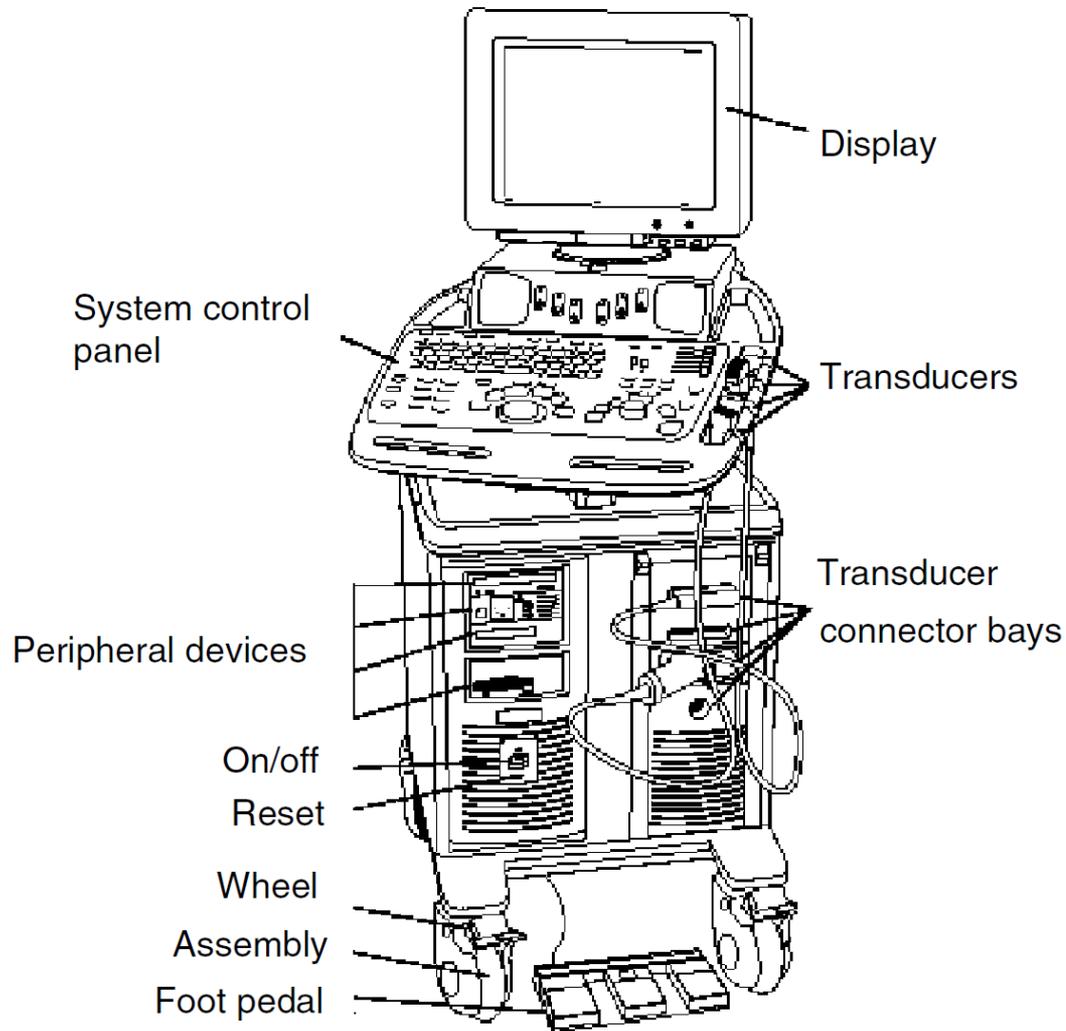




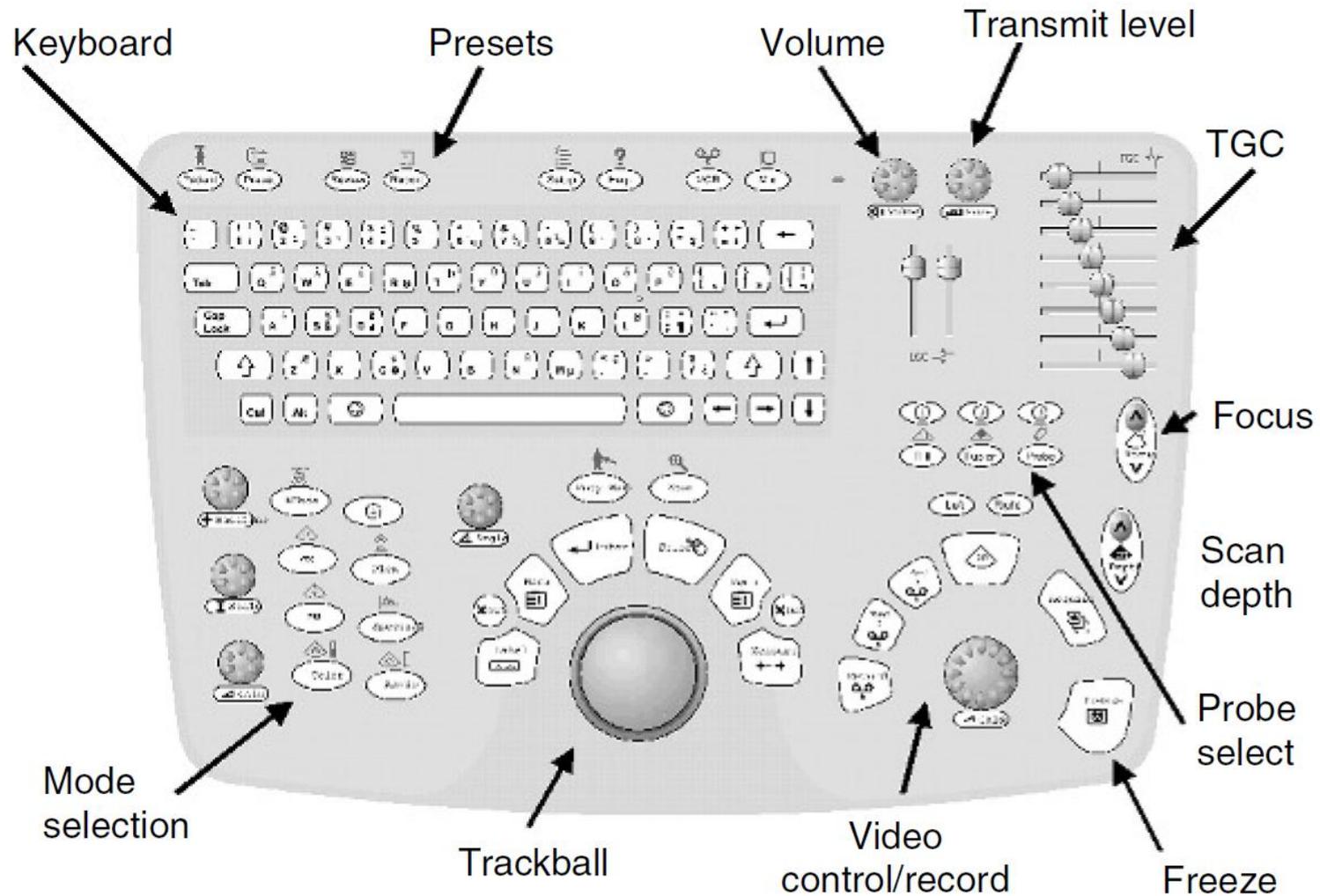
# MEDICAL EQUIPMENT (4)

## TOPIC 1: ULTRASOUND IMAGING

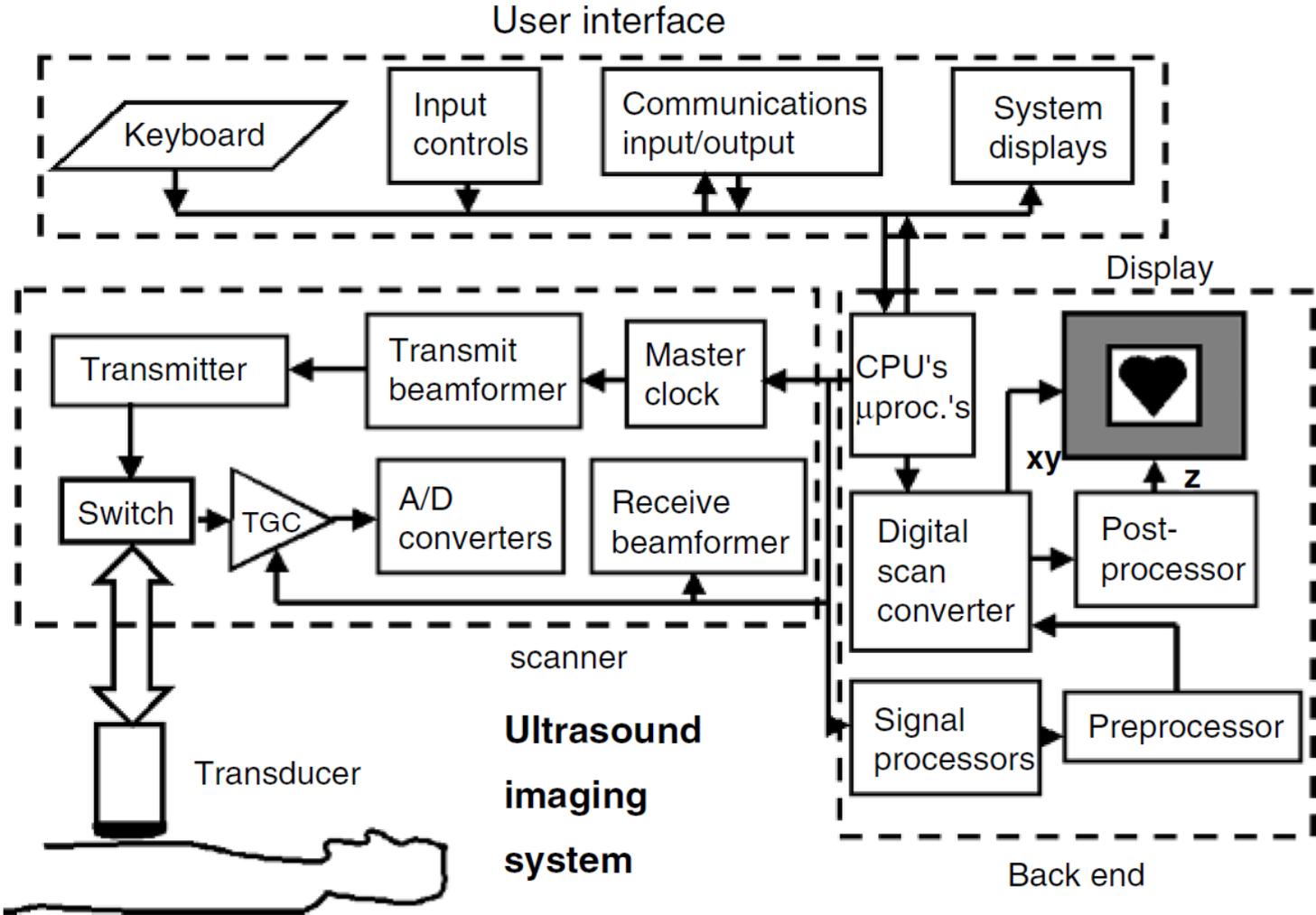
# Ultrasound Imaging System: External Look



# Keyboard Controls



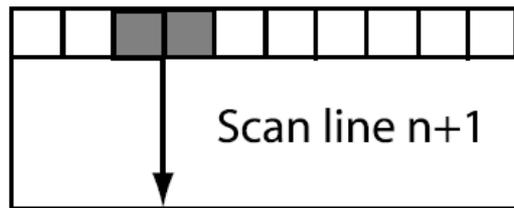
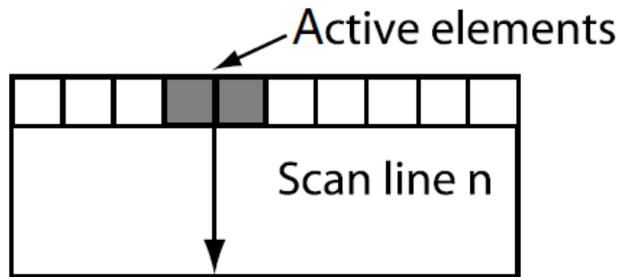
# Block Diagram



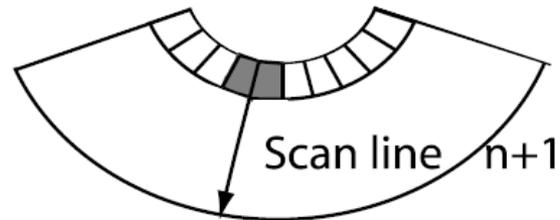
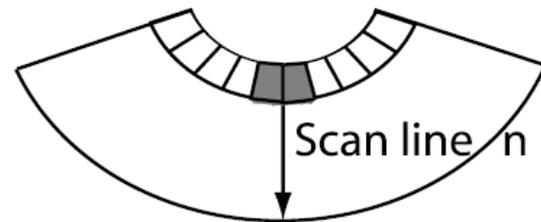
# Ultrasound Transducers



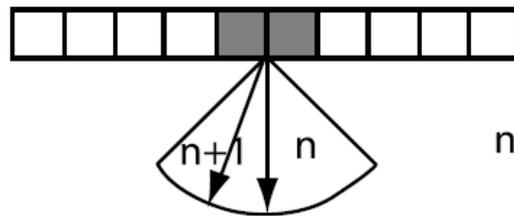
# Image Formats



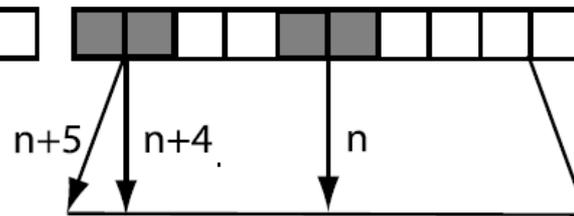
A Linear (translation)



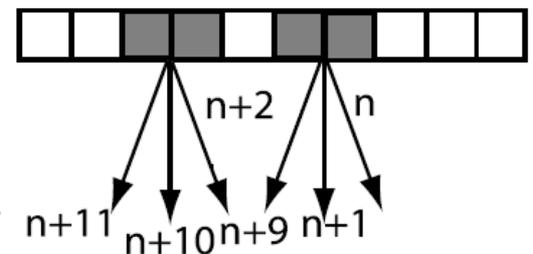
B Convex (translation)



C Sector (rotation)



D Trapezoidal (contiguous)



E Compound

# Major Modes:

## B-Mode (2D Mode)

- Brightness-modulated image in which depth is along the z axis and azimuth is along the x axis.
  - The position of the echo is determined by its acoustic transit time and beam direction in the plane.



# Major Modes:

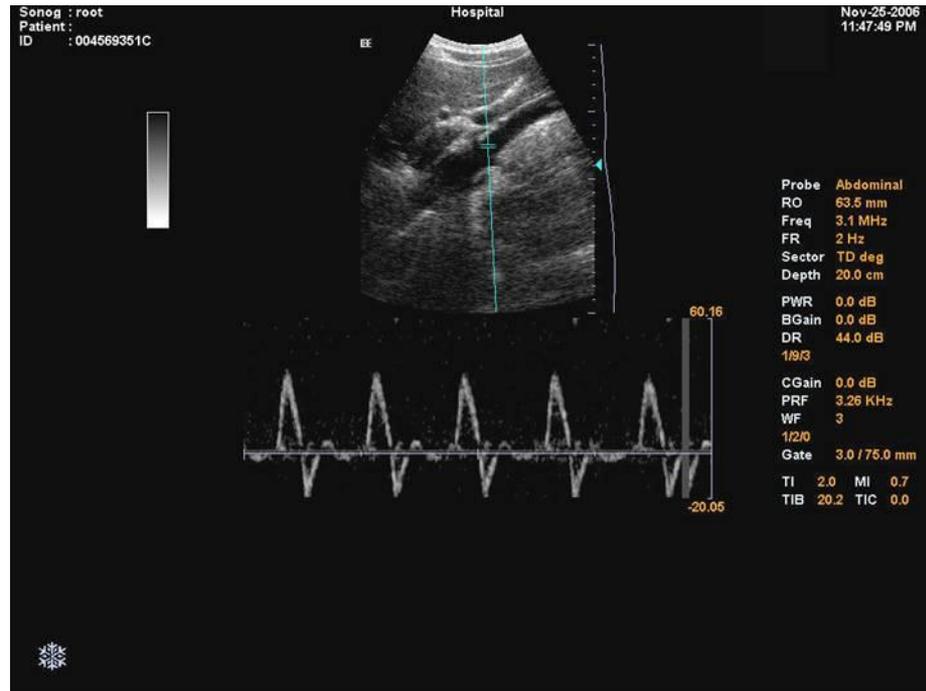
## M-Mode

- Brightness modulated, where depth is the y deflection (fast time), and the x deflection is the same imaging line shown as a function of slow time.
  - ▣ Time history of single line at the same position over time



# Major Modes: Doppler-Mode

- This is the presentation of the Doppler spectrum
  - ▣ Continuous wave (CW) Doppler
  - ▣ Pulsed wave (PW) Doppler



# Major Modes:

## Color Flow Mapping Mode (CFM)

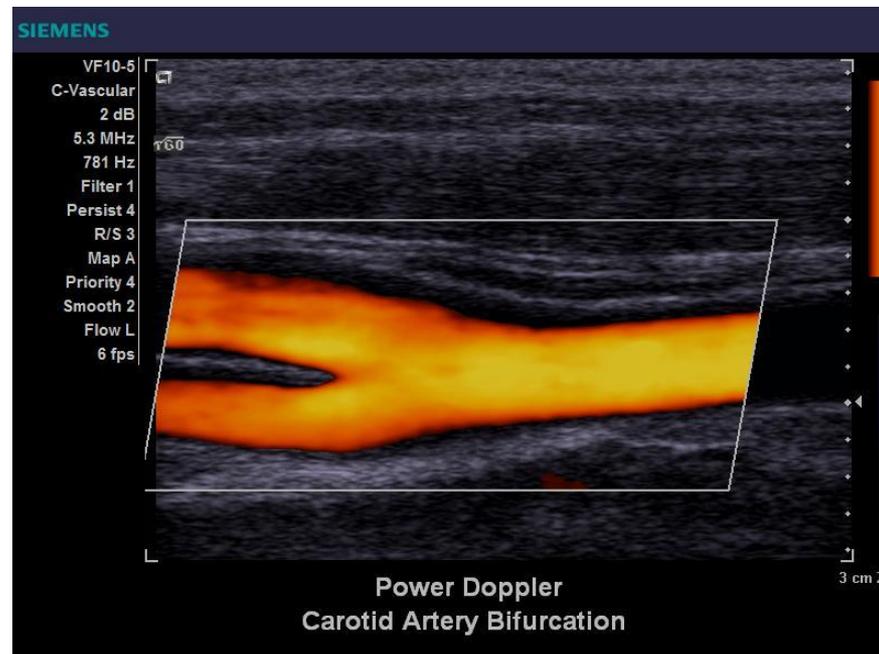
- Spatial map overlaid on a B-mode gray-scale image that depicts an estimate of blood flow mean velocity
  - Direction of flow encoded in colors (blue away from the transducer and red toward it)
  - Amplitude of mean velocity by brightness, and turbulence by a third color (often green).



# Major Modes:

## Power Doppler Mode

- This color-coded image of blood flow is based on intensity rather than on direction of flow, with a paler color representing higher intensity.
  - ▣ It is also known as “angio”



# Secondary Modes

- Duplex
  - ▣ Presentation of two modes simultaneously: usually 2D and pulsed (wave) Doppler
- Triplex
  - ▣ Presentation of three modes simultaneously: usually 2D, color flow, and pulsed Doppler
- 3D
  - ▣ Display or Surface/volume rendering used to visualize volume composed of multiple 2D slices.
- 4D
  - ▣ A 3D image moving in time

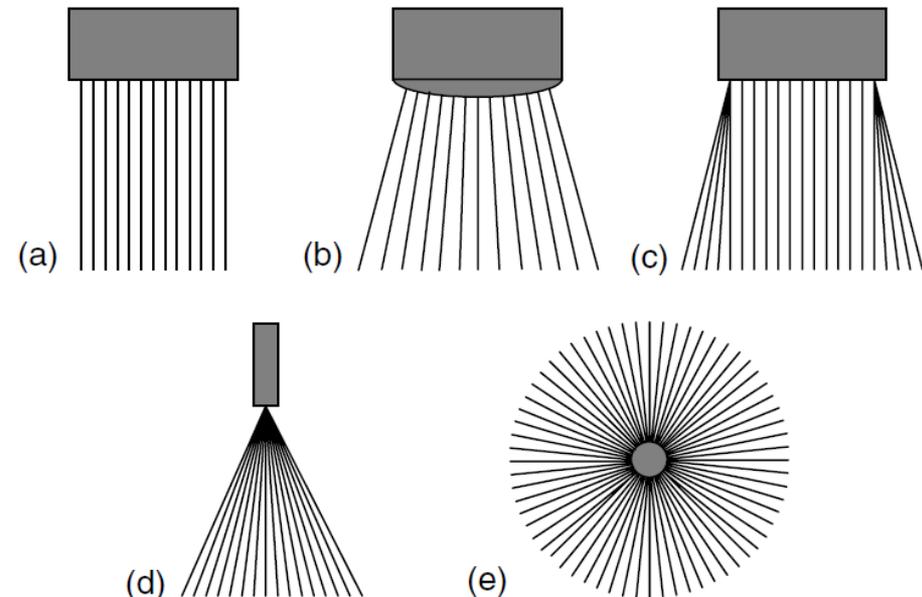
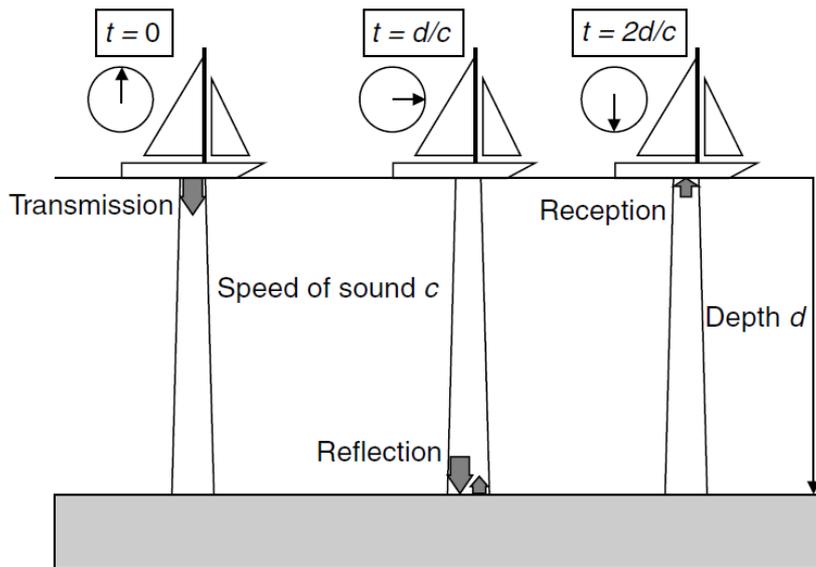
# Introduction to B-mode imaging

- B-mode image is an anatomic cross-sectional image
- Constructed from echoes (reflection and scattering) of waves
- Echo is displayed at a point in image, which corresponds to relative position of its origin within the body cross section
- Brightness of image at each point is related to strength of echo
  - ▣ Term B-mode stands for Brightness-mode



# Echo Ranging

- To display each echo in a position corresponding to that of the interface or feature (known as a target) that caused it, the B-mode system needs two pieces of information:
  - ▣ (1) Range (distance) of the target from the transducer
  - ▣ (2) Position and orientation of the ultrasound beam



# Ultrasound Physics

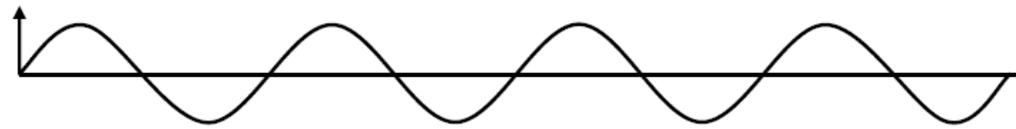
- Sound waves used to form medical images are longitudinal waves, which propagate (travel) only through a physical medium (usually tissue or liquid)
  - ▣ Characterized by frequency, wavelength, speed and phase

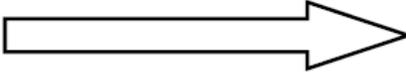
$$c = f\lambda$$

$$\text{Speed of sound } c = \sqrt{\frac{k}{\rho}}$$

Material	$c$ (m s <sup>-1</sup> )
Liver	1578
Kidney	1560
Amniotic fluid	1534
Fat	1430
Average tissue	1540
Water	1480
Bone	3190–3406
Air	333

Pressure



Direction of propagation 



Particle displacement

# Ultrasound Physics

- Medical ultrasound frequencies used in the range 2–15 MHz
  - Higher frequencies are now utilized for special applications
  - Resolution proportional to wavelength

$f$ (MHz)	$\lambda$ (mm)
2	0.77
5	0.31
10	0.15
15	0.1

- Acoustic impedance

- $p$  is the local pressure  $z = p/v$  the local particle velocity.
- Analogous to electrical impedance (or resistance  $R$ )

$$z = \sqrt{\rho k} = \rho c$$

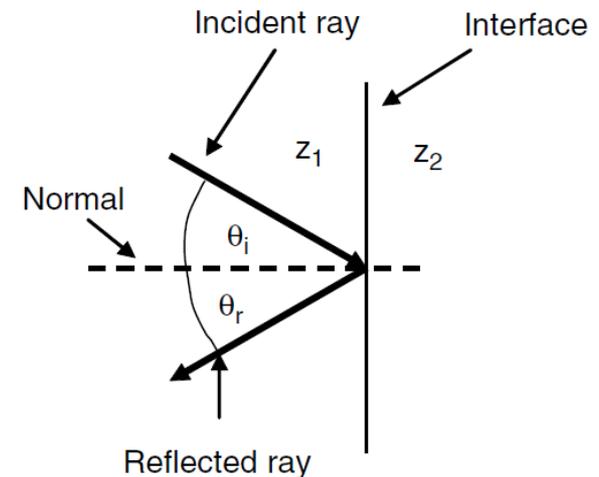
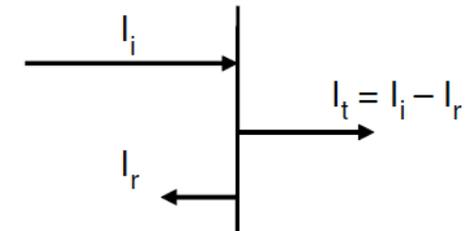
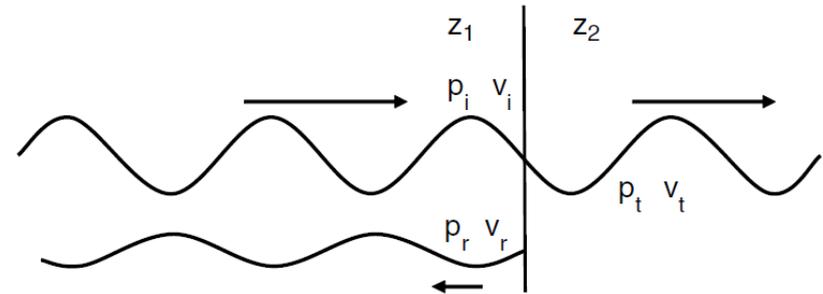
Material	$z$ ( $\text{kg m}^{-2} \text{s}^{-1}$ )
Liver	$1.66 \times 10^6$
Kidney	$1.64 \times 10^6$
Blood	$1.67 \times 10^6$
Fat	$1.33 \times 10^6$
Water	$1.48 \times 10^6$
Air	430
Bone	$6.47 \times 10^6$

# Ultrasound Physics

## □ Reflection: Large Interfaces

$$R_A = \frac{p_r}{p_i} = \frac{z_2 - z_1}{z_2 + z_1}$$

$$\frac{I_r}{I_i} = R_i = R_A^2$$



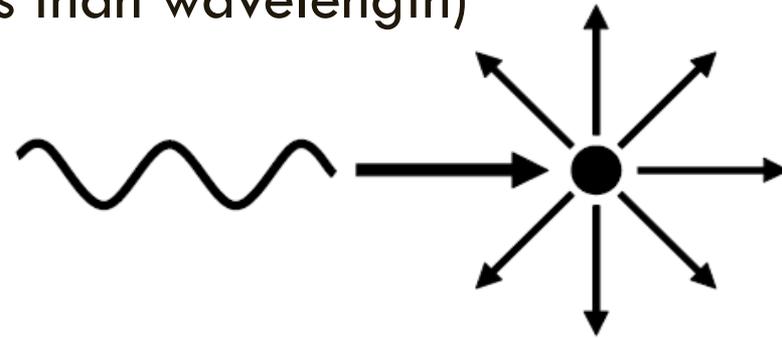
$$\theta_r = \theta_i$$

Interface	$R_A$
Liver-kidney	0.006
Kidney-spleen	0.003
Blood-kidney	0.009
Liver-fat	0.11
Liver-bone	0.59
Liver-air	0.9995

# Ultrasound Physics

- Scattering: **Small Interfaces** (size less than wavelength)

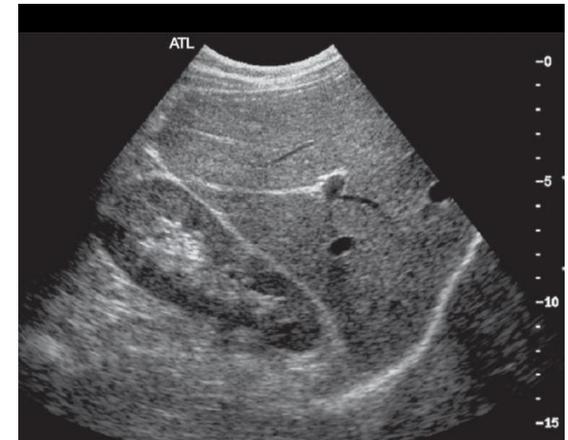
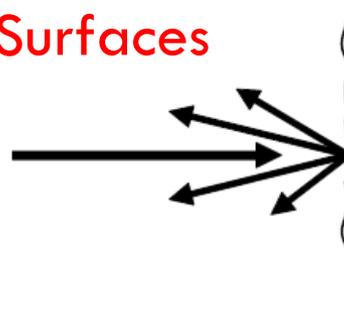
$$W_s \propto \frac{d^6}{\lambda^4} \propto d^6 f^4$$



- Two important aspects of scattering:

- ▣ Ultrasonic power scattered back is small compared to reflections
- ▣ Beam angle-independent appearance in the image unlike reflections

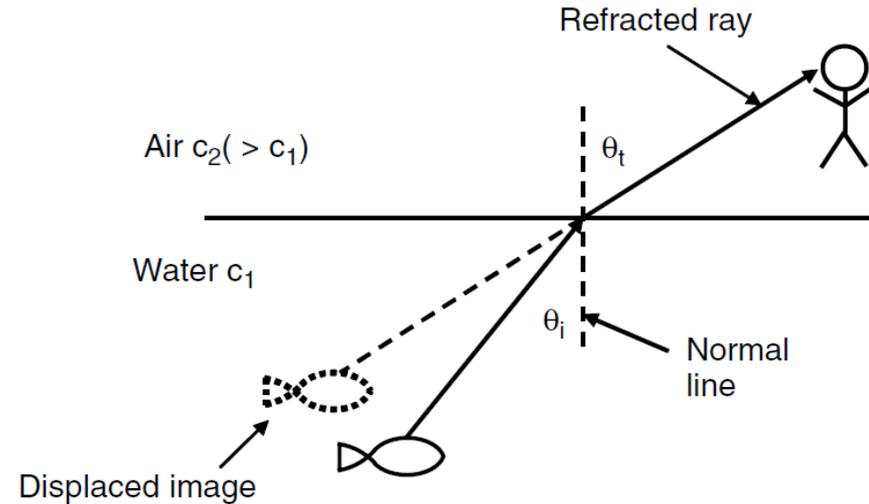
- Diffuse Reflection: **Rough Surfaces**



# Ultrasound Physics

## □ Refraction: Snell's law

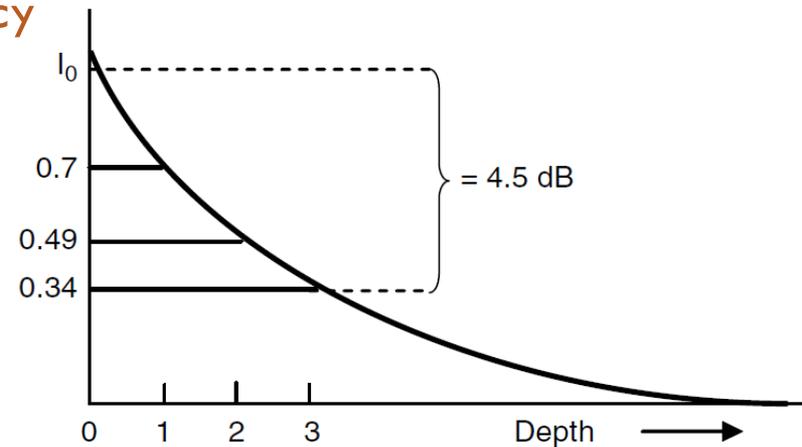
$$\frac{\sin \theta_i}{\sin \theta_t} = \frac{c_1}{c_2}$$



## □ Attenuation: gradual loss of beam energy

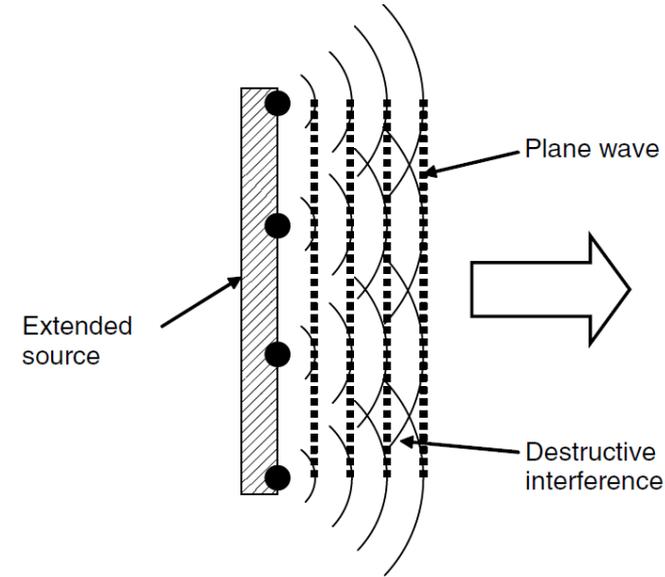
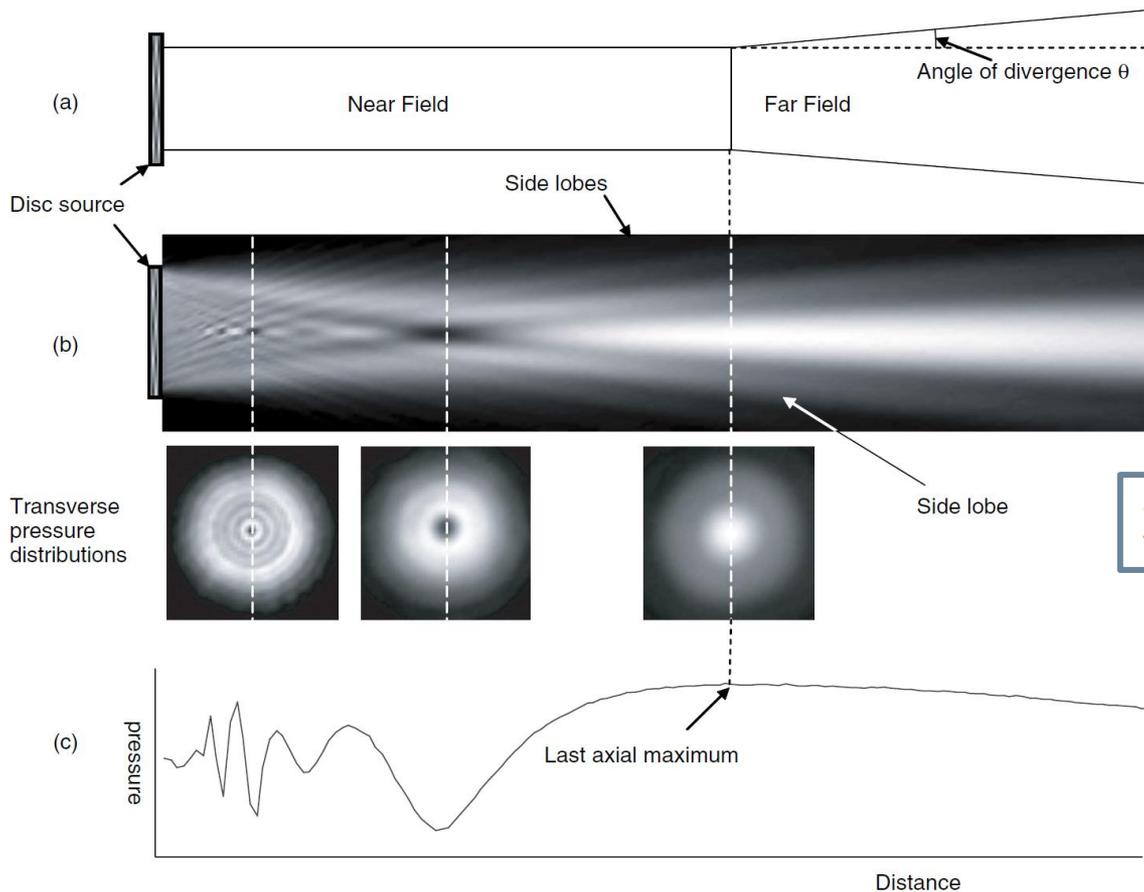
### ▣ Depends on both distance and frequency

Tissue	Attenuation (dB cm <sup>-1</sup> MHz <sup>-1</sup> )
Liver	0.399
Brain	0.435
Muscle	0.57
Blood	0.15
Water	0.02
Bone	22



# Ultrasound Physics

- Interference and diffraction
  - ▣ Constructive/Destructive interference

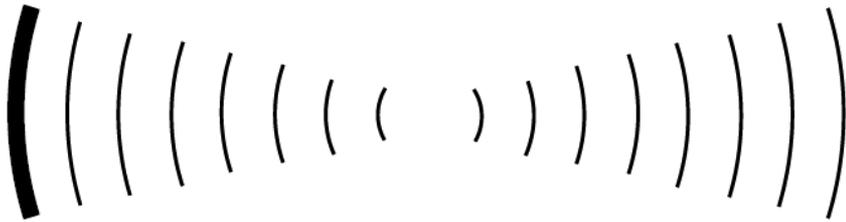


$$\text{near field length} = a^2/\lambda$$

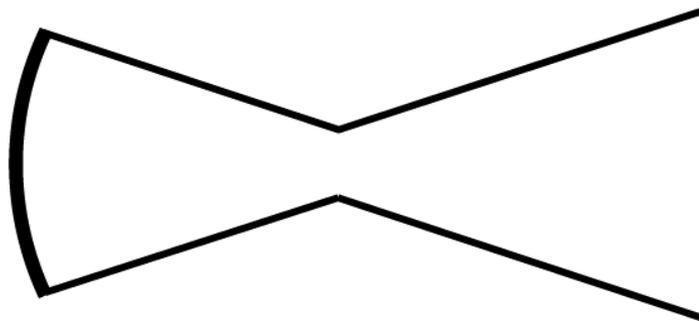
$$\sin \theta = 0.61 (\lambda/a)$$

# Ultrasound Physics

## □ Focusing: narrower ultrasound beam



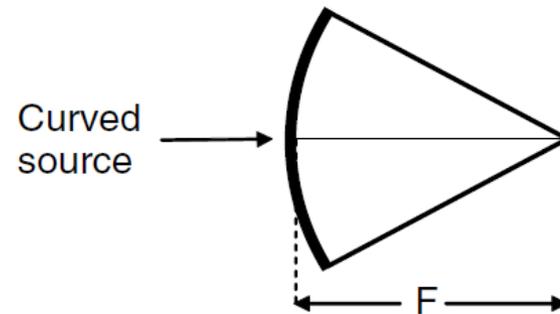
(a)



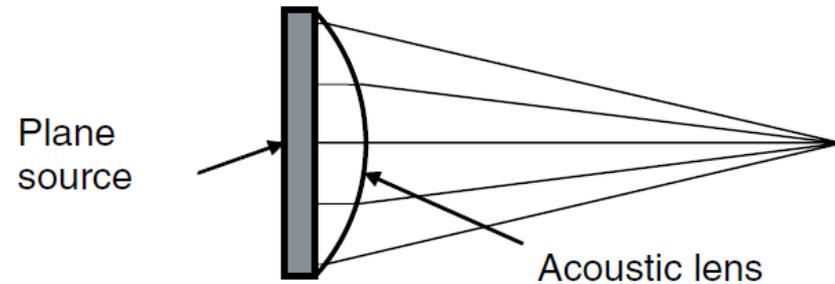
(b)



(c)



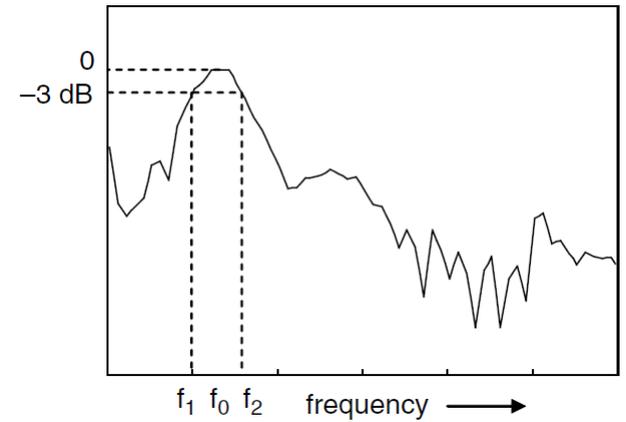
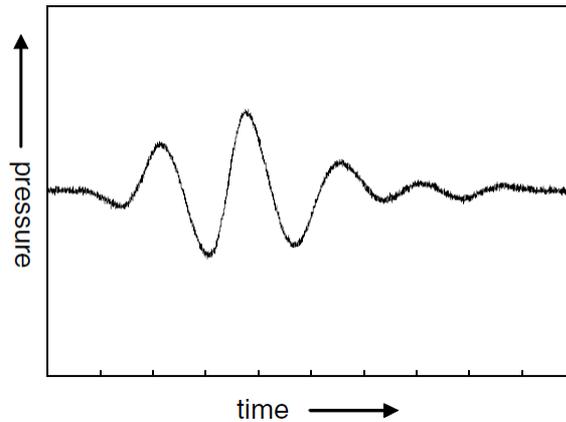
(a)



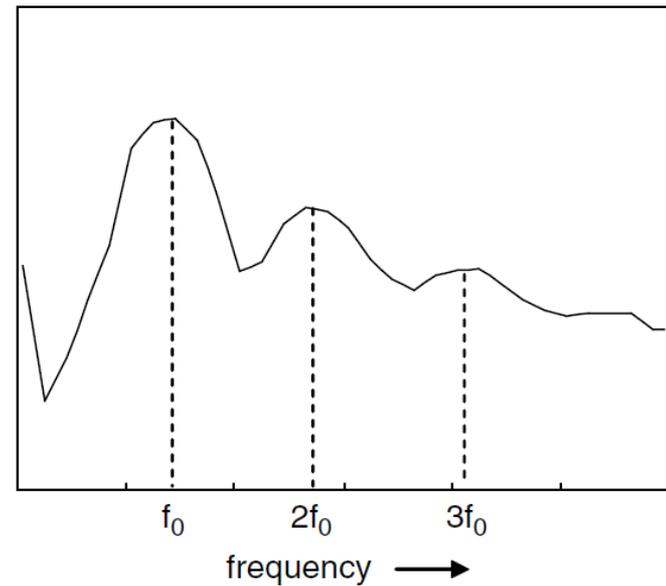
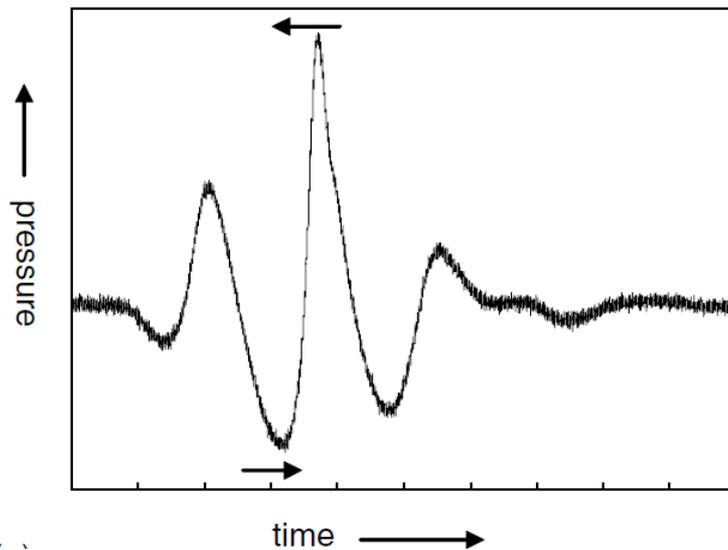
(b)

# Ultrasound Physics

## □ Ultrasound pulse

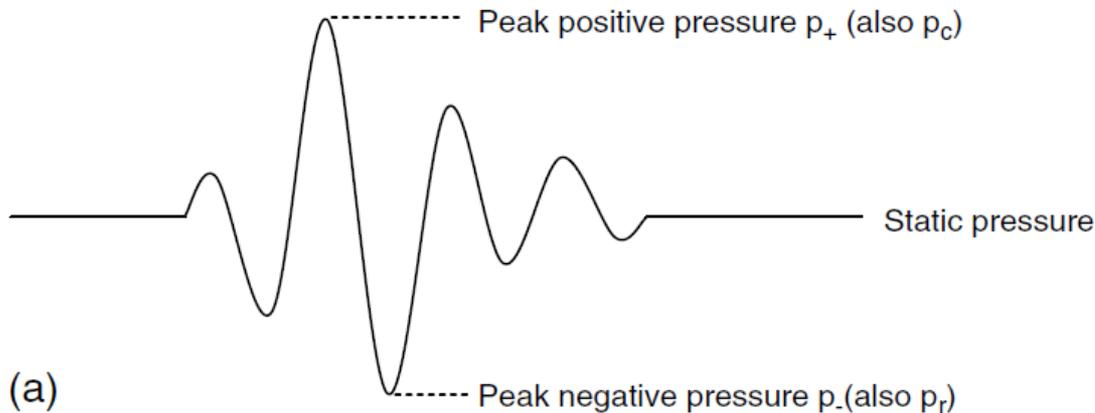


## □ Harmonic Imaging

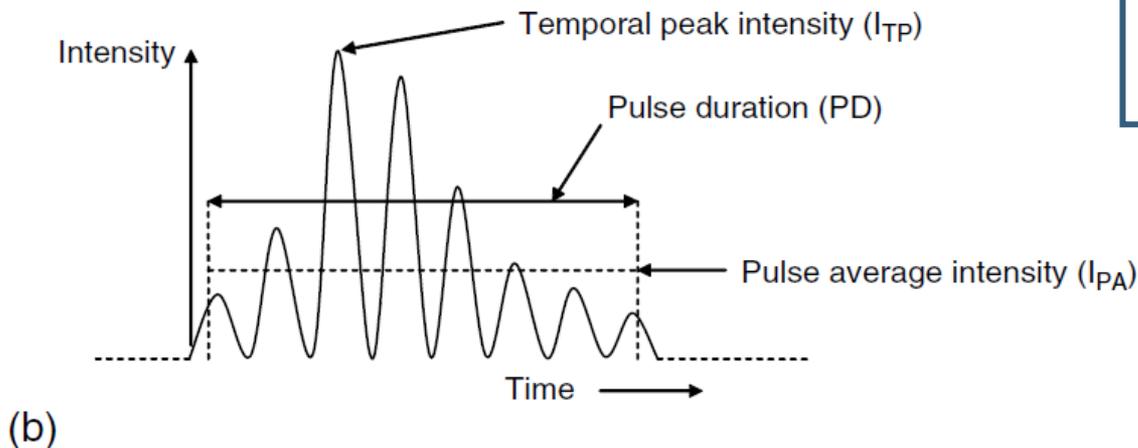


# Ultrasound Physics

## □ Acoustic pressure and intensities within ultrasound beam



$$I = \frac{p^2}{z}$$

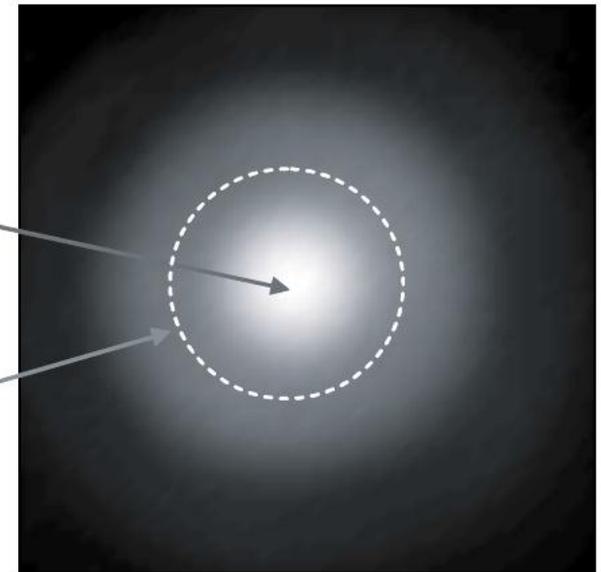
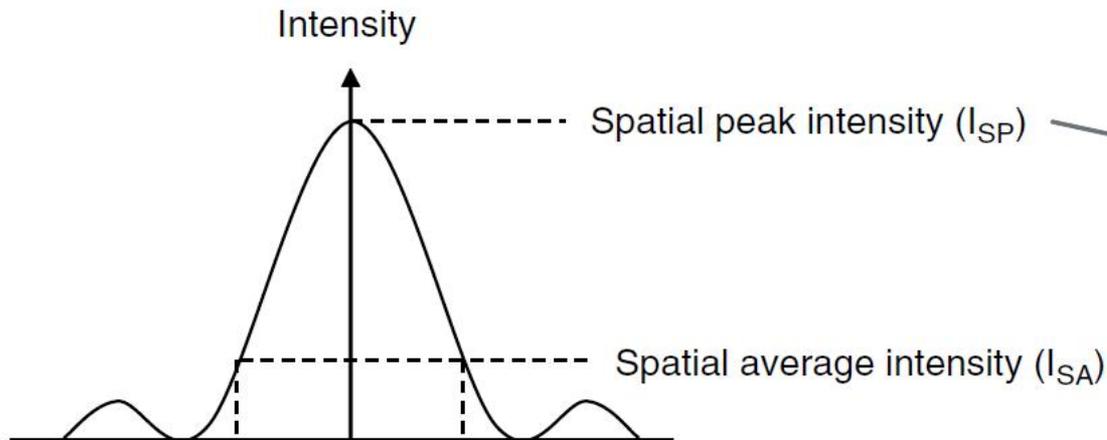
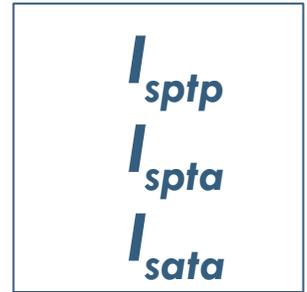
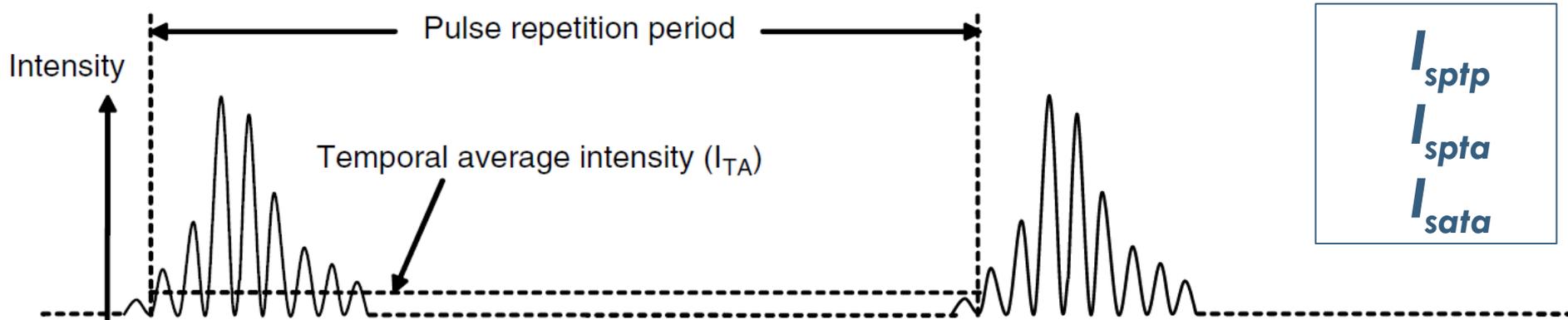


$$PD = 1.25 \times (T_{90} - T_{10})$$

$$I_{PA} = PII / PD$$

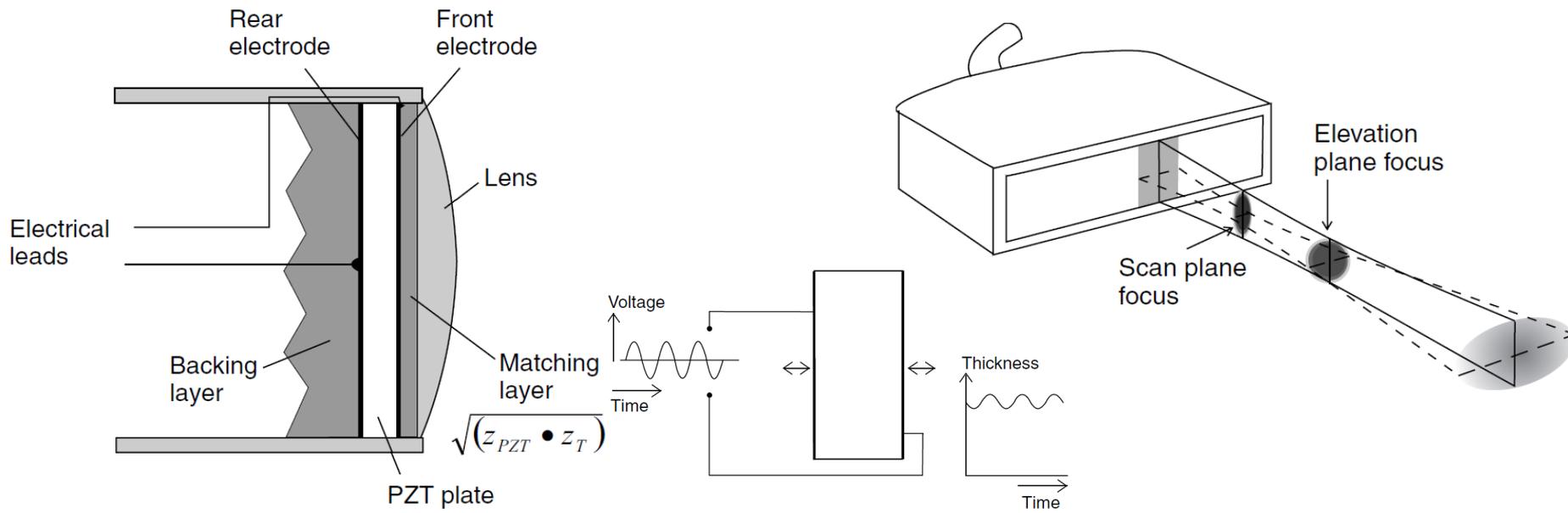
# Ultrasound Physics

## □ Acoustic pressure and intensities within ultrasound beam



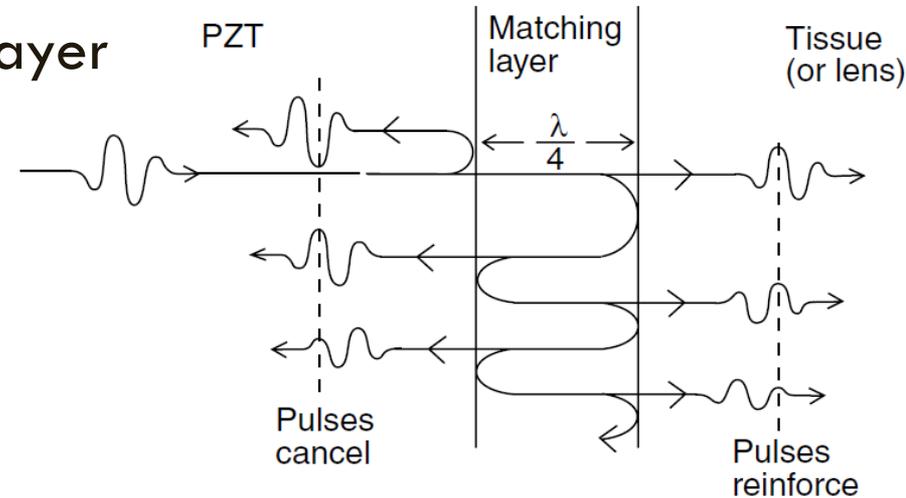
# Transducers and Beamforming

- Transducer: device that actually converts electrical transmission pulses into ultrasonic pulses and, conversely, ultrasonic echo pulses into electrical echo signals
- Beamformer: part of scanner that determines the shape, size and position of the interrogating beams by controlling electrical signals to and from the transducer array elements

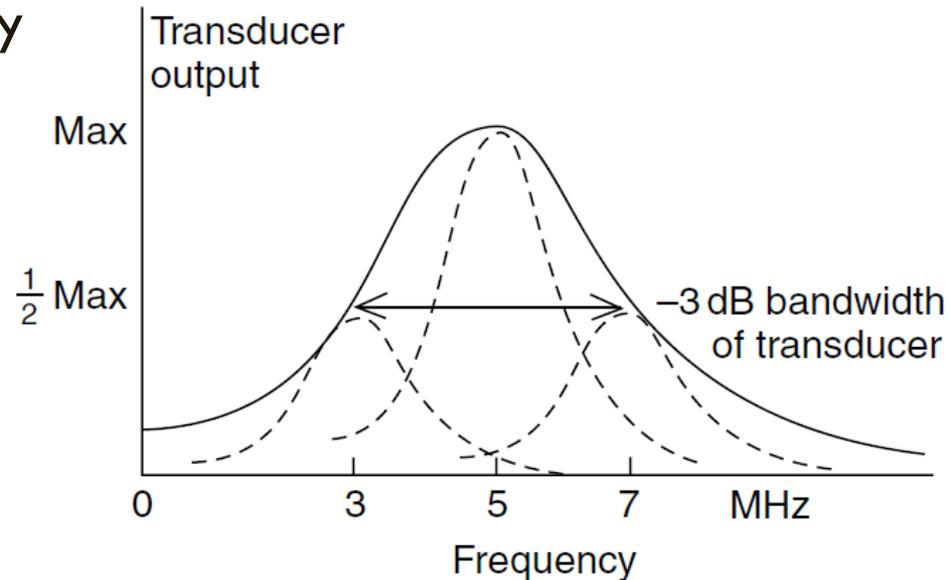


# Transducers and Beamforming

## □ Quarter-wavelength matching layer

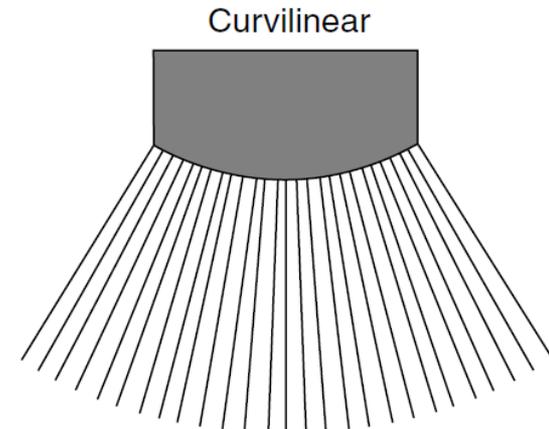
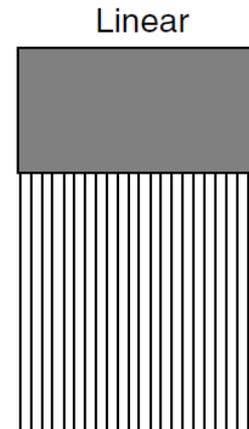
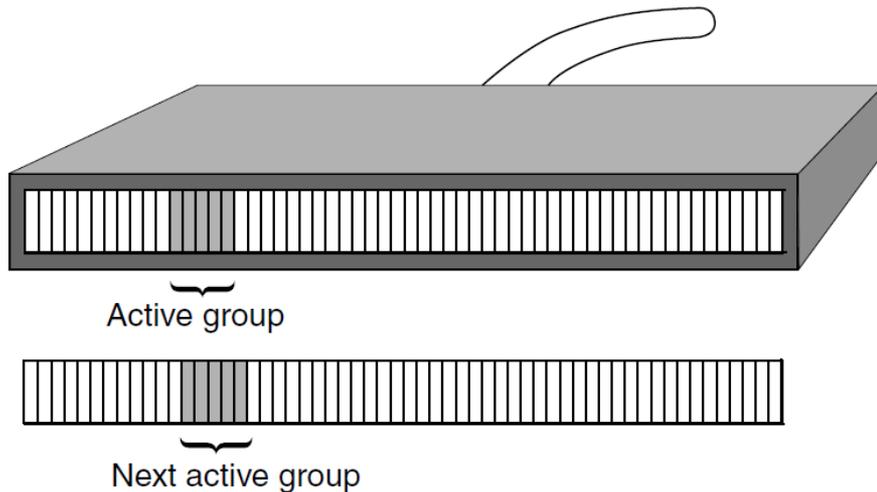
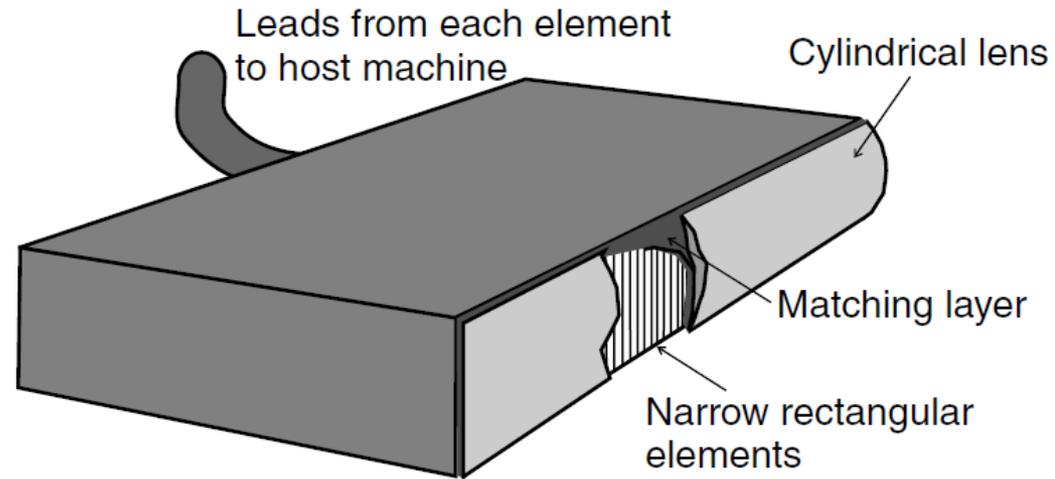
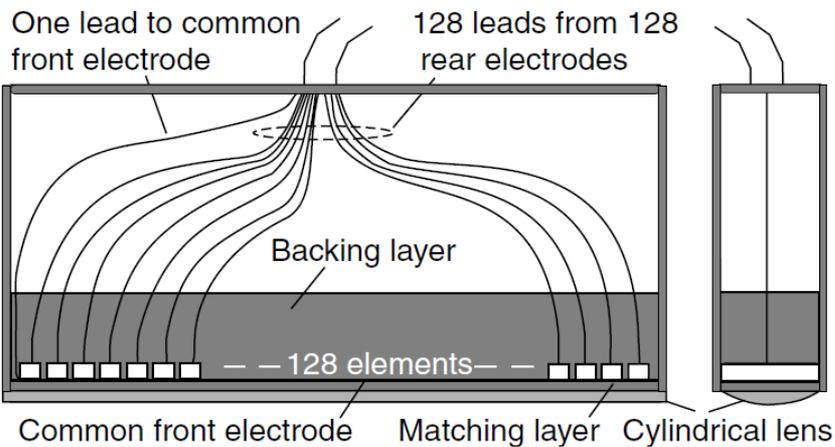


## □ Bandwidth for multi-frequency transducers



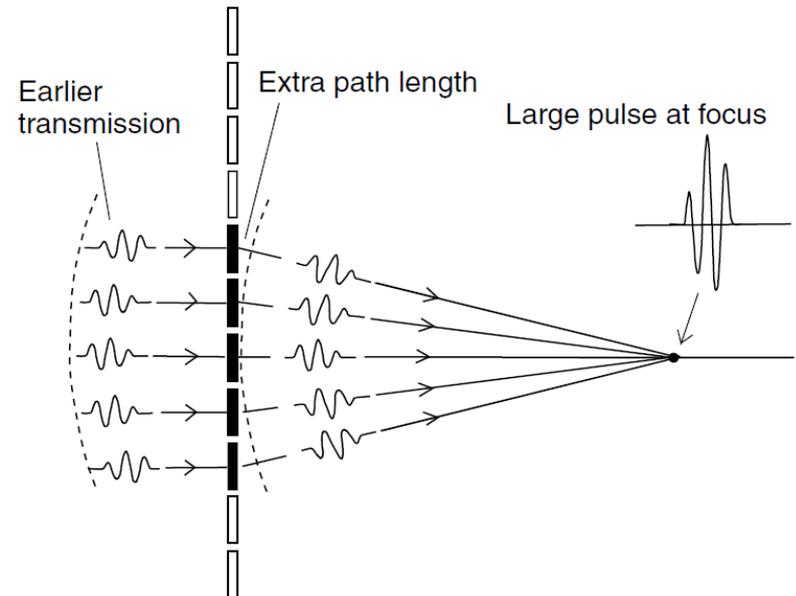
# Transducers and Beamforming

## Linear- and curvilinear-array transducers



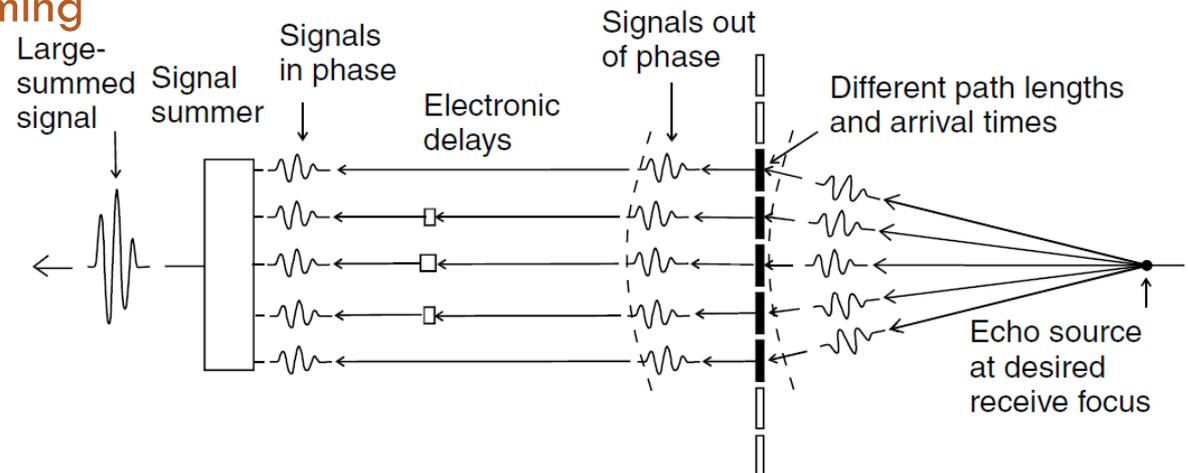
# Transducers and Beamforming

## □ Transmission Focusing



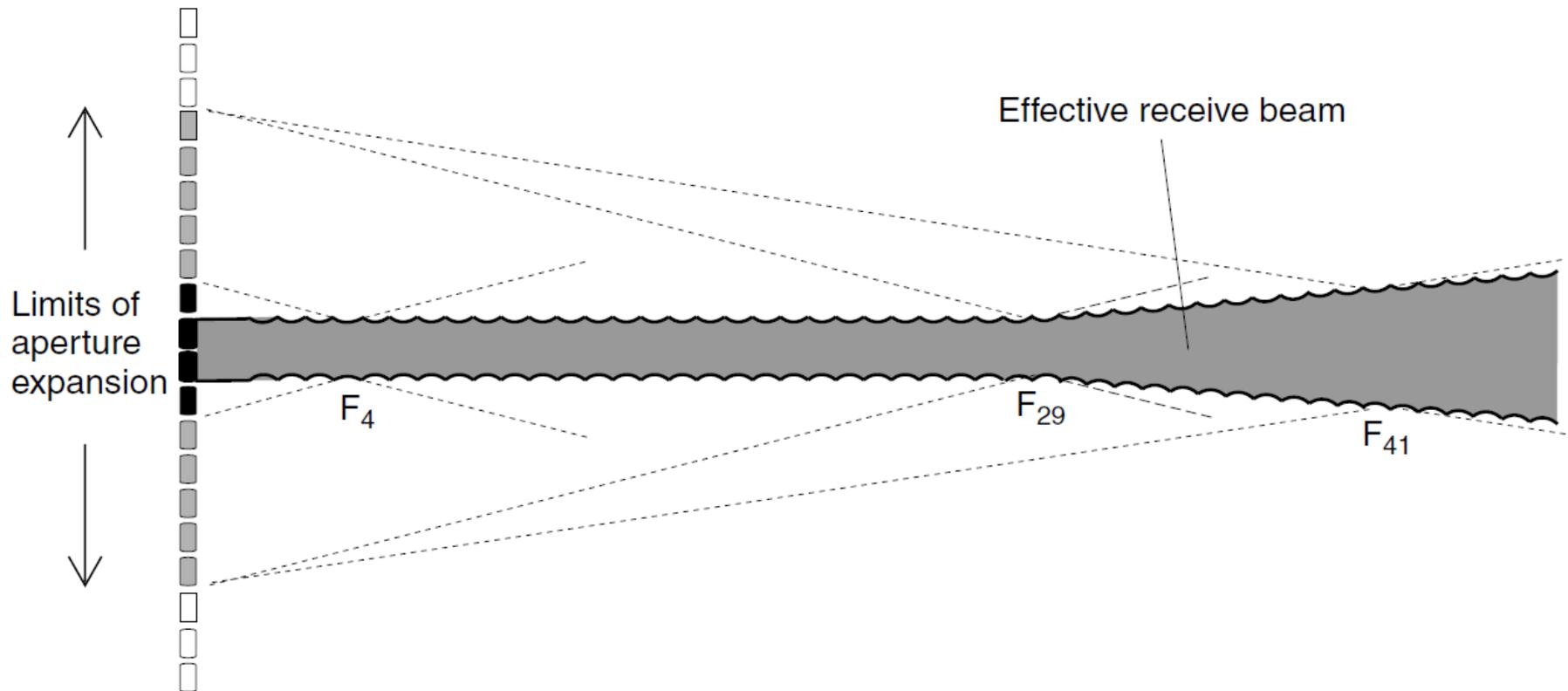
## □ Reception focusing

### ▣ Delay-Sum beamforming



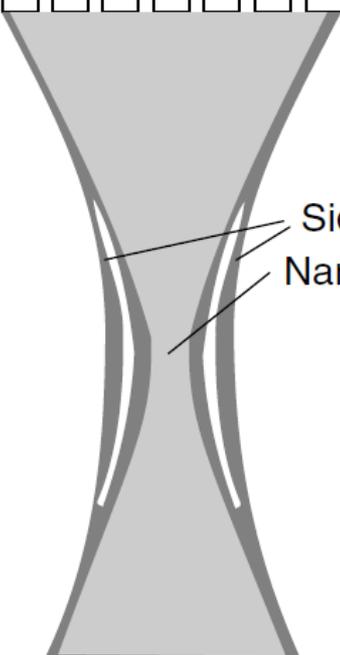
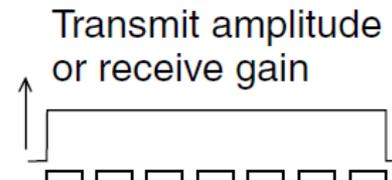
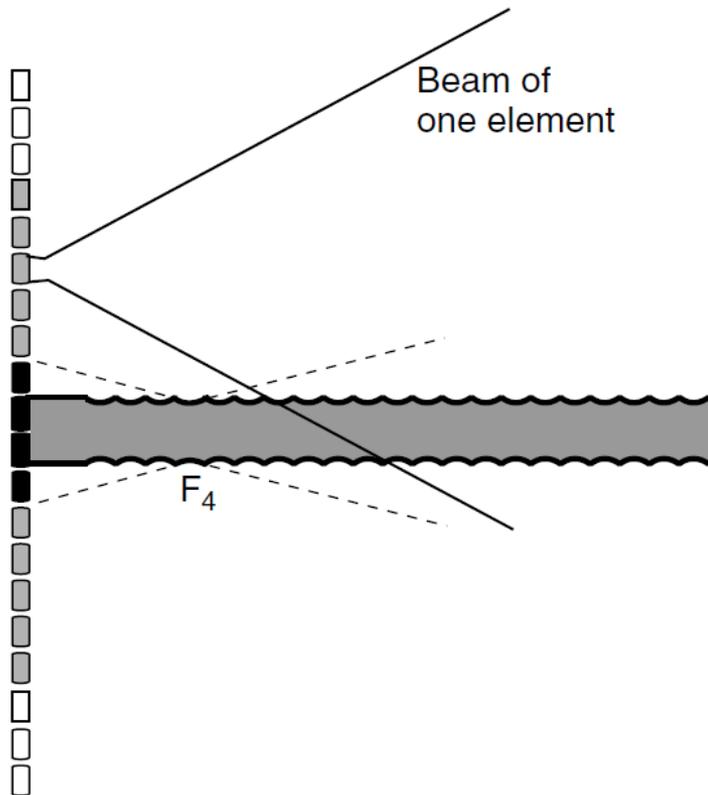
# Transducers and Beamforming

- Dynamic reception focusing

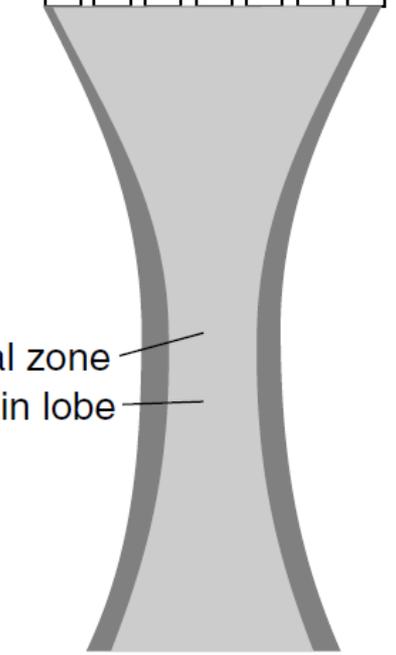
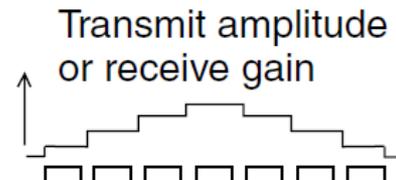


# Transducers and Beamforming

- Beamforming: selecting active elements and apodization



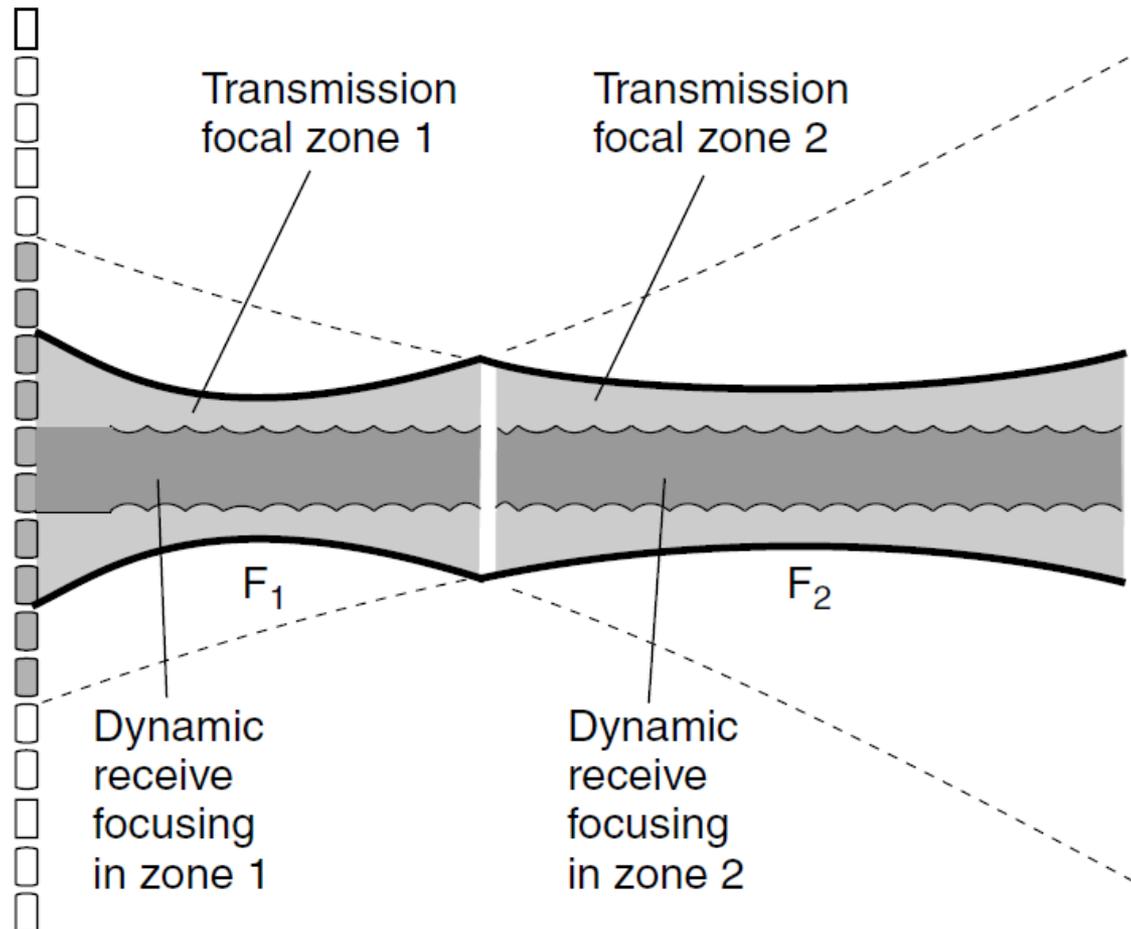
Uniform excitation



Non-uniform excitation (apodization)

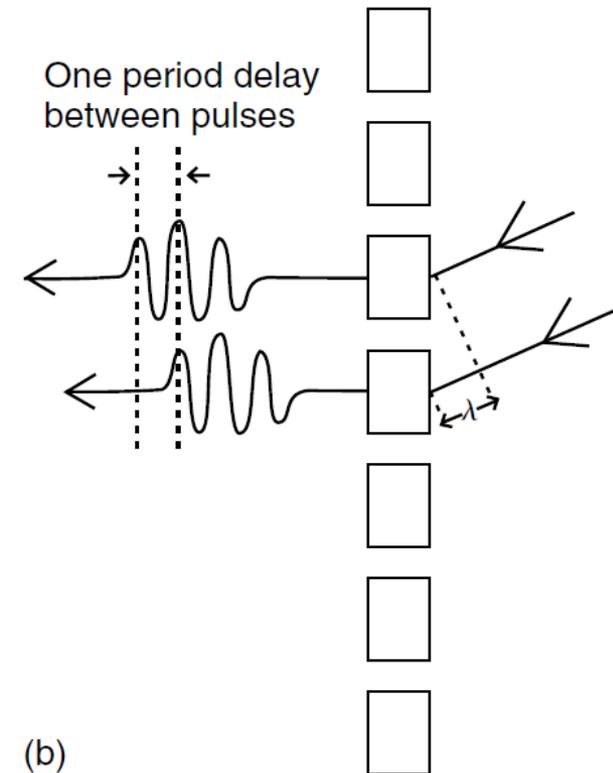
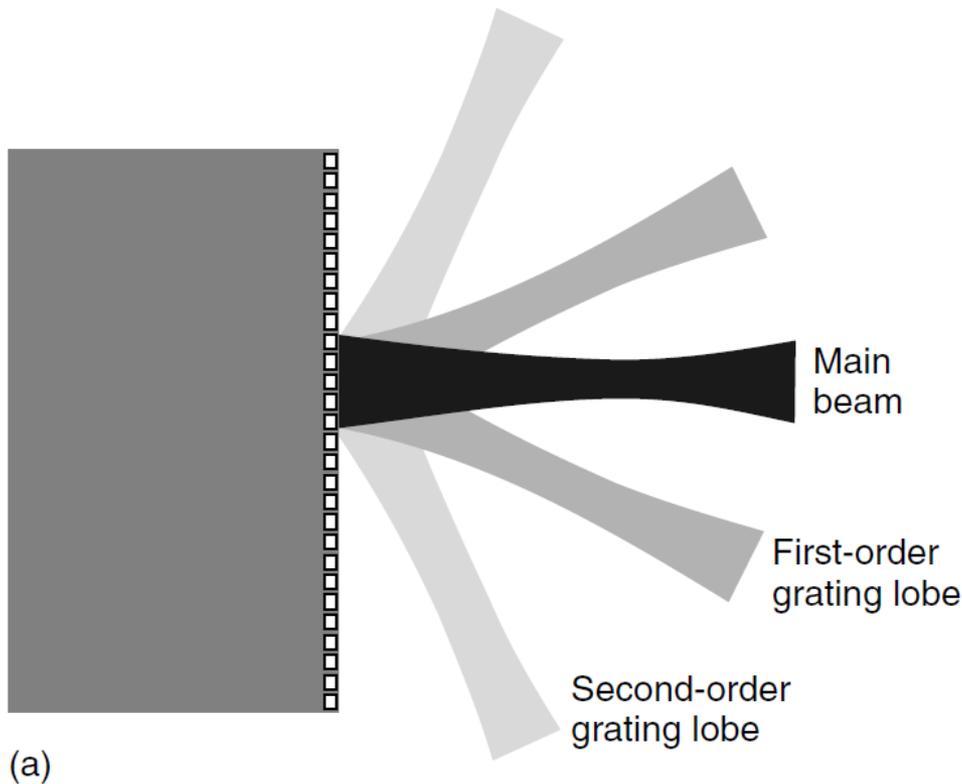
# Transducers and Beamforming

- Beamforming: Multiple Transmission zones



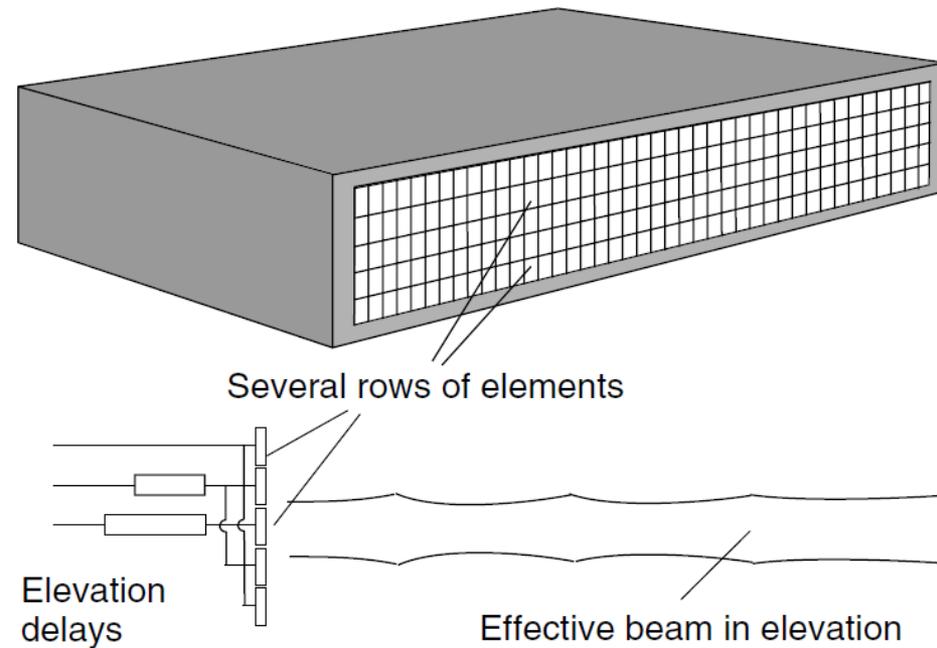
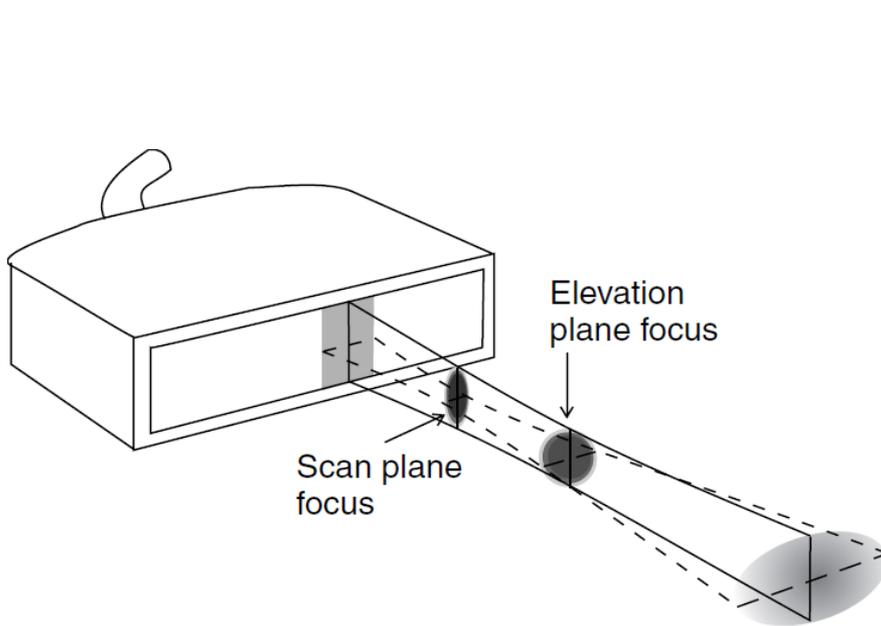
# Transducers and Beamforming

- Beamforming: Grating lobes
  - ▣ No grating lobes, if the center-to-center distance between elements is half a wavelength or less



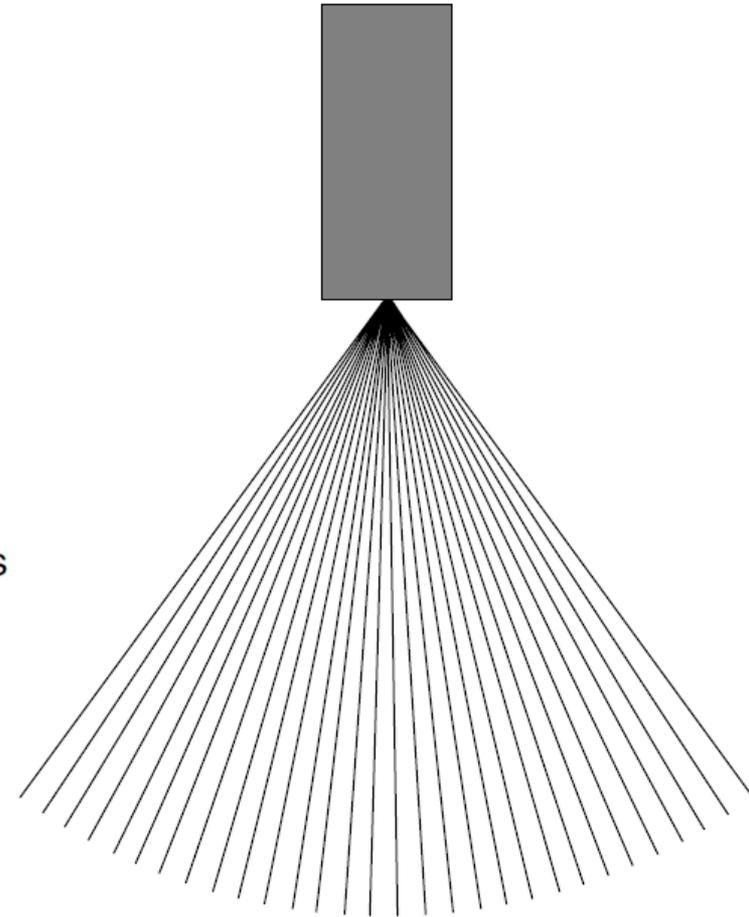
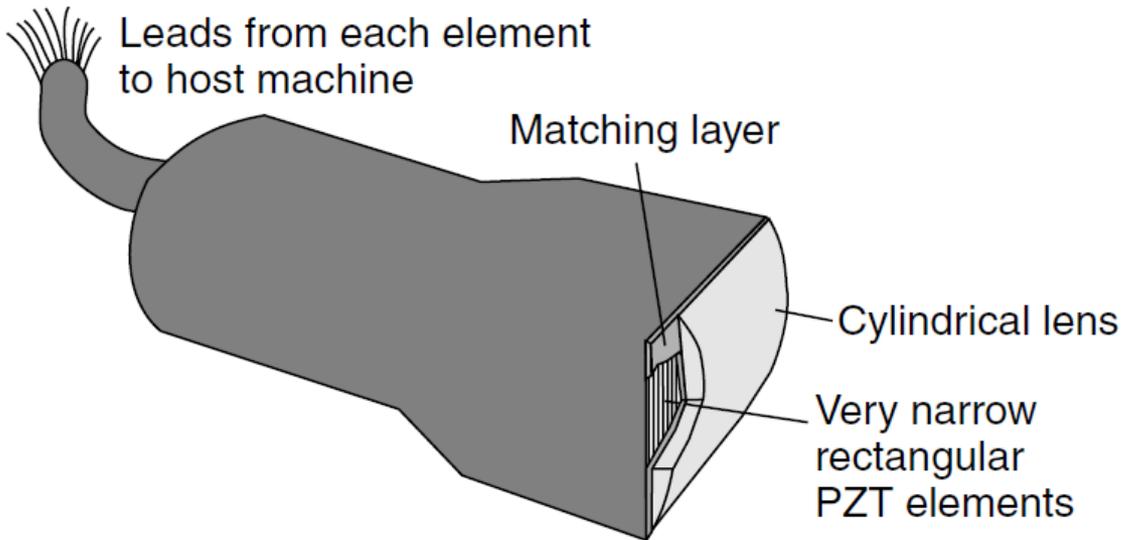
# Transducers and Beamforming

- Slice thickness: elevation direction
  - ▣ 1.5D or 2D arrays



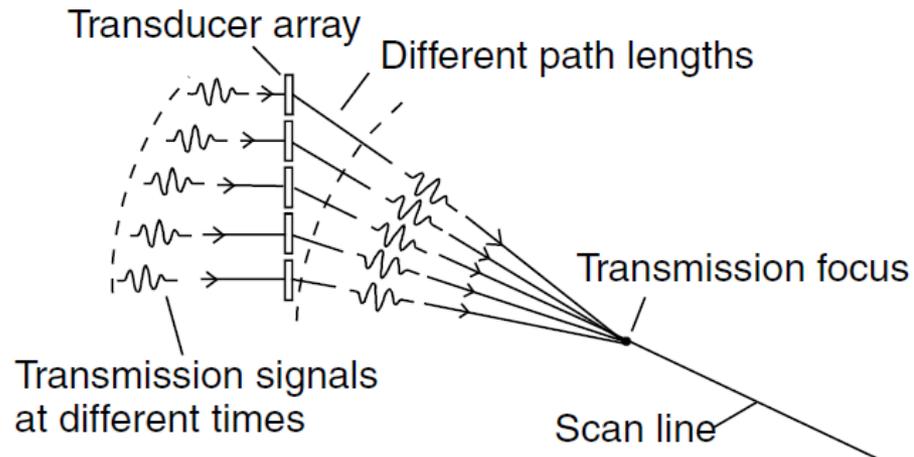
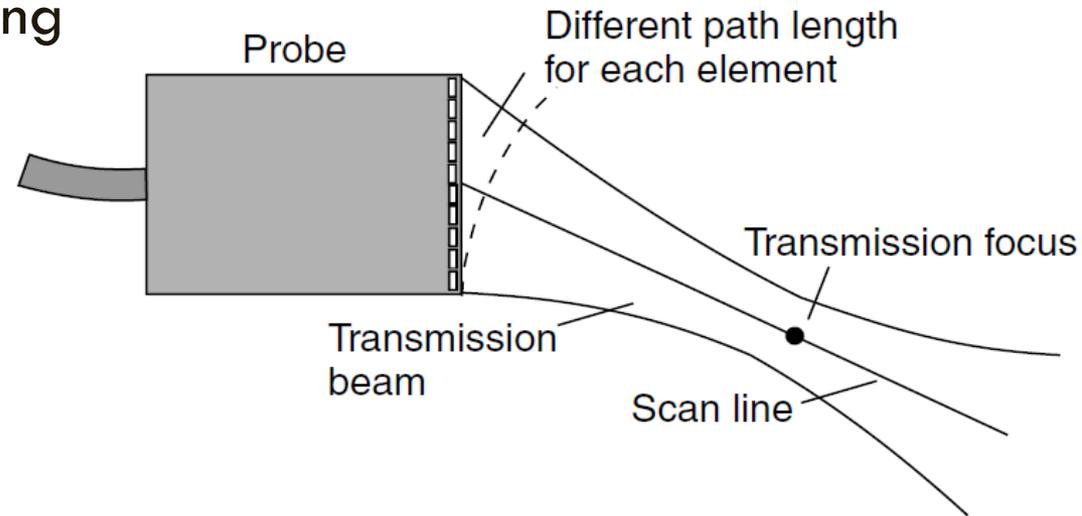
# Transducers and Beamforming

## □ Phased Array transducers



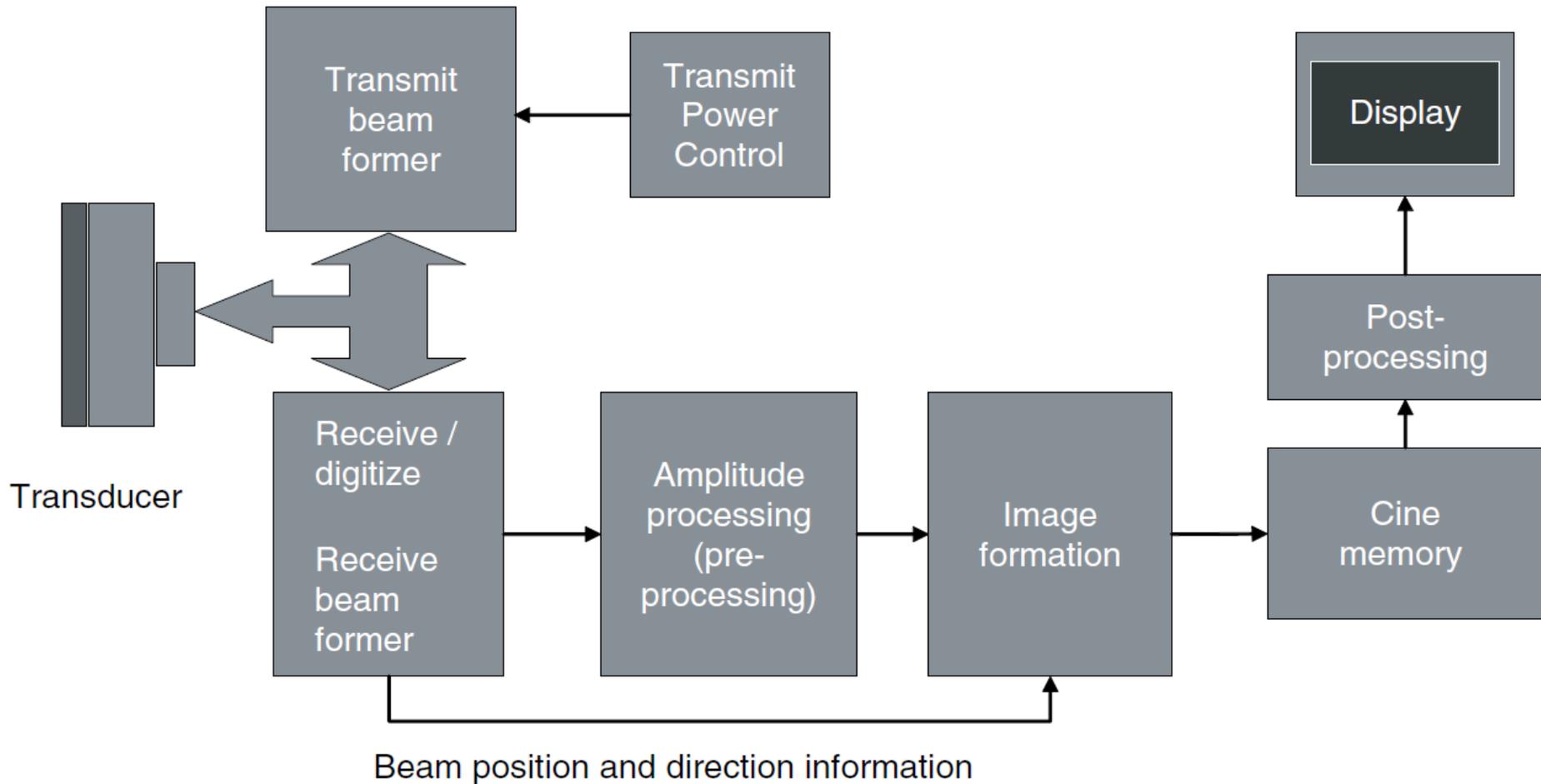
# Transducers and Beamforming

## □ Electronic steering/focusing



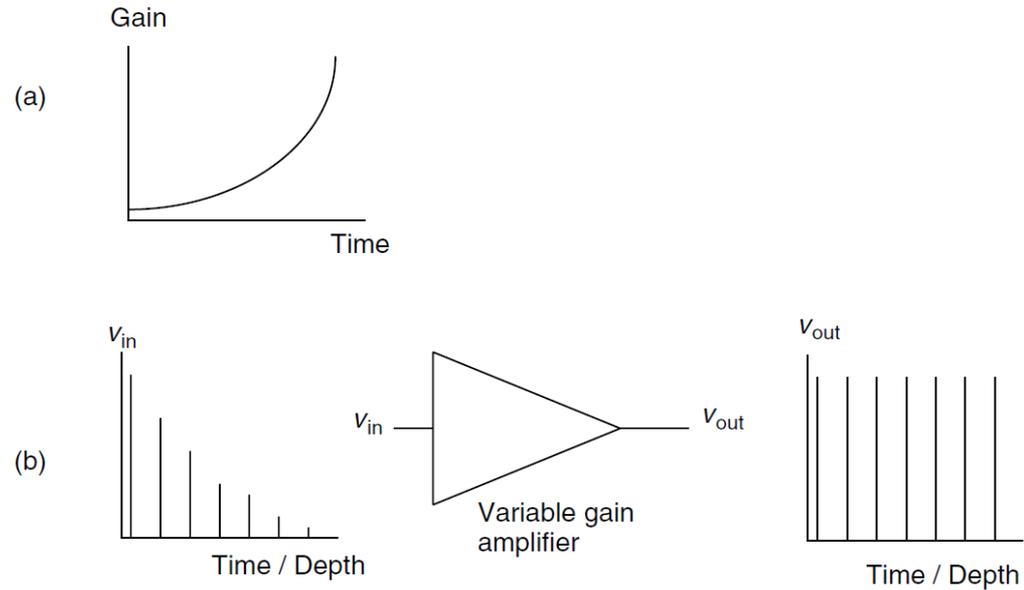
# B-Mode Instrumentation

## □ Processing block diagram



# B-Mode Instrumentation

## □ Time-Gain Compensation



TGC slide controls

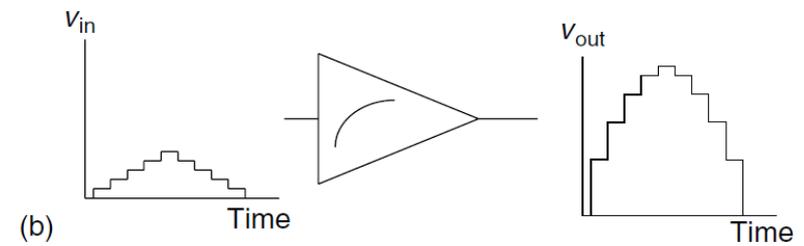
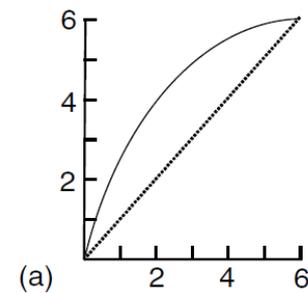
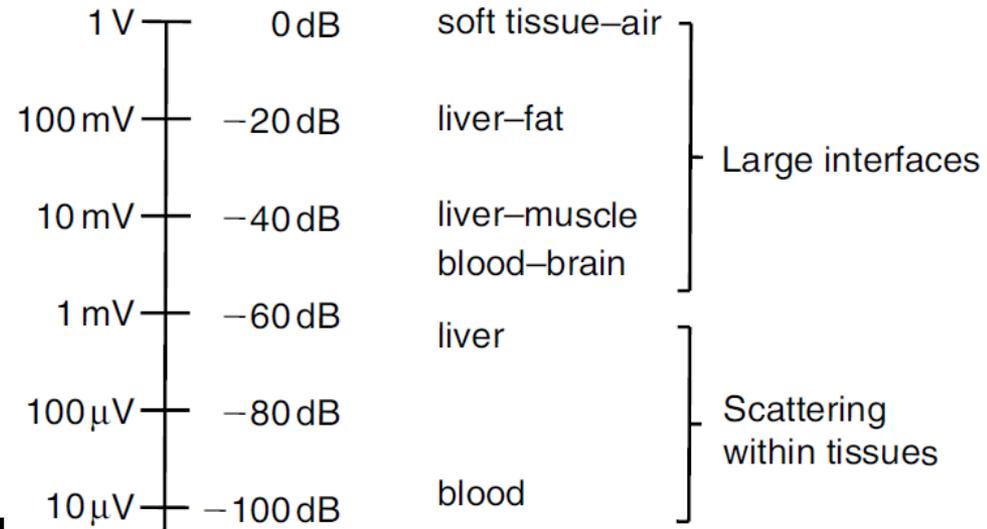
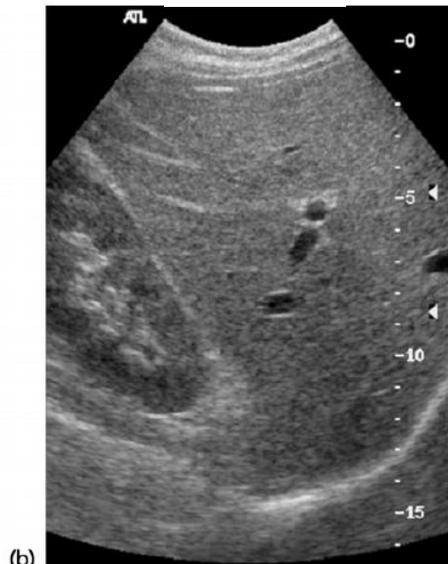
# B-Mode Instrumentation

## Dynamic range of echoes

Bits	Max count	DR (dB)
4	15	24
8	255	48
10	1023	60
12	4095	72

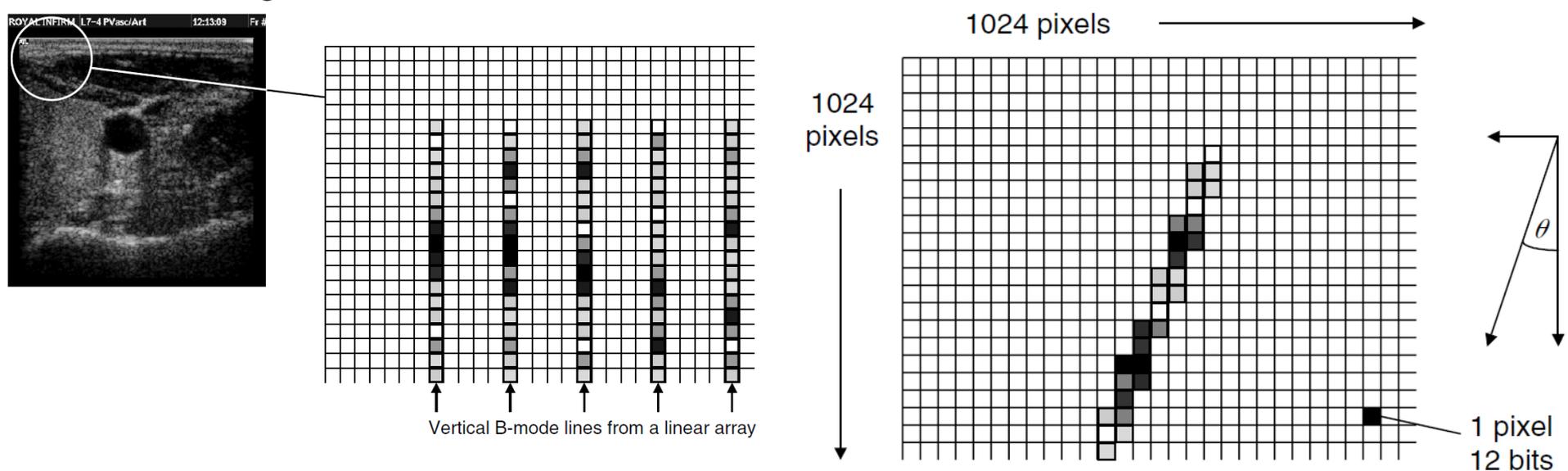
40 dB

80 dB



# B-Mode Instrumentation

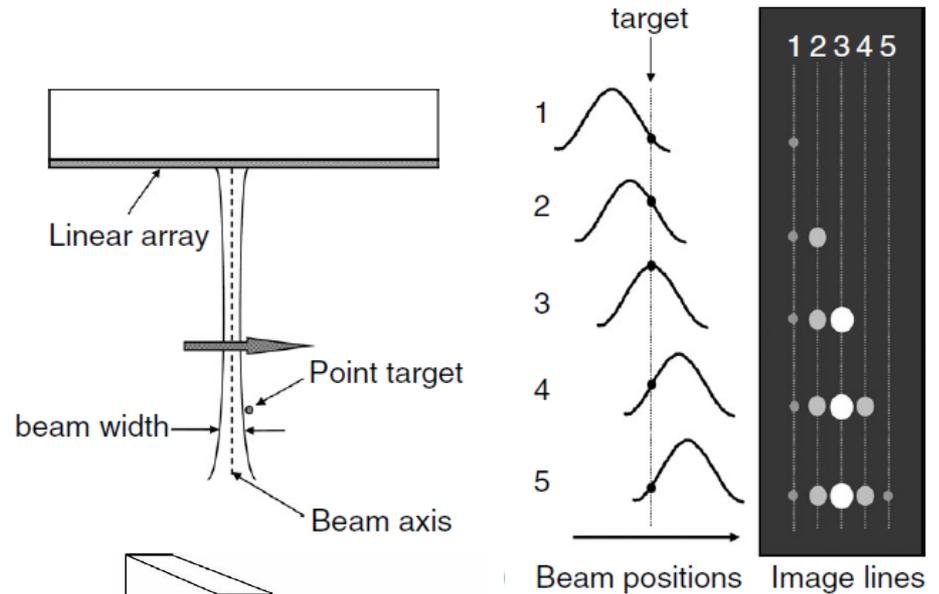
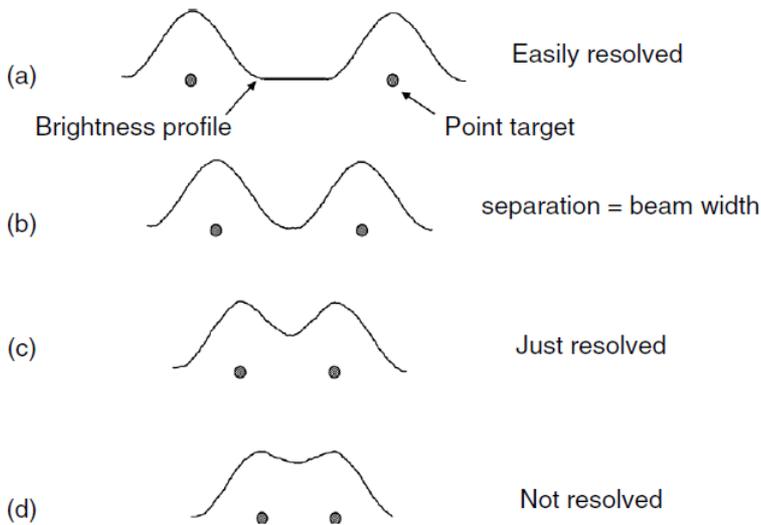
- Image reconstruction: scan conversion and interpolation



- Real-time display: frame every  $1/25$  s
- Freeze: updating frame stops
- Cine Loop: recording of real-time scan as a movie
- Frame Averaging: moving average filter to improve SNR

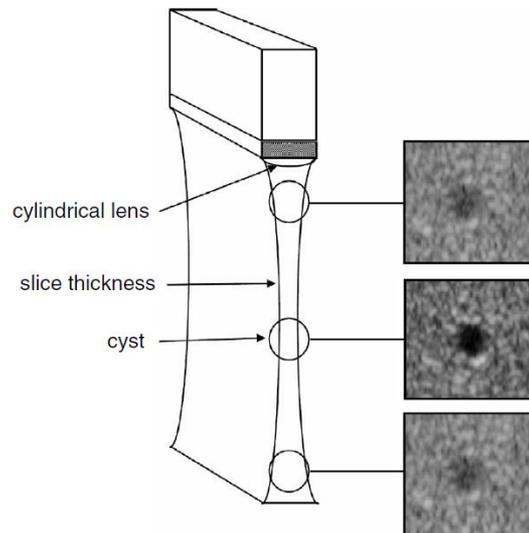
# B-Mode Image Properties

## □ Lateral Resolution



## □ Thickness resolution

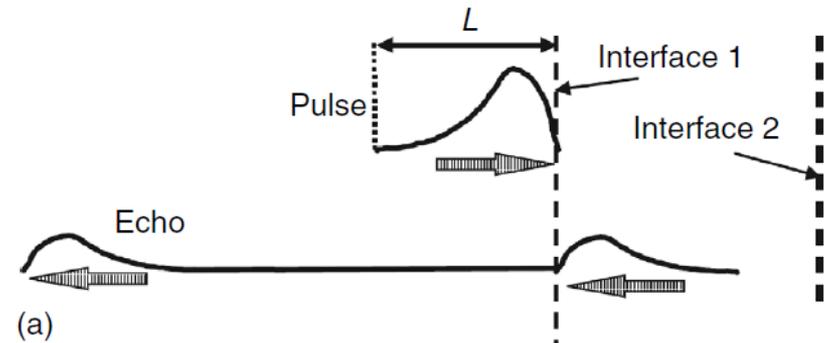
### ▣ Elevation



# B-Mode Image Properties

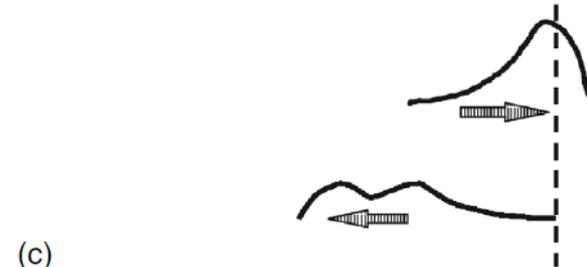
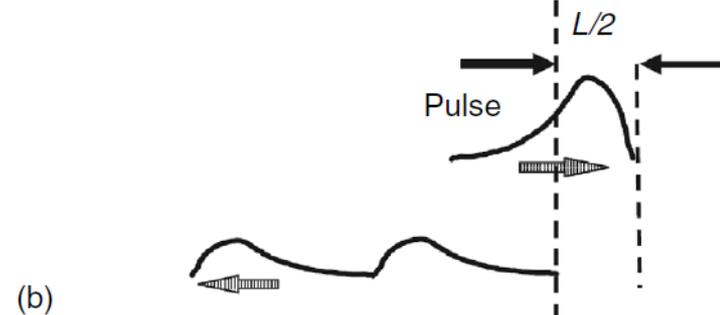
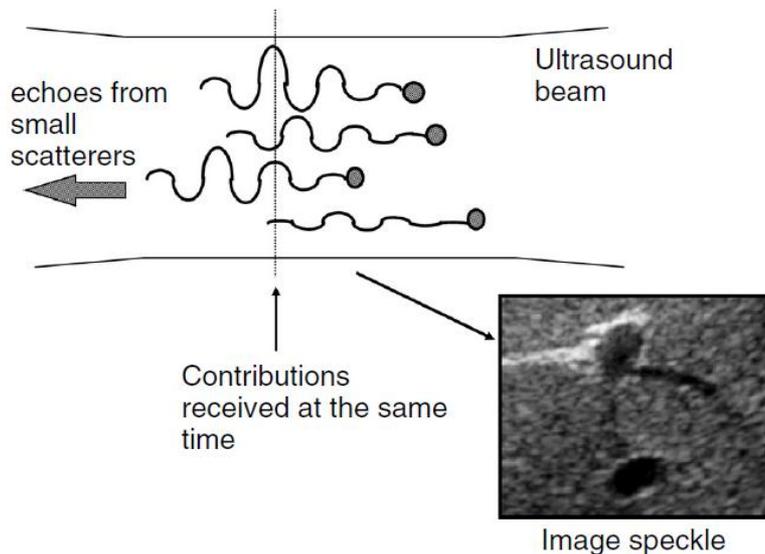
## □ Axial resolution

- Half pulse length



## □ Speckle

- Random yet stationary pattern

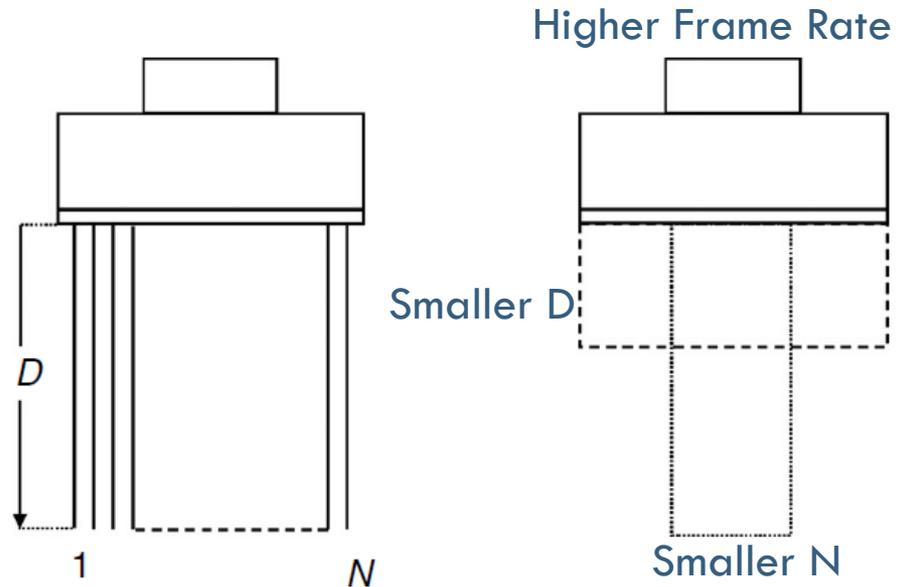


# B-Mode Image Properties

- Frame time / Frame rate
  - ▣ Time to scan a complete image

$$\text{frame time} = 2DN/c$$

$$\text{frame rate} = (c/2DN)$$



- ▣ Example: time to scan 1 cm =  $2 \times 1 \text{ cm} / c = 2 \text{ cm} / (1540 \text{ m/s}) = 13 \mu\text{s}$   
Then, frame time to scan a 20 cm depth with 128 lines =  $13 \mu\text{s} \times 20 \times 128$   
Frame rate =  $1 / \text{frame time} = 30 \text{ frames/s}$

# Assignments

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- Chapter 2: problems 3, 4, 5, 7, 10
- Chapter 3: problems 1, 2, 3, 4, 5, 6, 7, 8, 9, 10
- Chapter 4: problems 1, 2, 3, 4, 5