

Medical Image Reconstruction Term II – 2010

Topic 2: Reconstruction from Nonuniformly Sampled k-Space (2)

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Kadah's Method

Progressive Magnetic Resonance Image Reconstruction Based on Iterative Solution of a Sparse Linear System

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- Algebraic Solution
- Iterative reconstruction method that provides an optimal solution in the least-squares sense
- Based on a practical imaging model
- Progressive reconstruction capability
- Simple mechanism to control trade-off between accuracy and speed
- Embedded inhomogeneity correction and spatial domain constraints

Disadvantages of Previous Methods

- Reconstructed images do not represent optimality in any sense
- Variation of performance with form of k-space trajectory
- Lack of explicit methodology to trade-off accuracy and speed of reconstruction
- Not possible to progressively improve the accuracy of reconstruction
- Not possible to embed field inhomogeneity correction or constraints into the reconstruction

Theory

- Assume a piecewise constant spatial domain representing display using pixels
 - Image composed of pixel each of uniform intensity
 - Image can be represented by a sum of 2D RECT functions
- Assume spatial domain to be compact
 - Field of view is always finite in length
- > The image can be expressed in terms of gate functions as,

$$f(x, y) = \sum_{n=0}^{N-1} \sum_{m=0}^{M-1} \alpha_{n,m} \cdot \Pi(x - x_n, y - y_m)$$

Theory

Applying continuous Fourier transform,

$$F(k_{x},k_{y}) = \int_{-\infty-\infty}^{\infty} \int_{n=0}^{\infty} \sum_{m=0}^{N-1} \sum_{m=0}^{M-1} \alpha_{n,m} \cdot \Pi(x-x_{n}, y-y_{m}) \cdot e^{-j2\pi(k_{x}x+k_{y}y)} dxdy,$$

Hence,

$$F(k_{x},k_{y}) = Sinc(w_{x}k_{x}) \cdot Sinc(w_{y}k_{y}) \sum_{n=0}^{N-1} \sum_{m=0}^{M-1} \alpha_{n,m} \cdot e^{-j2\pi(k_{x}x_{n}+k_{y}y_{m})}.$$

This can be expressed in the form of a linear system as

$$\vec{b} = \mathbf{A}\vec{v}$$

• A matrix is $\sim N^2 \times N^2$ and complex-valued

Theory

- Observation: A matrix is ~N²xN² and complex-valued
 - Solve a 16384x16384 linear system to get a 128x128 image
 - Very difficult to solve in practice because of size

$$\begin{bmatrix} \frac{F(k_x^0, k_y^0)}{\operatorname{Sinc}(w_x k_x^0) \cdot \operatorname{Sinc}(w_y k_y^0)} \\ \frac{F(k_x^1, k_y^1)}{\operatorname{Sinc}(w_x k_x^1) \cdot \operatorname{Sinc}(w_y k_y^1)} \\ \vdots \\ \frac{F(k_x^{L-1}, k_y^{L-1})}{\operatorname{Sinc}(w_x k_x^{L-1}) \cdot \operatorname{Sinc}(w_y k_y^{L-1})} \end{bmatrix}_{L \times 1}$$

$$= \vec{b} = A \cdot \vec{v}$$

$$= \begin{bmatrix} e^{-j\pi(k_x^0 \cdot x_0 + k_y^0 \cdot y_0)} & e^{-j\pi(k_x^0 \cdot x_0 + k_y^0 \cdot y_1)} & \cdots & e^{-j\pi(k_x^0 \cdot x_{N-1} + k_y^0 \cdot y_{M-1})} \\ e^{-j\pi(k_x^1 \cdot x_0 + k_y^1 \cdot y_0)} & e^{-j\pi(k_x^1 \cdot x_0 + k_y^1 \cdot y_1)} & \cdots & e^{-j\pi(k_x^1 \cdot x_{N-1} + k_y^1 \cdot y_{M-1})} \\ \vdots & \vdots & \cdots & \vdots \\ e^{-j\pi(k_x^{L-1} \cdot x_0 + k_y^{L-1} \cdot y_0)} & e^{-j\pi(k_x^{L-1} \cdot x_0 + k_y^{L-1} \cdot y_1)} & \cdots & e^{-j\pi(k_x^{L-1} \cdot x_{N-1} + k_y^{L-1} \cdot y_{M-1})} \end{bmatrix}_{L \times N \cdot M} \cdot \begin{bmatrix} \alpha_{0,0} \\ \alpha_{0,1} \\ \vdots \\ \alpha_{N-1,M-1} \end{bmatrix}_{N \cdot M \times 1}$$

Idea

- Problem: A matrix is dense and computational complexity of solution is prohibitive
- Solution Strategy: Try to make the A matrix sparse by seeking a compact representation of rows in terms of suitable basis functions
- Observation: applying a I-D Fourier transformation to the rows of A matrix results in energy concentration in only a few elements

Methods

 Multiply the rows of the system matrix by the NxM-point discrete Fourier transform matrix H in the following



Methods

How to multiply H without changing the linear system?

Row energy compacting transformation converts the system into a sparse linear system as follows:

$$\vec{b} = \mathbf{A}\vec{v} = \mathbf{A}\cdot\mathbf{H}^H\cdot\mathbf{H}\cdot\vec{v} = (\mathbf{H}\cdot\mathbf{A}^H)^H\cdot\vec{V} = \mathbf{M}\cdot\vec{V},$$

- To convert to sparse form, only a percentage η of kernel energy in each row is retained
 - The only parameter in the new method
 - Correlates directly to both image quality and computational complexity
- Sparse matrix techniques are used to store and manipulate the new linear system
 - Since the linear system is sparse, iterative methods such as conjugate gradient can be used to solve the system with very low complexity



Results

256x256
 Analytical
 Shepp-Logan
 Phantom
 (Radial sampling)



Results

 256x256 Real data from a resolution phantom at 3T from a Siemens Magnetom Trio system using a spiral trajectory



Results



Discussion

- Full control over the accuracy versus complexity trade-off through η selection
- Computational complexity is comparable to conventional gridding with small kernel
 - O(g(η)·L) per CGM step, where g(η) is the average # of elements/row, L=# of acquired k-space samples
 - Average 4.9 elements/row to retain 92% of energy
- Progressive reconstruction is possible
 - Add more iterations to process
 - > Use a different reconstruction table with higher η

Exercise

- Verify the energy compactness transformation and generate Figure 2 (c) for any trajectory you prefer. [I Point]
- Assuming that we have a rectilinear sampling instead of the nonuniform sampling in this paper, how do you expect the linear system to look like? [I Points]
- Assume that we are constructing an NxN image, compute the exact number of computation (not an order or computation) detailing the list of computations in each step in the implementation. [I Point]