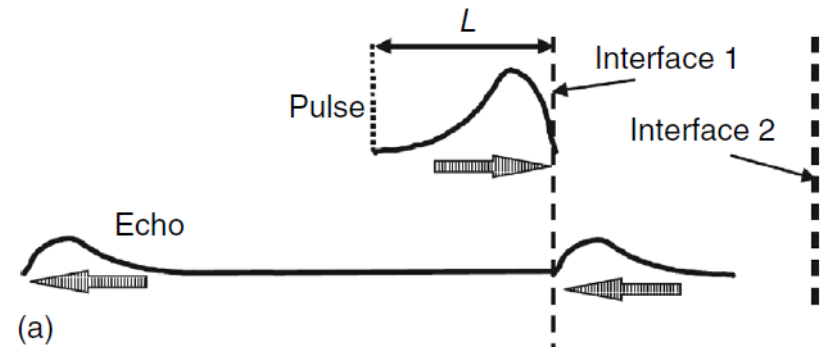
▣ Elevation



B-Mode Image Properties

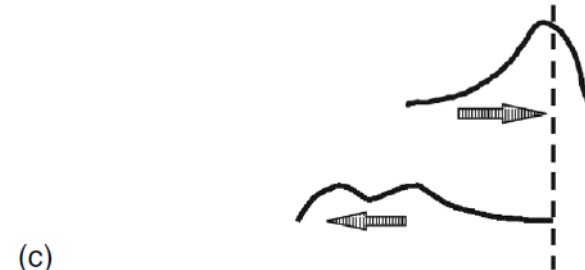
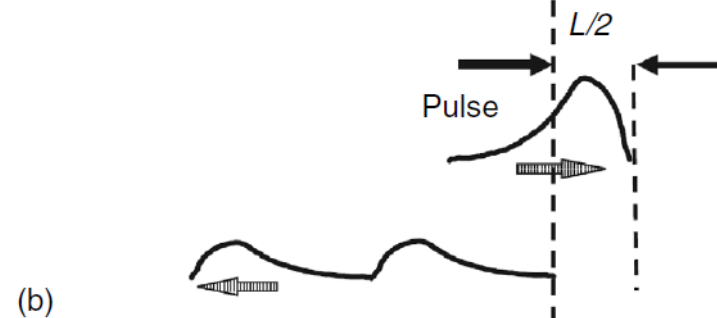
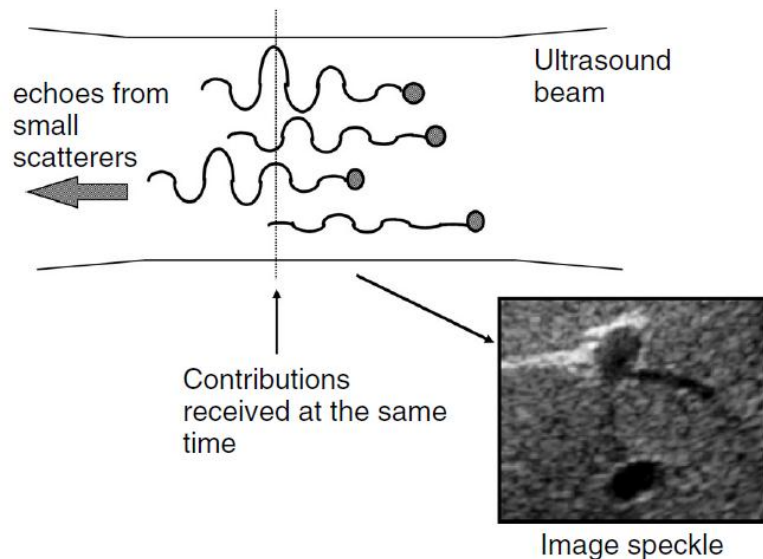
□ Axial resolution

- Half pulse length



□ Speckle

- Random yet stationary pattern

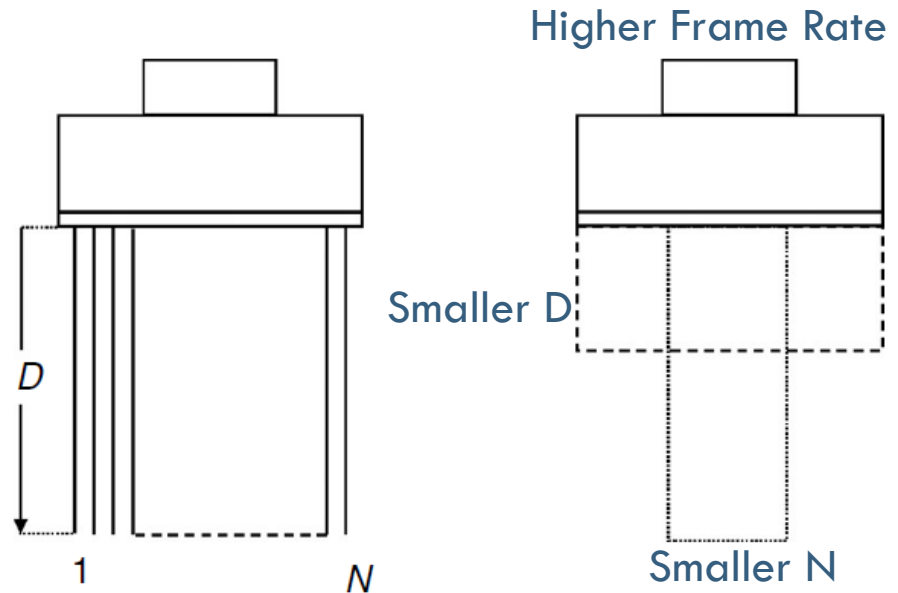


B-Mode Image Properties

- Frame time / Frame rate
 - ▣ Time to scan a complete image

$$\text{frame time} = 2DN/c$$

$$\text{frame rate} = (c/2DN)$$



- ▣ Example: time to scan 1 cm = $2 \times 1 \text{ cm} / c = 2 \text{ cm} / (1540 \text{ m/s}) = 13 \mu\text{s}$
Then, frame time to scan a 20 cm depth with 128 lines = $13 \mu\text{s} \times 20 \times 128$
Frame rate = $1 / \text{frame time} = 30 \text{ frames/s}$

Assignments

- Chapter 2: problems 3, 4, 5, 7, 10
- Chapter 3: problems 1, 2, 3, 4, 5, 6, 7, 8, 9, 10
- Chapter 4: problems 1, 2, 3, 4, 5